

Active Contours — Snakes

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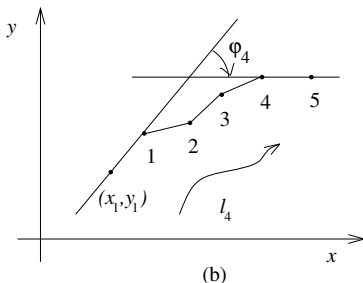
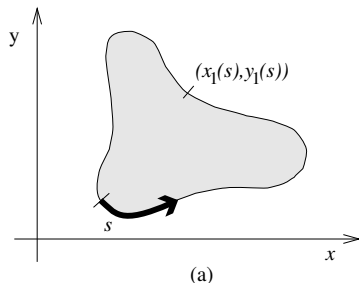
Snake principles

- ▶ Initial curve (manual)
- ▶ Curve evolves using image data
- ▶ ... until finds desired boundary
- ▶ Criterion = image term + smoothness (internal) term + shape term

(show animate heart.gif, ventricles_movie.gif)

Traditional snakes

Curve is parameterized as $\mathbf{v}(s) = [x(s), y(s)]$ with $s \in [0, 1]$



Minimize energy

$$\begin{aligned} E_{\text{snake}}^* &= \int_0^1 E_{\text{snake}}(\mathbf{v}(s)) ds \\ &= \int_0^1 \left(E_{\text{int}}(\mathbf{v}(s)) + E_{\text{image}}(\mathbf{v}(s)) + E_{\text{con}}(\mathbf{v}(s)) \right) ds, \end{aligned}$$

Internal energy term

$$E_{\text{int}} = \alpha \left| \frac{d\mathbf{v}}{ds} \right|^2 + \beta \left| \frac{d^2\mathbf{v}}{ds^2} \right|^2 ,$$

α, β specify *elasticity* and *stiffness*. Can depend on s .

Image energy term

$$E_{\text{image}} = w_{\text{line}} E_{\text{line}} + w_{\text{edge}} E_{\text{edge}}$$

- ▶ Line functional attracts to white/black parts

$$E_{\text{line}} = \pm f(x, y)$$

- ▶ Edge functional attracts to strong edges

$$E_{\text{edge}} = -|\nabla f(x, y)|^2$$

smooth/denoise before/after taking the gradient

- ▶ Other application-dependent image energy terms.

Shape term — prefer likely shapes.

Euler-Lagrange equations

$$E_{\text{snake}}^* = \int_0^1 E_{\text{snake}}(\mathbf{v}(s), \mathbf{v}'(s)) ds = \int_0^1 E_{\text{snake}}(\mathbf{v}, \mathbf{v}_s) ds$$

For optimal $\mathbf{v}(s)$ it must hold

$$\frac{d}{ds} E_{\mathbf{v}_s} - E_{\mathbf{v}} = 0$$

Substituting for E_{int} in $E_{\text{snake}} = E_{\text{int}} + E_{\text{image}}$:

$$-\frac{d}{ds} \left(\alpha(s) \frac{d\mathbf{v}}{ds} \right) + \frac{d^2}{ds^2} \left(\beta(s) \frac{d^2\mathbf{v}}{ds^2} \right) + \nabla E_{\text{ext}}(\mathbf{v}(s)) = 0$$

Supposing constant α, β

$$-\alpha \frac{d^2\mathbf{v}}{ds^2} + \beta \frac{d^4\mathbf{v}}{ds^4} + \underbrace{\nabla E_{\text{ext}}(\mathbf{v}(s))}_{\mathbf{f}_E} = 0$$

where \mathbf{f}_E is an external force

Solving EL equations

Euler-Lagrange equation for $\mathbf{v}(s)$

$$-\alpha \frac{d^2 \mathbf{v}}{ds^2} + \beta \frac{d^4 \mathbf{v}}{ds^4} + \kappa \mathbf{f}_E = 0$$

Gradient descent — time evolution converges to a solution

$$\frac{\partial \mathbf{v}}{\partial t} = \alpha \frac{\partial^2 \mathbf{v}}{\partial s^2} - \beta \frac{\partial^4 \mathbf{v}}{\partial s^4} + \kappa \mathbf{f}_E$$

Balloon force

What to do, when no image information is available? Grow/shrink.

$$\frac{\partial \mathbf{v}}{\partial t} = \alpha \frac{\partial^2 \mathbf{v}}{\partial s^2} - \beta \frac{\partial^4 \mathbf{v}}{\partial s^4} + \kappa \mathbf{f}_E + \lambda \mathbf{f}_B$$

Balloon force \mathbf{f}_B perpendicular to the snake curve.

Discretization and implementation

- ▶ Unit time steps $\Delta t = 1$
- ▶ Snake is represented by two vectors containing the x and y coordinates of a sequence of points on the snake curve.
- ▶ Distance between subsequent points is maintained close to 1 pixel.
- ▶ Resample if needed.
- ▶ Snake is supposed to be closed and non-intersecting.

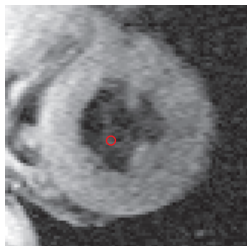
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- ▶ Snake is supposed to be closed and non-intersecting.
- ▶ Derivatives approximated by discrete convolution

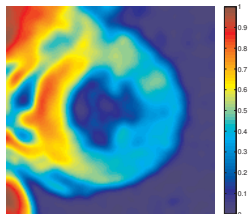
$$\alpha \frac{\partial^2 \mathbf{v}}{\partial s^2} - \beta \frac{\partial^4 \mathbf{v}}{\partial s^4} \Big|_{s=s_i} \approx h * \begin{bmatrix} x(s_i) \\ y(s_i) \end{bmatrix} .$$

- ▶ Stop when area no longer changes.

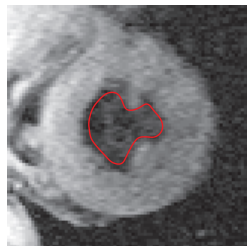
Snake example 1



MRI image



Energy



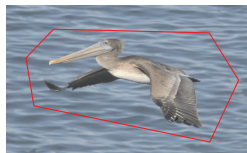
result

Energy = smoothed image

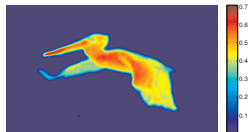
$\alpha = 0.1$, $\beta = 0.01$, $\kappa = 0.2$, $\lambda = 0.05$.

Growing balloon force.

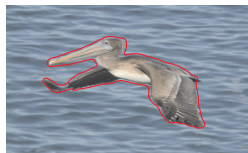
Snake example 2



MRI image



Energy



result

Energy = image converted to grayscale, thresholded, smoothed.

$\alpha = 0.1$, $\beta = 0.1$, $\kappa = 0.3$, $\lambda = -0.05$

Shrinking balloon force.

Gradient vector flow (GVF) snakes

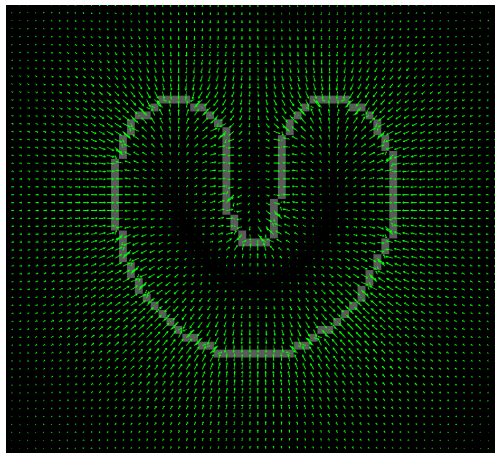
(Xu and Prince)

- ▶ Image gives information close to edges
- ▶ No information in flat region
- ▶ An *edge map* f is high where we want the snake to be attracted, i.e. $\mathbf{f}_E = \nabla f$
- ▶ GVF provides a smooth interpolation $\mathbf{g} = (u, v)$ everywhere from f
- ▶ Alternative to balloon force, less parameter tuning.

GVF field

Minimize

$$\iint \mu (u_x^2 + u_y^2 + v_x^2 + v_y^2) + \|\nabla f\|^2 \|\mathbf{g} - \nabla f\|^2 dx dy$$



GVF minimization

$$\iint \mu (u_x^2 + u_y^2 + v_x^2 + v_y^2) + \|\nabla f\|^2 \|\mathbf{g} - \nabla f\|^2 dx dy$$

At minimum, Euler-Lagrange equations must hold

$$\mu \Delta u - (u - f_x) (f_x^2 + f_y^2) = 0,$$

$$\mu \Delta v - (v - f_y) (f_x^2 + f_y^2) = 0,$$

Solved by gradient descent / time evolution:

$$u_t(x, y, t) = \mu \Delta u(x, y, t) - (u(x, y, t) - f_x(x, y)) (f_x(x, y)^2 + f_y(x, y)^2)$$

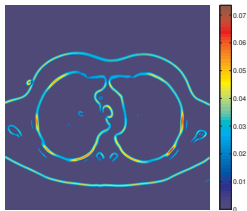
$$v_t(x, y, t) = \mu \Delta v(x, y, t) - (v(x, y, t) - f_y(x, y)) (f_x(x, y)^2 + f_y(x, y)^2)$$

- ▶ Equations are discretized and solved by numeric integration with a fixed time step on a uniform grid.
- ▶ Multiresolution needed for speed and robustness.

GVF example



Lung slice



Energy



result

Energy = thresholded smoothed edge map $E = \|\nabla G_\sigma * f\|$

No balloon force needed.