Medical ultrasound imaging

Modern ultrasound imaging

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Doppler ultrasound

US contrast agents

Harmonic imaging

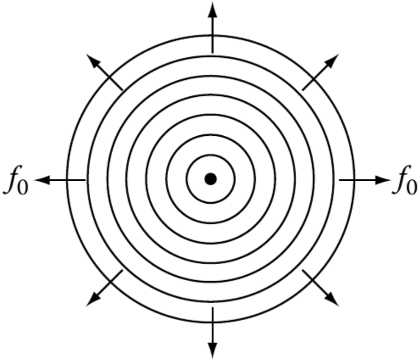
3D US imaging

Christian Doppler

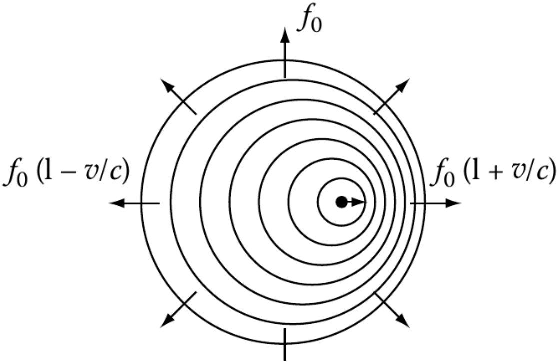
1803–1853

During his time in Prague as a professor he married and had five children, whilst he published over 50 articles on mathematics, physics and astronomy. In 1842 he published his most famous paper Über das farbige Licht der Doppelsterne ("Concerning the Colored Light of Double Stars"), which contained his first statement of the Doppler effect.

Doppler frequency shift

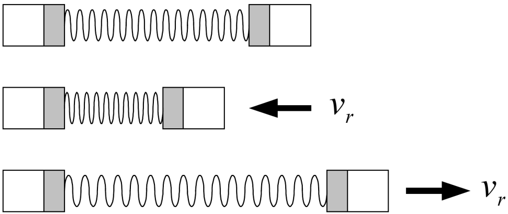


stationary



moving source

Stationary source, moving receiver

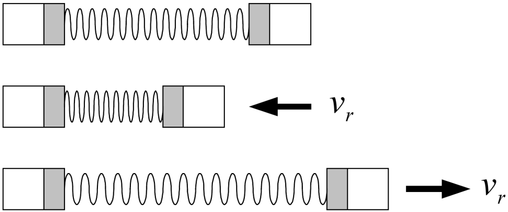


$$f_r = f_s + \frac{v_r}{\lambda_s} = f_s + \frac{v_r}{c} f_s = f_s + f_d, \quad \text{since} \quad \lambda_s = \frac{c}{f_s}$$

Doppler shift

$$f_d = \frac{v_r}{c} f_s$$

Stationary source, moving receiver



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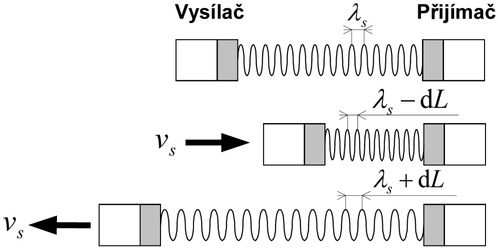
Doppler shift

$$f_d = \frac{v_r}{c} f_s$$

Example: For $f = 5\,\text{MHz}$, $v_r = 1\,\text{cm/s}$, $f_d = 33\,\text{Hz}$.

Stationary receiver, moving source



Wavelength change

$$\delta\lambda = v_s T_s = \frac{v_s}{f_s}$$

$$\lambda_r = \lambda_s - \delta\lambda = \frac{c}{f_s} - \frac{v_s}{f_s}$$

$$f_r = \frac{c}{\lambda_r} = \frac{c}{c - v_s} f_s$$

Stationary receiver, moving source (2)

$$f_r = \frac{c}{\lambda_r} = \frac{c}{c - v_s} f_s = \frac{1}{1 - \frac{v_s}{c}} f_s$$

Stationary receiver, moving source (2)

$$f_r = \frac{c}{\lambda_r} = \frac{c}{c - v_s} f_s = \frac{1}{1 - \frac{v_s}{c}} f_s$$

From Taylor series, for $x \ll 1$

$$\frac{1}{1-x} = 1 + x + \frac{x^2}{2} + \cdots \approx 1 + x$$

For $v \ll c$

$$f_r \approx \left(1 + \frac{v_s}{c}\right) f_s = f_s + f_d$$

Doppler shift

$$f_d = \frac{v_s}{c} f_s$$

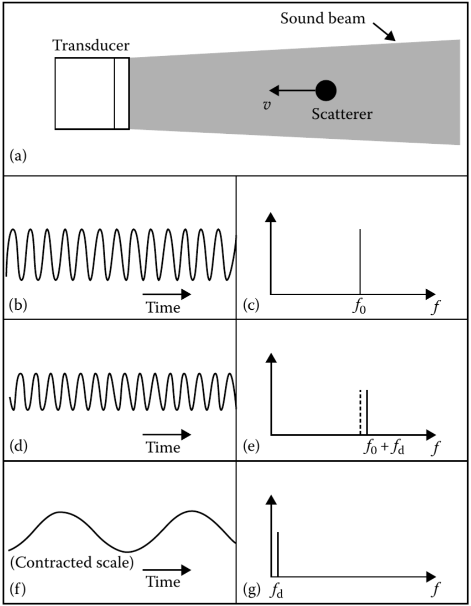
Blood flow speed measurement

- Doppler effect: Frequence changes if the source moves with respect to the receiver.
- Reflection from red blood cells
- Red blood cells
  - Moving receiver
  - Moving source
- Doppler shift

$$f_r = f_t + f_d \qquad \boxed{f_d \approx 2\frac{v}{c} f_c}$$

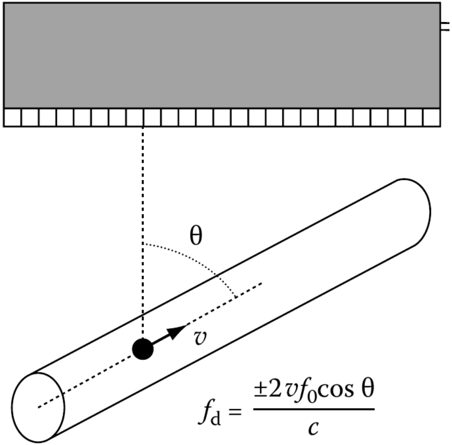
Moving scatterer

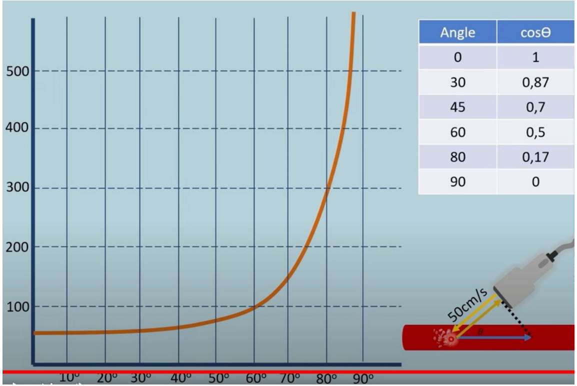
time and frequency domains



Angle dependency

We only measure the projection along the ray: $v \cos \theta$



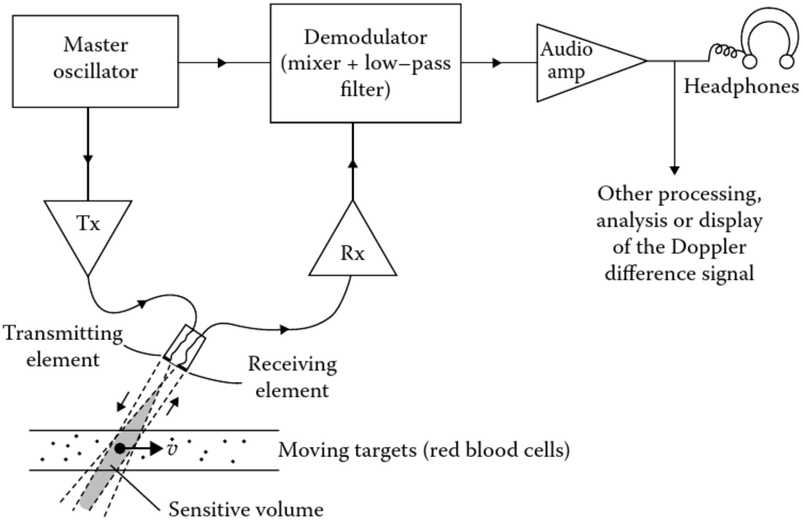


$f_0 = f_s$

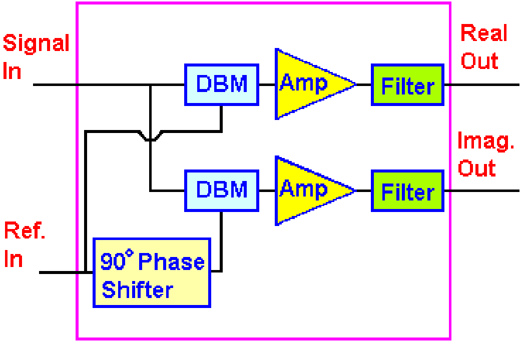
Angle dependency (2)

- Insonation angle $90^\circ \longrightarrow$ weak or no signal.
- Known angle $\longrightarrow$ angle correction.

Continuous wave Doppler



Quadrature detector (1)



- *Input:* $g_a = \cos(at)$, $\quad g_b = \cos(bt)$
- *Output:* $g = g_a g_b = \frac{1}{2}\cos((a+b)t) + \frac{1}{2}\cos((a-b)t)$
- Signal $\cos((a+b)t)$ can be filtered (low-pass filter)
- Difference frequence signal $s_r = \cos((a-b)t)$
- "Imaginary" signal s_i shifted by 90°: $\sin((a-b)t)$

Quadrature detector (2)

DBM (Double-Balanced Mixer) in Ultrasound Demodulation
A Double-Balanced Mixer (DBM) is an electronic component used in signal processing, including ultrasound demodulation.

- Extract modulated signals by mixing the incoming ultrasound wave with a reference signal.
- Suppress unwanted noise and harmonics by canceling out common-mode signals.
- Improve directional selectivity in ultrasound imaging and communication systems.

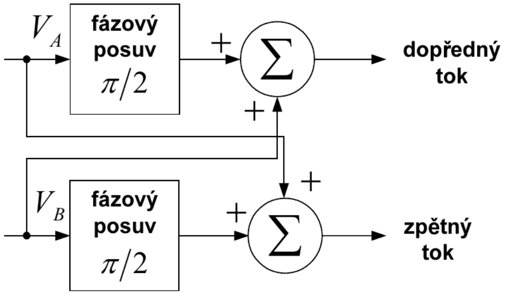
Directional demodulation

To distinguish positive/negative flow direction, $\pm f_d$.

Method 1: Phase-domain processing

- Quadrature mixer with f_s
- Phase offset $\angle s_r = \angle s_i = \pm 90^\circ$

	$f_d > 0$	$f_d < 0$
$s_r + T_{90} s_i$	0	$2 s_r$
$T_{90} s_r + s_i$	$2 s_r$	0



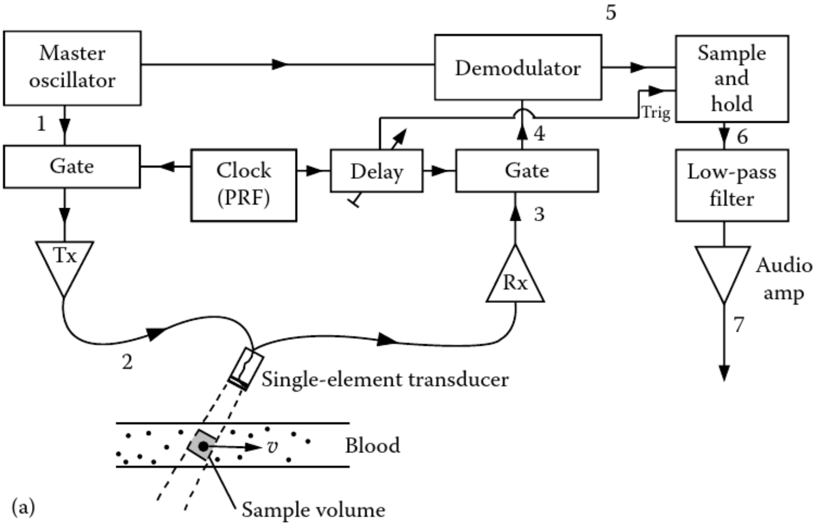
Directional demodulation

To distinguish positive/negative flow direction, $\pm f_d$.

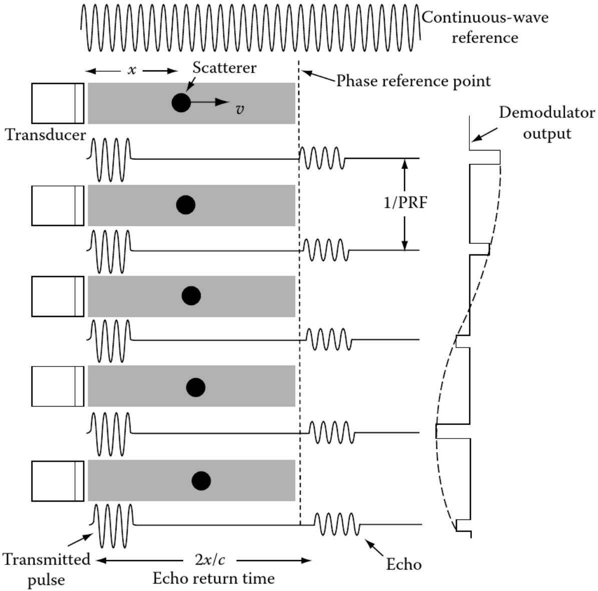
Method 2: Frequency shift

- Quadrature mixer with $f_s + f_o$
- $f_d = 0 \longrightarrow$ mixer output f_o
- $f_d = \mathrm{freq}(s_r) - f_o$

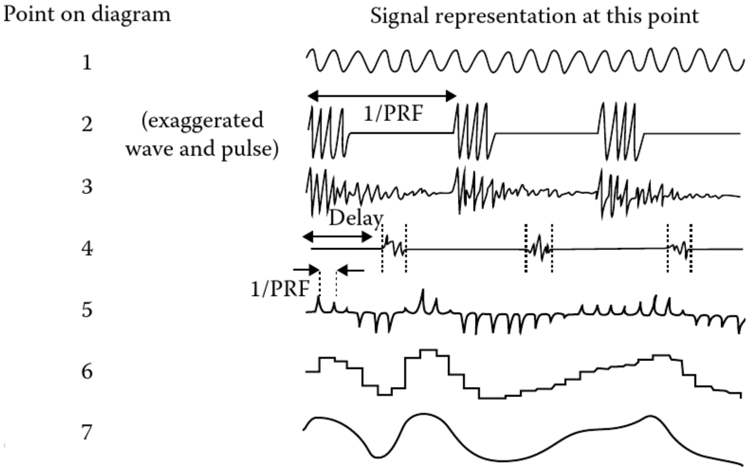
Pulsed wave Doppler
(PW)



Sampled Doppler shift signal

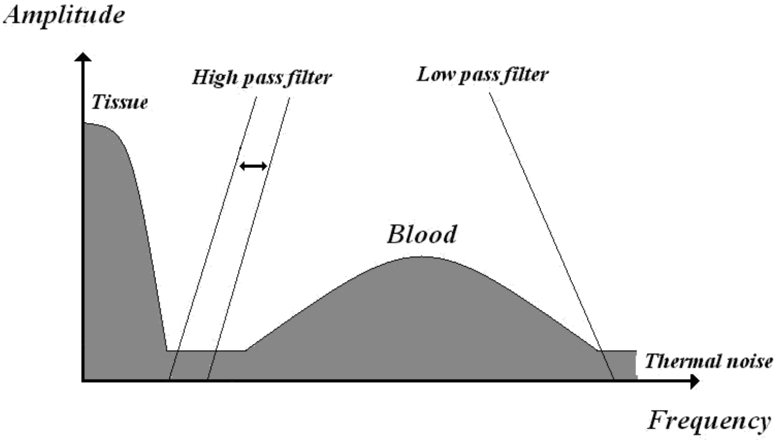


PW Doppler shift signals

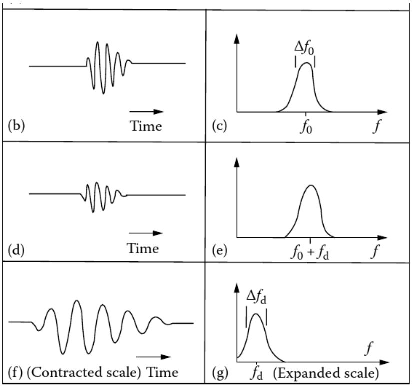


PRF:pulse repetition frequency, 2:transmitted signal, 3:received signal, 4:gated signal, 5:demodulated signal, 6:interpolated signal, 7:output

PW Doppler spectrum



Speed uncertainty

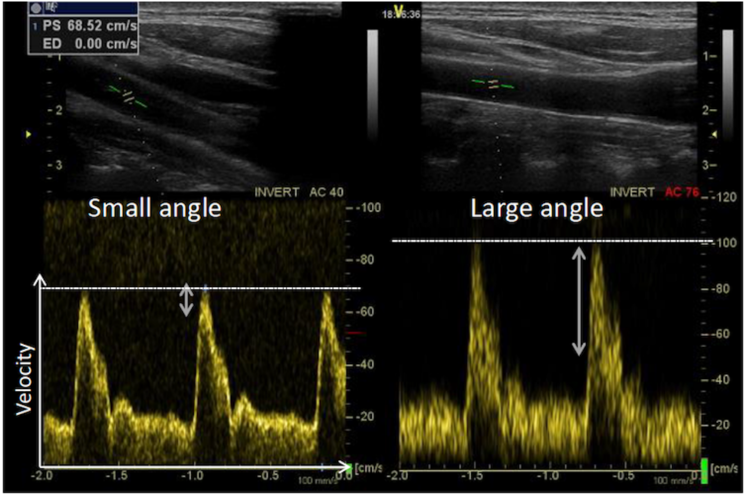


$$\Delta f_d = \frac{2v}{c\tau} = \frac{f_d}{\underbrace{f_s\tau}_{Q}}, \qquad \Delta v = \frac{v}{Q}$$

τ — pulse length, Q — quality factor, number of cycles in a pulse

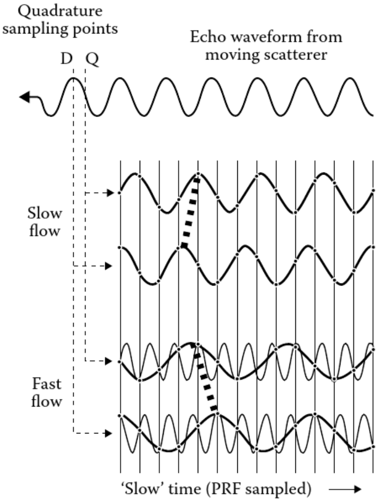
Speed uncertainty

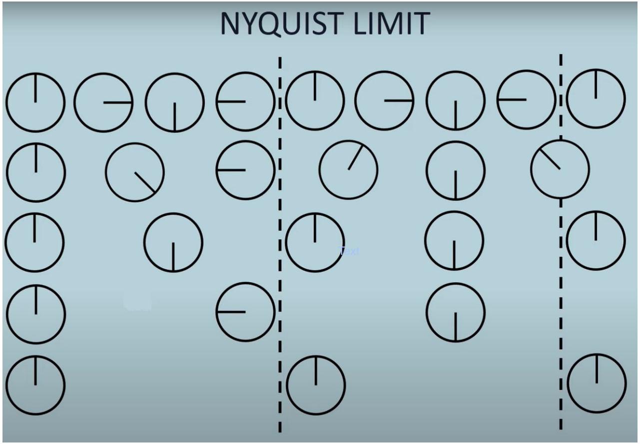
Angle dependency



small angle $\longrightarrow$ higher number of cycles Q

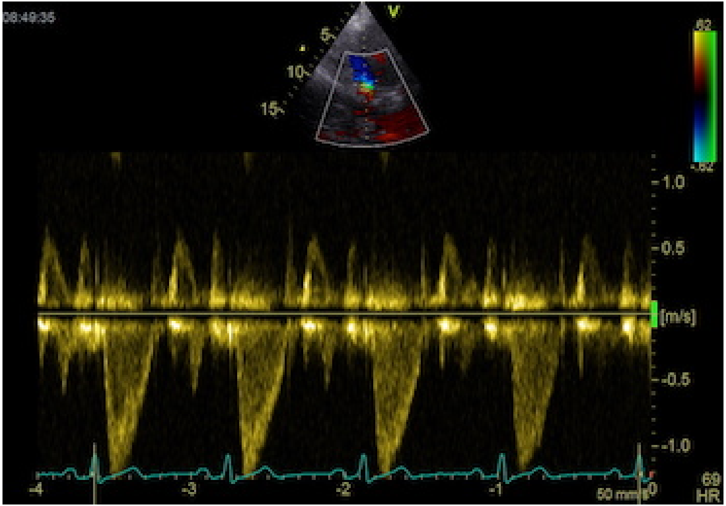
Aliasing (PRF too low)





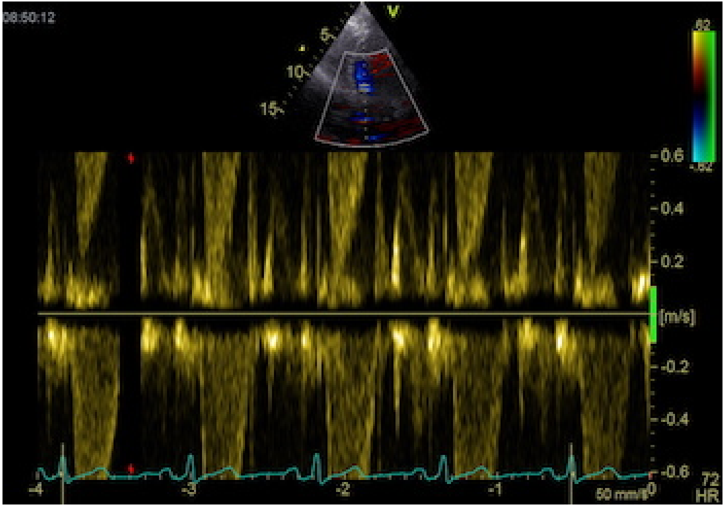
Nyquist $\longrightarrow$ $f_d < f_p/2$

Aliasing example



B-mode+Doppler+velocity spectrum — high PRF f_p

Aliasing example



B-mode+Doppler+velocity spectrum — low PRF f_p

Range-velocity tradeoff

$$f_d < f_p/2 \quad \longrightarrow \quad v_{\max} = \frac{f_p c}{4 f_s}$$

$$z_{\max} = \frac{T_p c}{2} = \frac{c}{2 f_p}$$

$$\boxed{v_{\max} z_{\max} = \frac{c^2}{8 f_s}}$$

Range-velocity tradeoff

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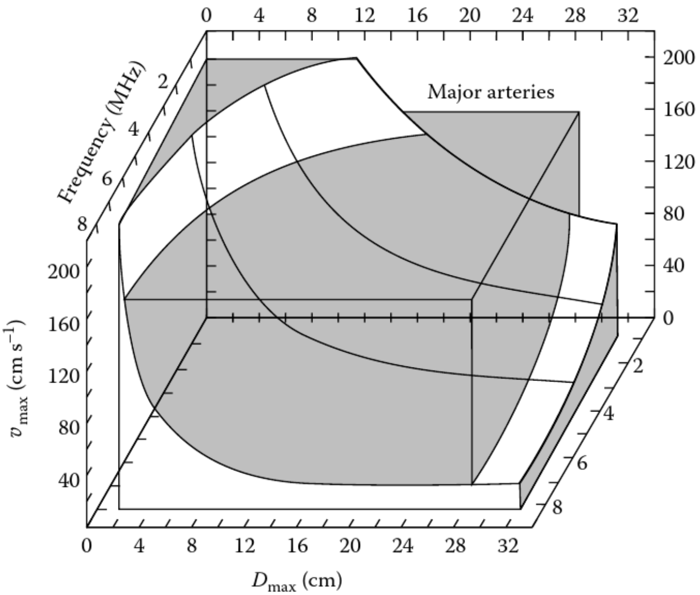
Limitation is for $(v \cos\theta)_{\max}$.

Range-velocity tradeoff



Minimum velocity

Observe at least one period of f_d

$$T_d < NT_p$$

with N transmissions per line

$$f_d > \frac{f_p}{N}$$
$$v_{\text{min}} = \frac{f_p c}{2Nf_s}$$

Minimum velocity

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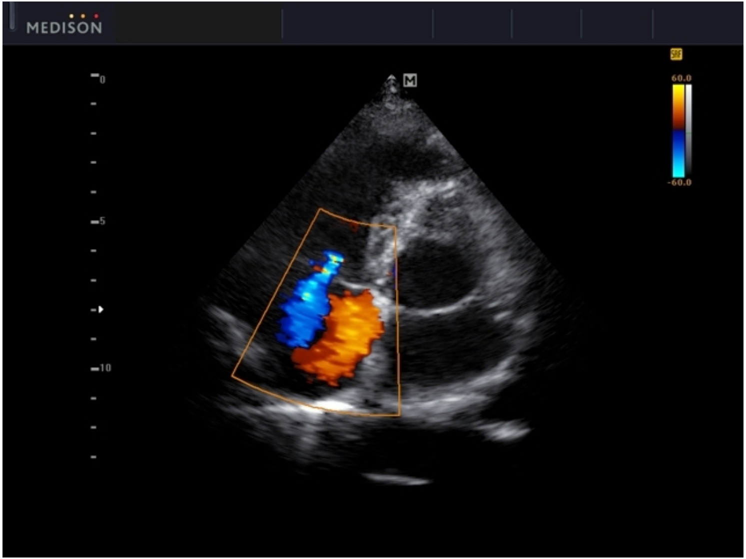
with N transmissions per line

$$f_d > \frac{f_p}{N}$$
$$v_{\min} = \frac{f_p c}{2Nf_s}$$

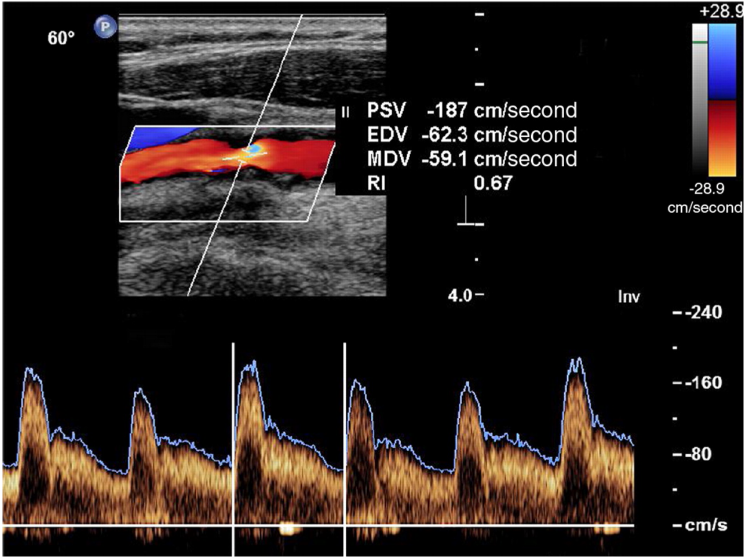
- Usually $2 \sim 3$ cycles required
- $N = 5 \sim 10$ or more
- Temporal averaging
- $\longrightarrow$ slow f_p

Doppler US — examples



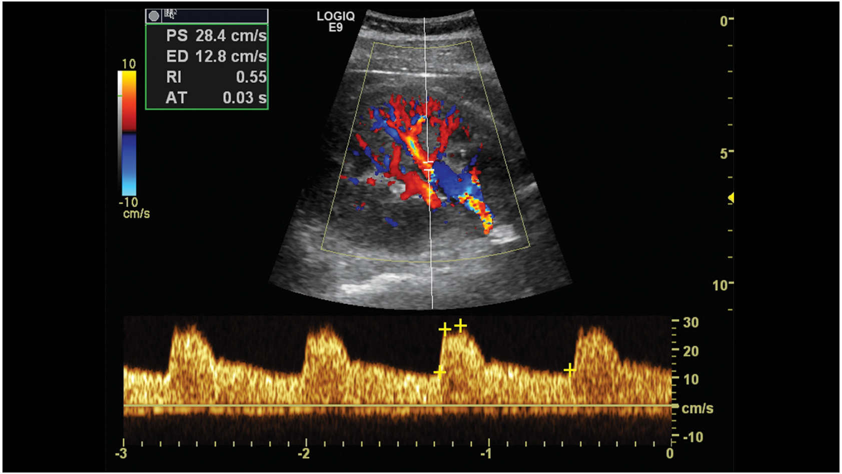
heart

Doppler US — examples



artery

Doppler US — examples



liver

Doppler ultrasound

US contrast agents

Harmonic imaging

3D US imaging

Contrast agents

- *1968, Gramiak, saline injection*
- Microbubbles ($2 \sim 5\,\mu$m)
- Asymmetric compression/expansion
- Stabilization (synthetic polymers), up to $5 - 10$ min.
- Injection
- Albunex, Optison, Echovist, Levovist...

Flash contrast imaging

US bubble destabilization.

normal

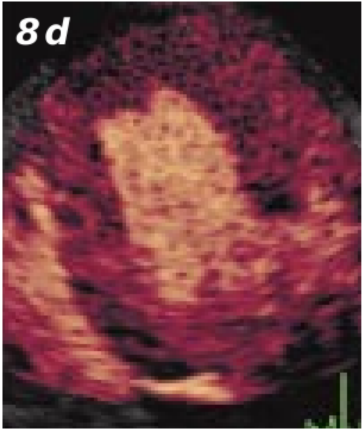
Flash contrast imaging

US bubble destabilization.

flash, bubbles broken

Flash contrast imaging

US bubble destabilization.



filling up

Myocardial perfusion evaluation.

Doppler ultrasound

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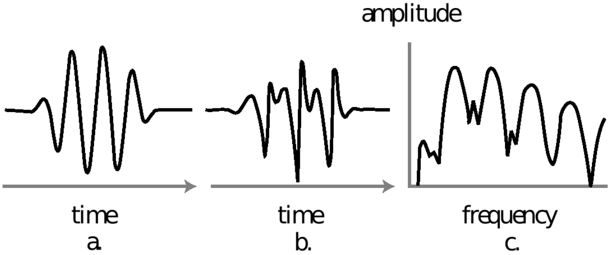
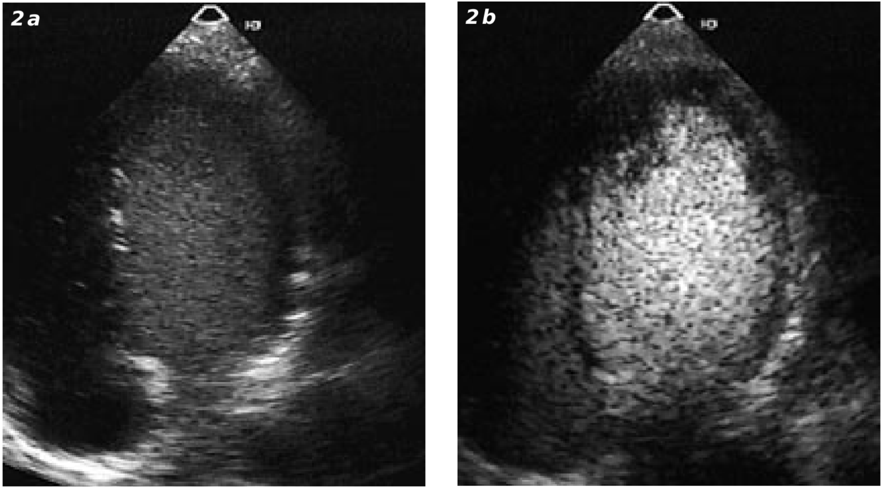
Nonlinear response

Assymetric bubble compression



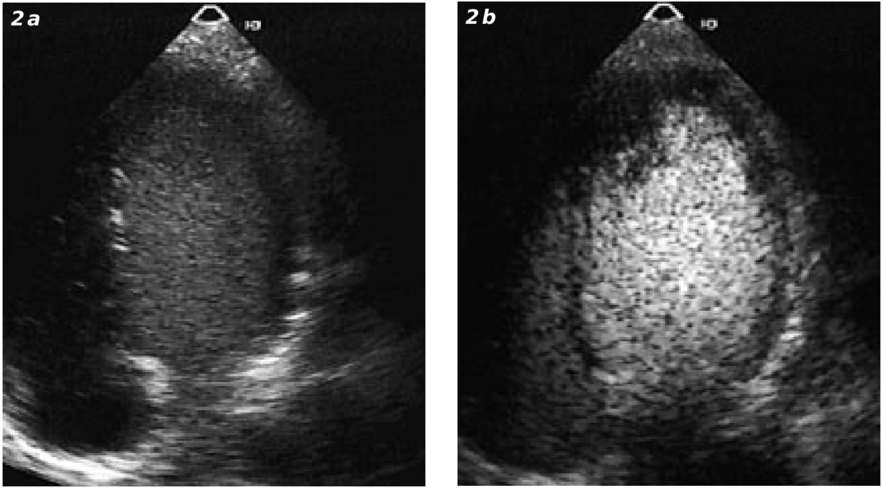
Harmonic imaging

- Transmit f_0, receive $2f_0$



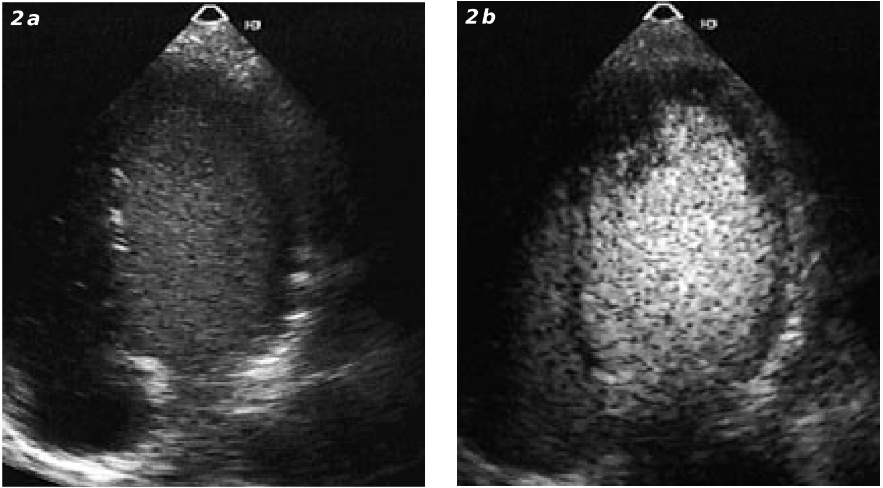
Harmonic imaging

- Transmit f_0, receive $2f_0$
- Bandwith limitation



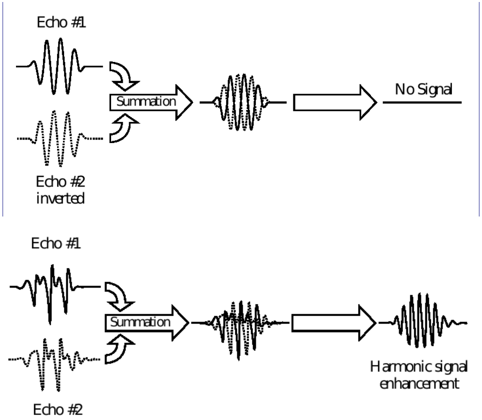
Harmonic imaging

- Transmit f_0, receive $2f_0$
- Bandwith limitation
- Bubbles not needed, tissue nonlinearity



Pulse Inversion Harmonic Imaging

- Two pulses, second inverted
- Responses summed
- Filtration not needed



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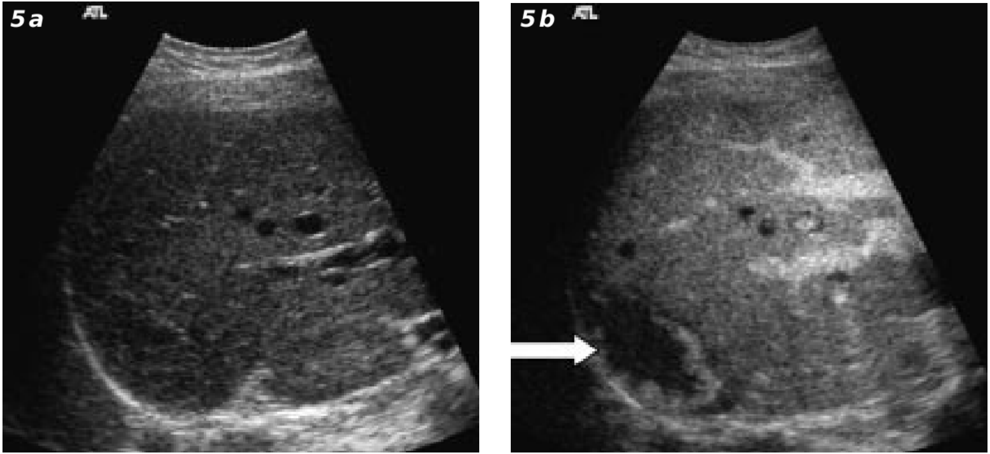
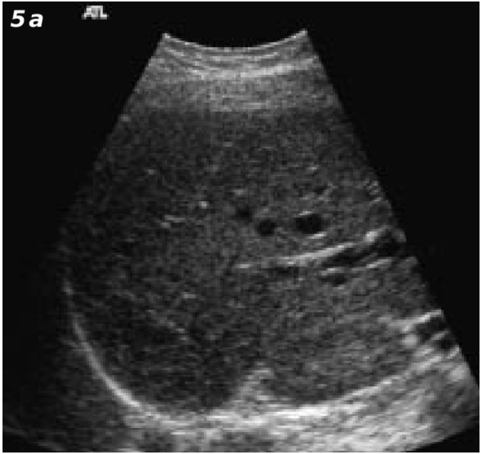
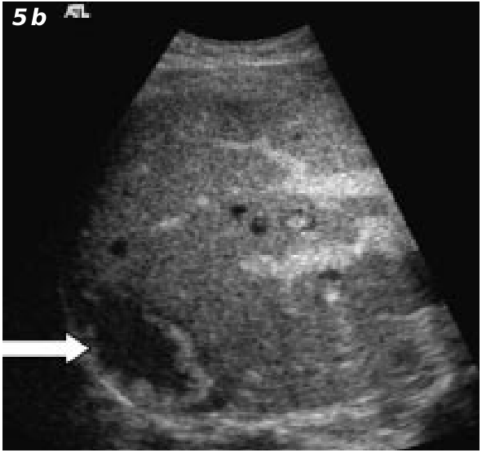


Pulse Inversion Harmonic Imaging

- Two pulses, second inverted
- Responses summed
- Filtration not needed
- Several pulses (Power Pulse Inversion)





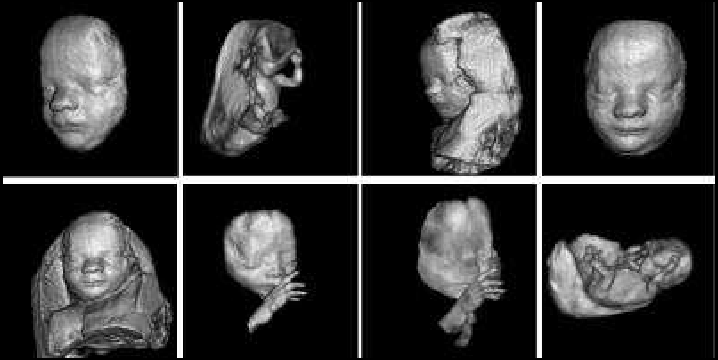
Doppler ultrasound

US contrast agents

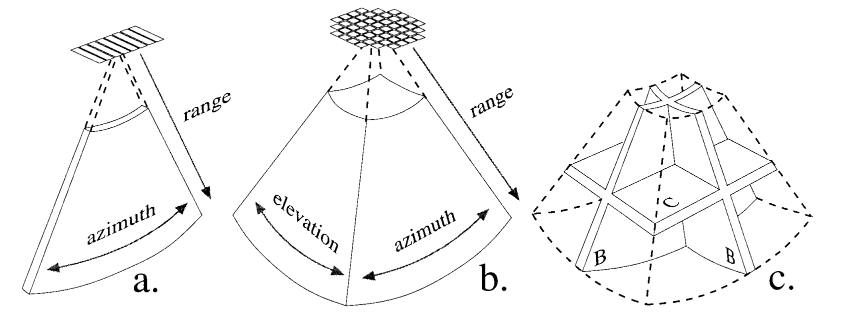
Harmonic imaging

3D US imaging

3D Reconstruction



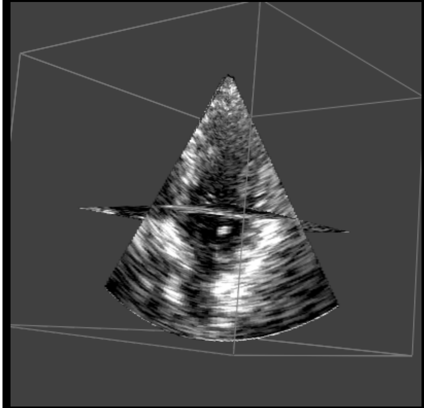
3D Ultrasound

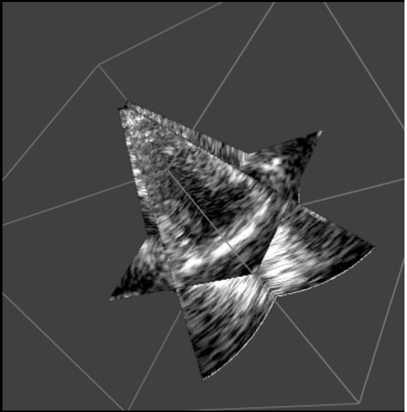


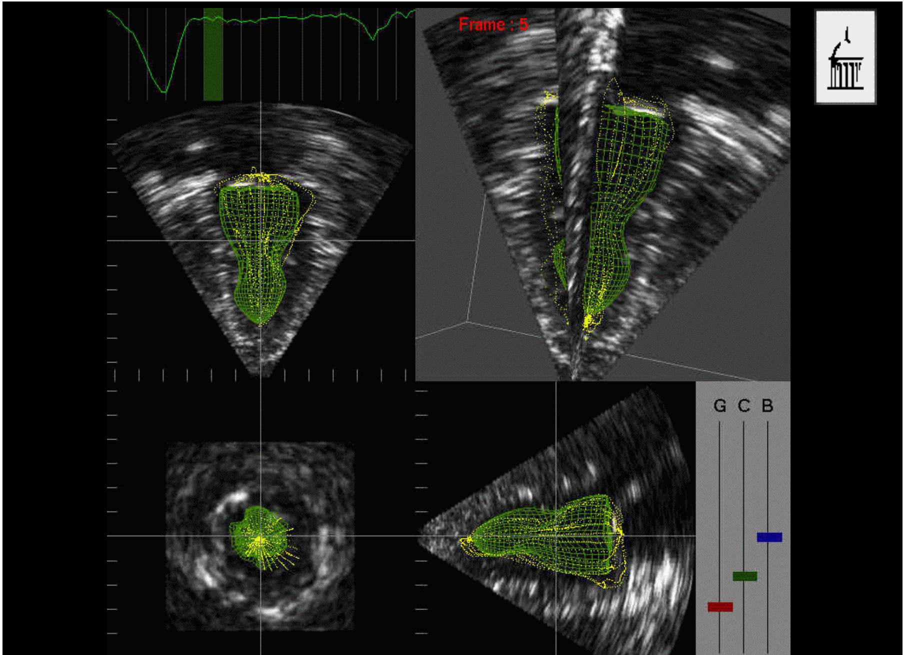
Traditional 2D

New 3D

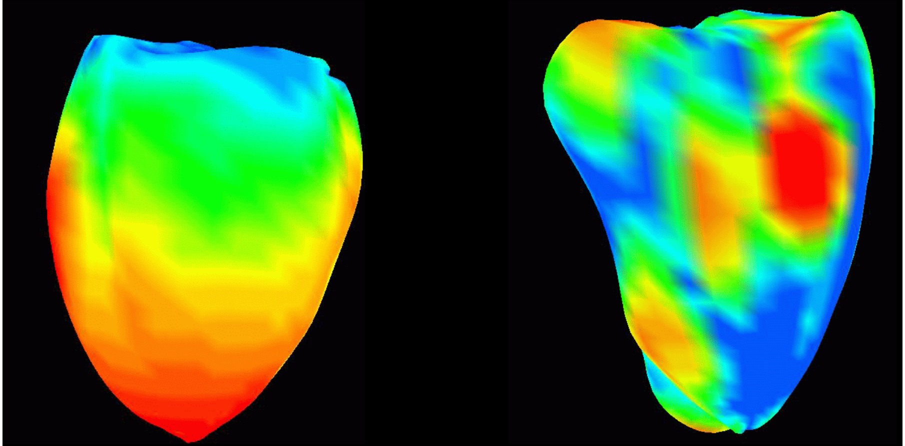
Real-time 3D Ultrasound






Frame : 5
G C B

Velocity of Contraction



Biological effects

- Thermal effects
  - 1.5 °C indefinitely or 6 °C for 1 min
  - highest risk in bones (transcranial imaging)
- Cavitation — growth/collapse of bubbles
  - for long pulse lengths or high pressure
  - may damage cells
  - unlikely to occur *in vivo*
- Radiation pressure — makes tissues/fluids move

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- Clinical studies found no harmful effects
- ... ultrasound power output is increasing.

Conclusions

- Non-invasive, affordable and portable imaging technique
- Excellent soft tissue imaging
- Lower image quality (wrt CT or MRI) due to speckle but improving
- Low penetration depth versus resolution
- Does not pass through air or gas
- Does not pass through bones, shadows
- Modern techniques — 3D, contract agents, Doppler