

Brain-computer interfaces

Jiří Hammer, PhD

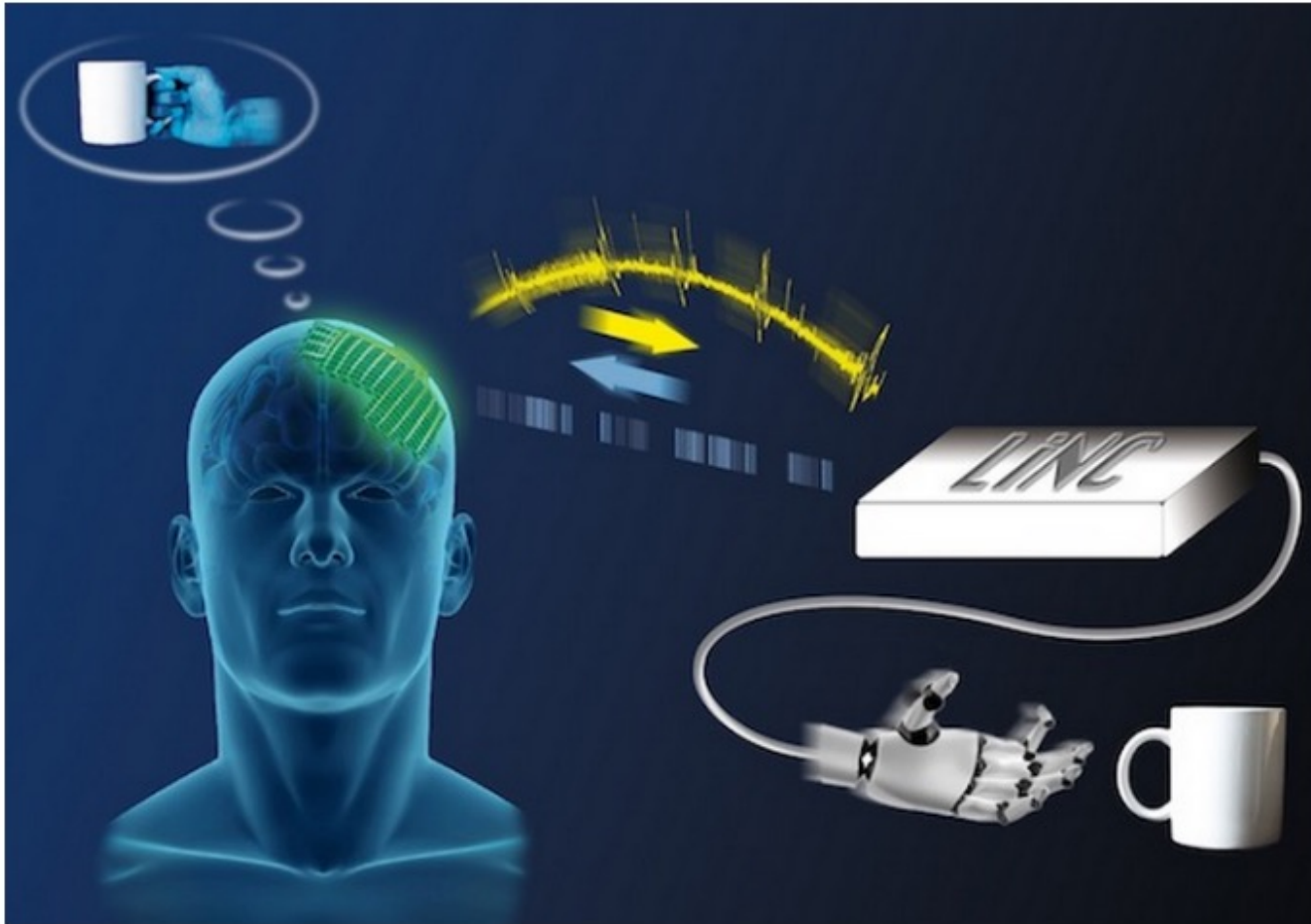
Neurologická klinika
2. LF UK

15.05.2024

Outline ...

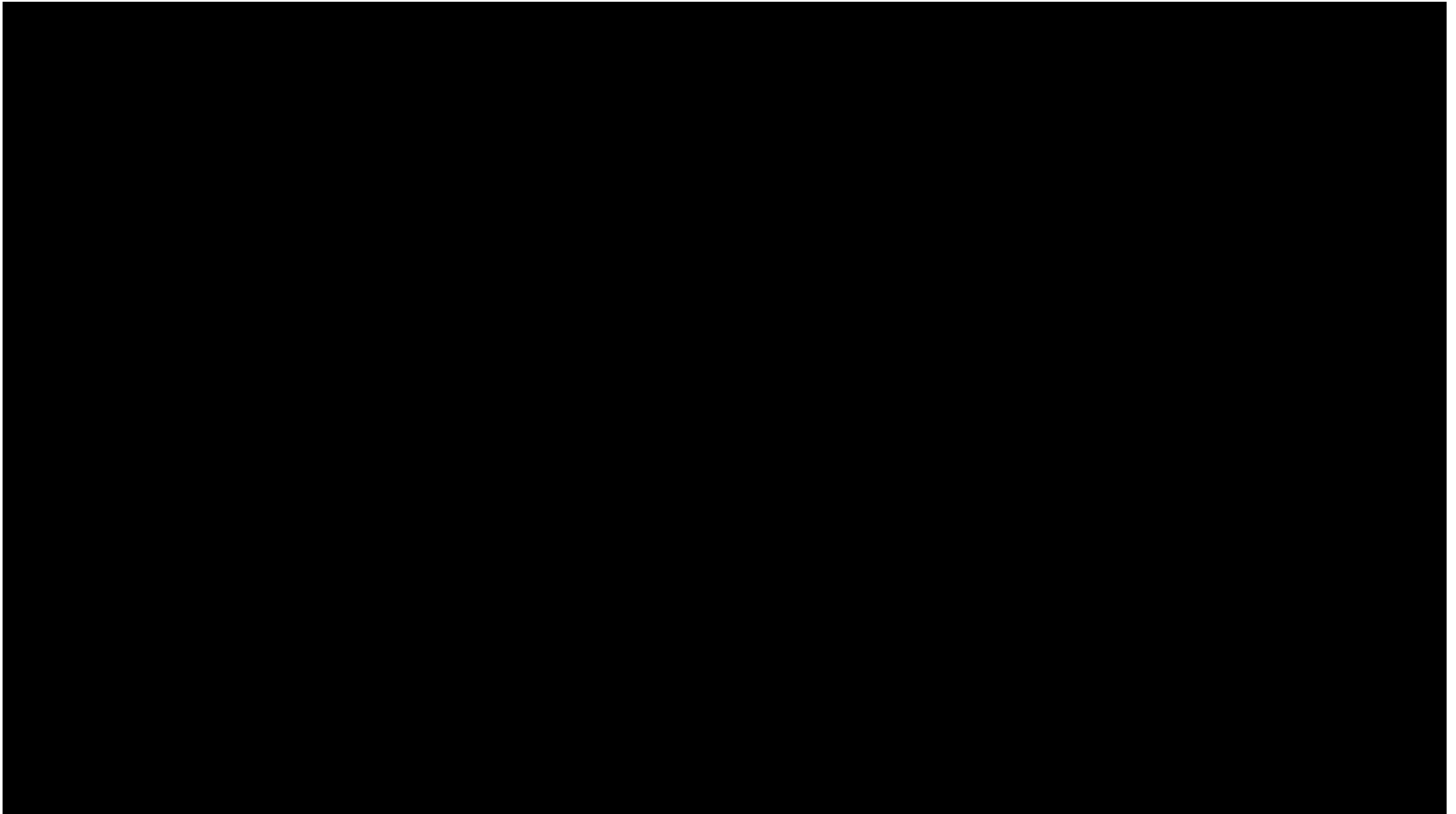
- What is a brain-machine interface (BMI) ?
- Examples of BMI
 - P300 (EEG)
 - SSVEP (EEG)
 - SCP (EEG)
 - MRP (EEG)
 - Biomimetic BMI (SUA)
- My own research
 - Biomimetic BMI (intracranial EEG)
 - Deep learning for BMI

What is brain-computer interface (BCI)?



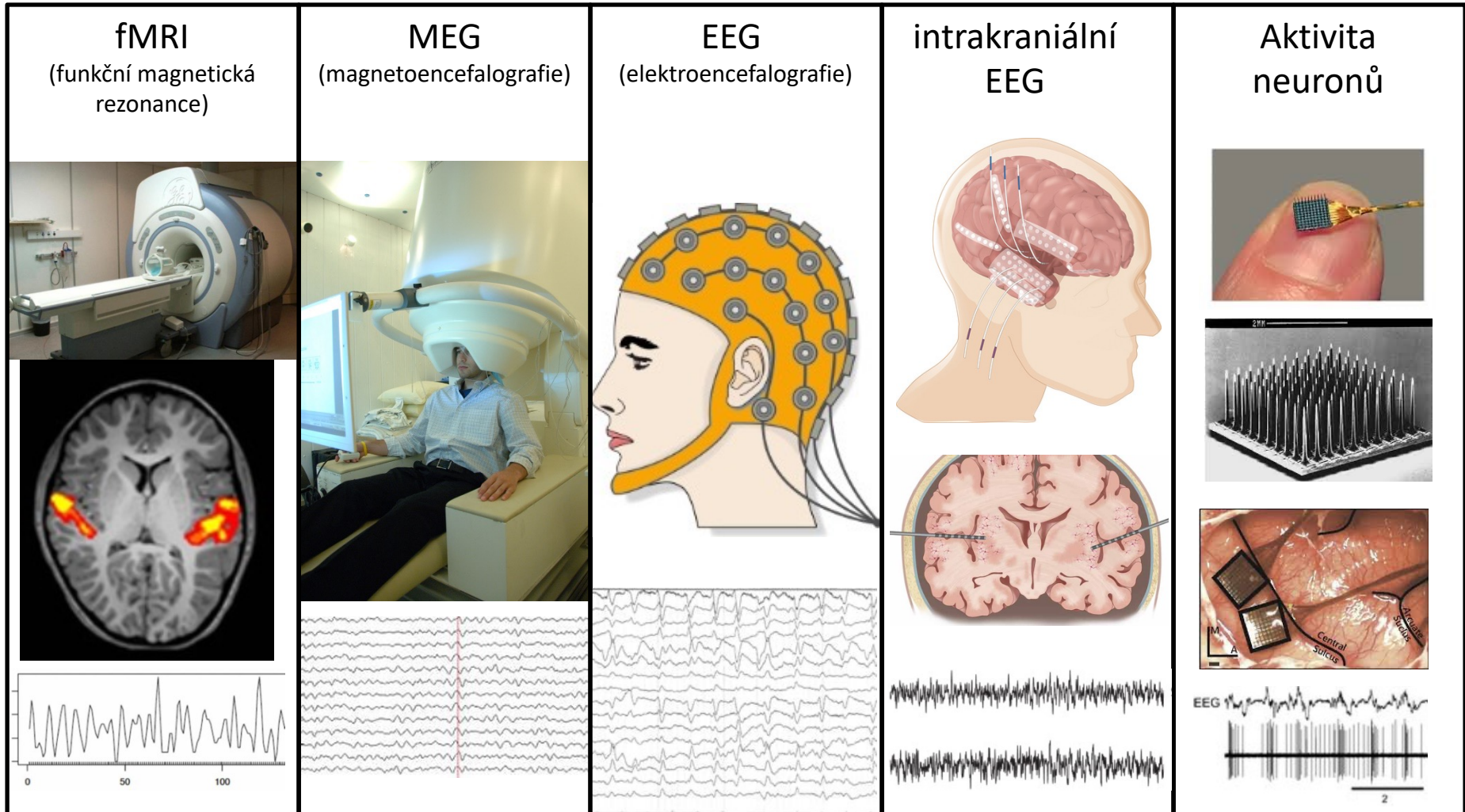
Brain-Computer Interface

Mysteries of the Brain

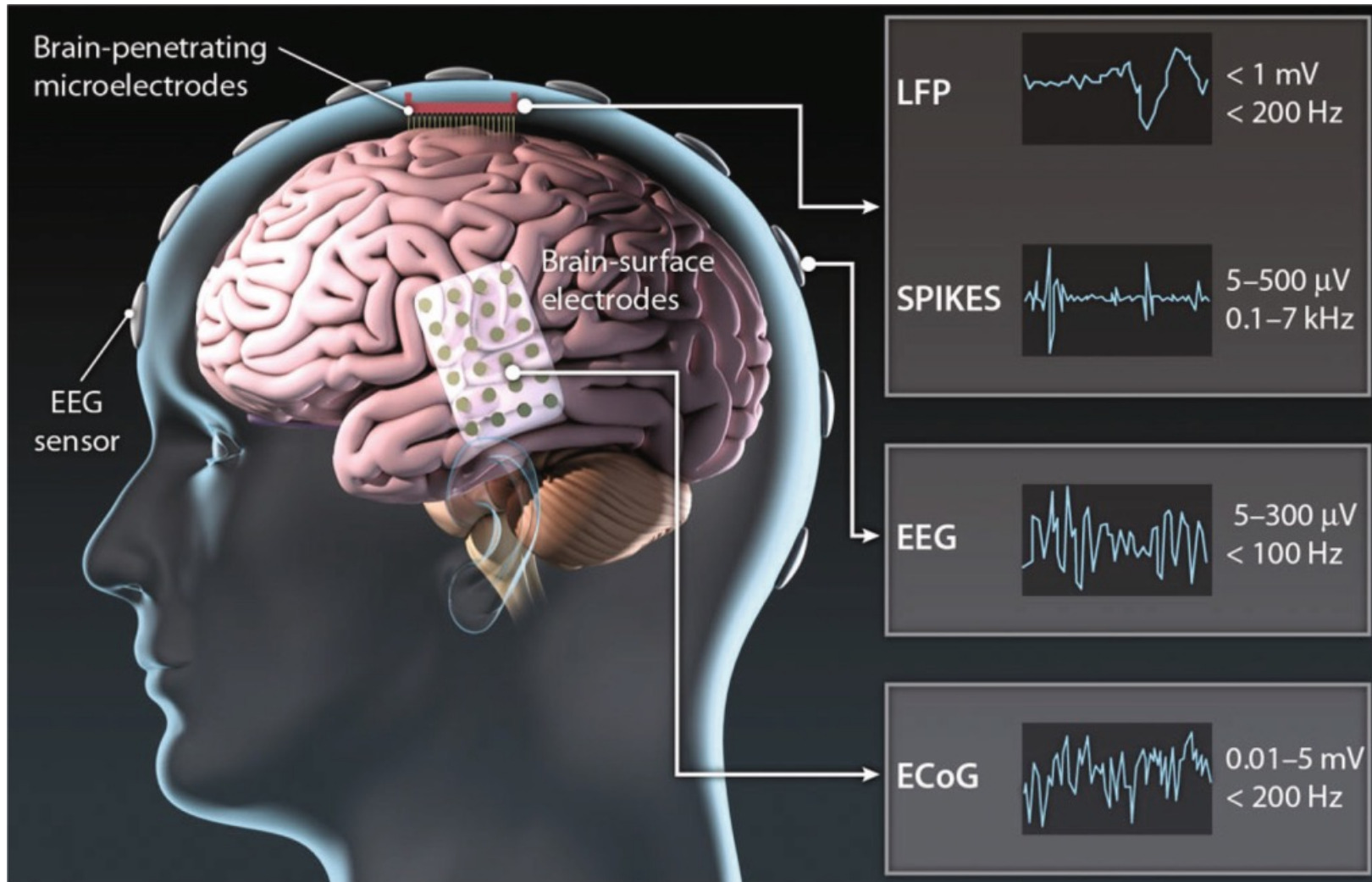


from YouTube

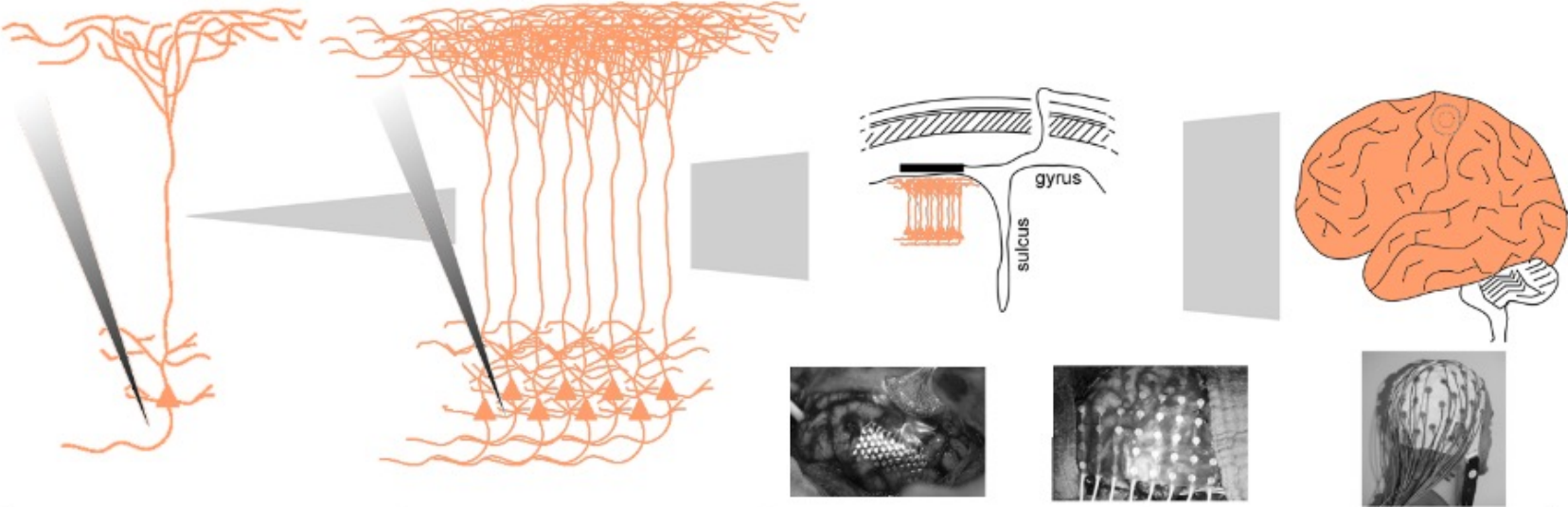
Overview of most common brain signals



Electrophysiological brain signals



Electrophysiological brain signals

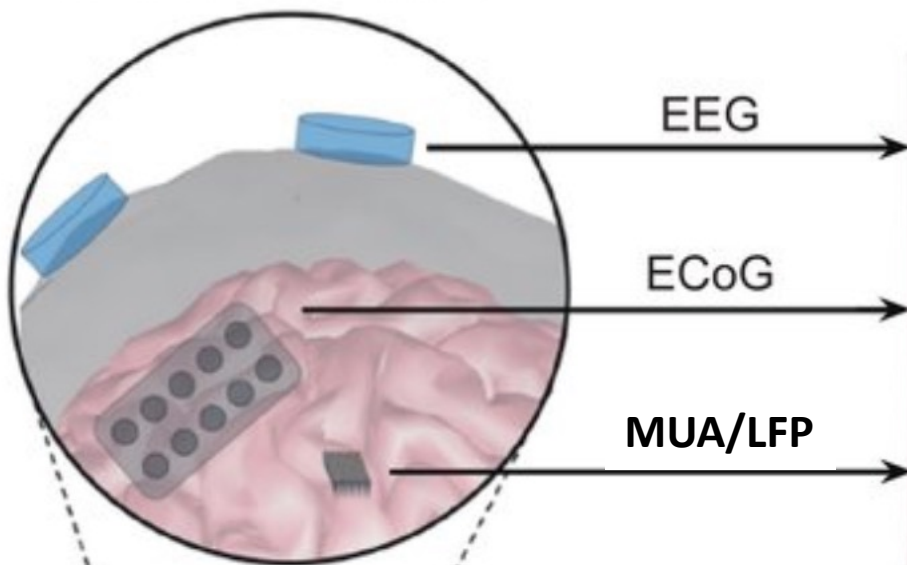


SUA / MUA	LFP	μ ECoG	ECoG	EEG
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1 ← size of neuronal cluster → >100.000
 high ← spatial resolution → low
 invasive ← → non-invasive

1.

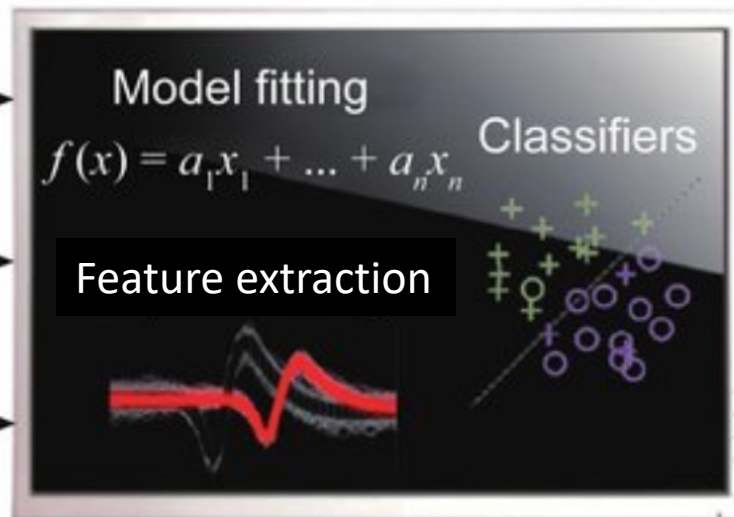
Record neural signals



2.

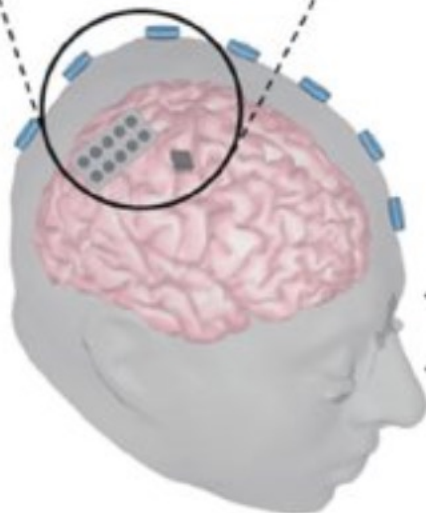
Decode mental intent

Feature extraction + Decoding



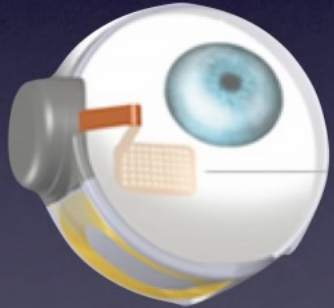
3.

Device control



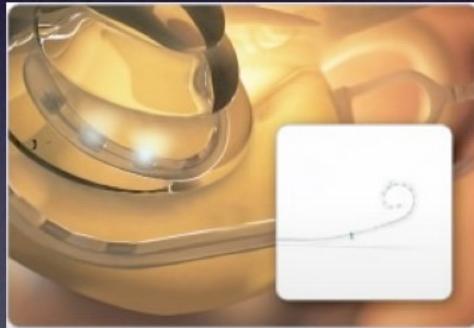
Visual feedback

Retinal implant



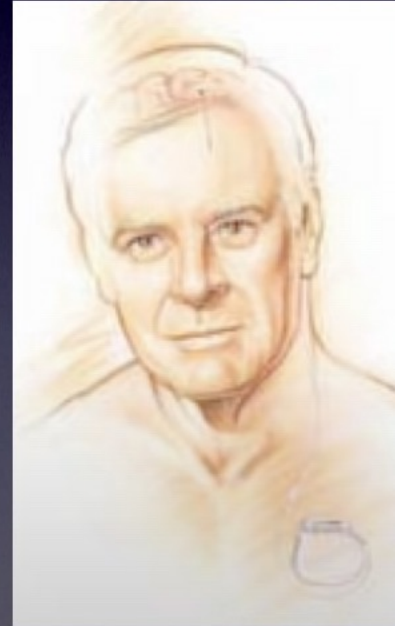
Second Sight

Cochlear implant



Advanced Bionics

Parkinsons implant



Medtronic

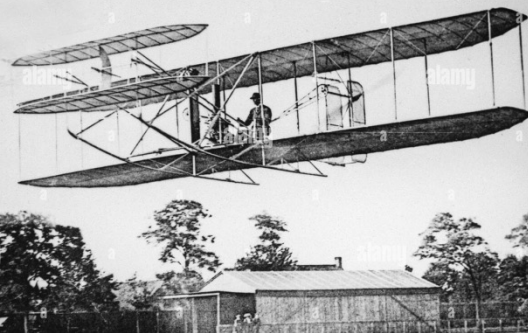
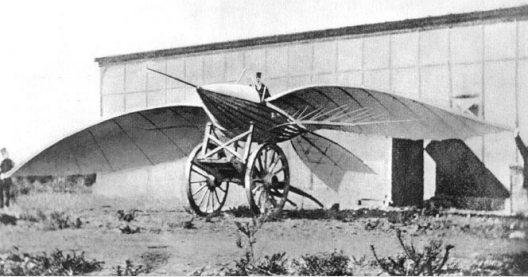
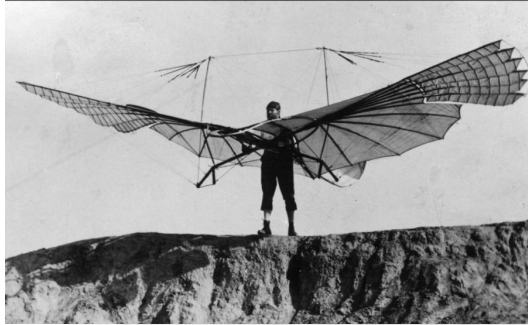
Epilepsy implant



Neuropace

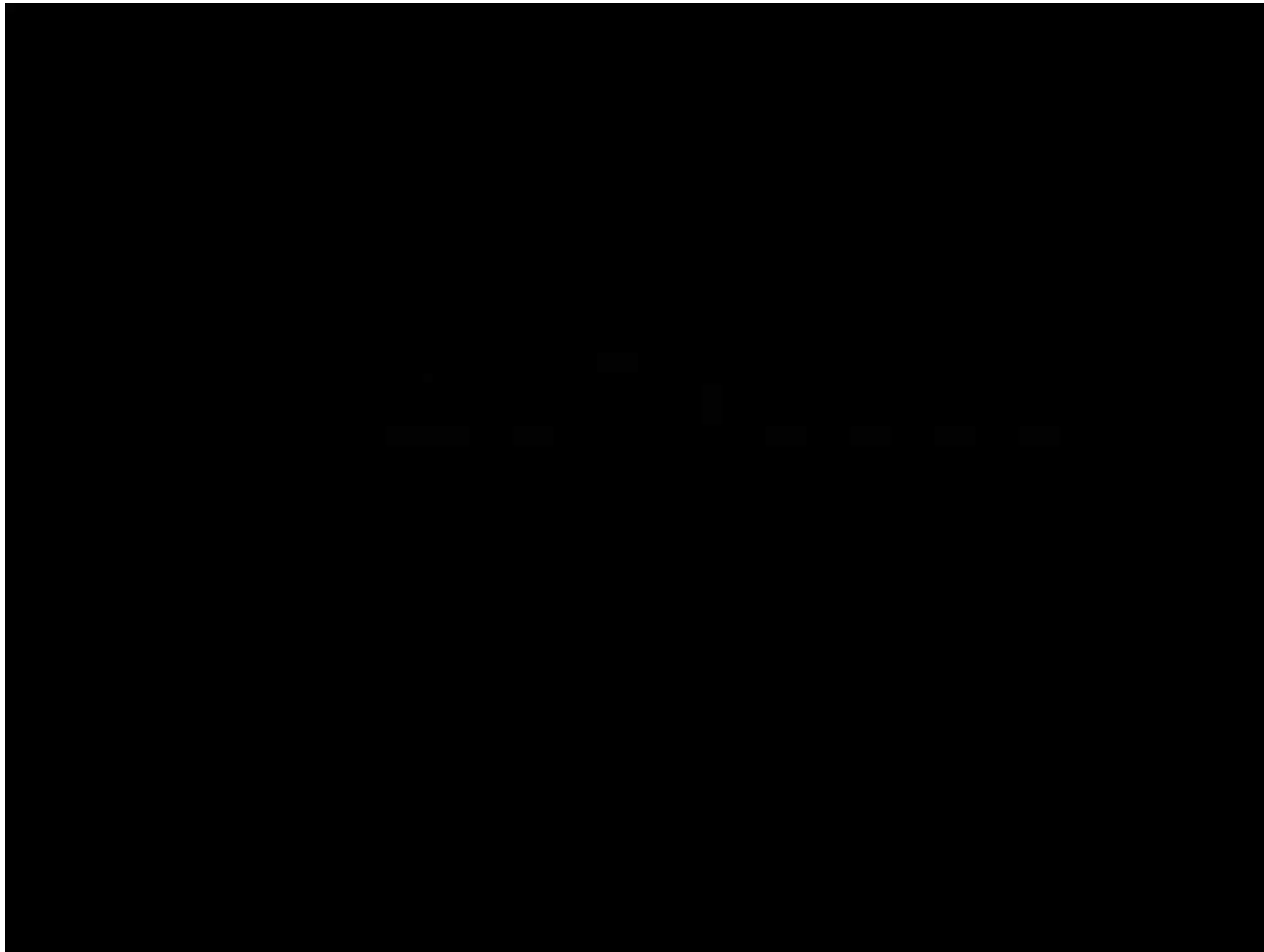
BCI examples

Brain-Computer Interface (BCI): we are at the beginning ...



P300 (EEG) speller: example

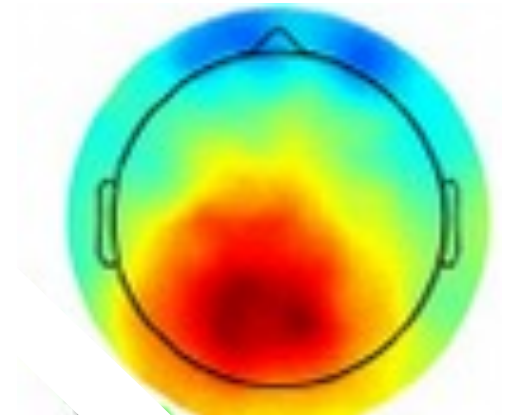
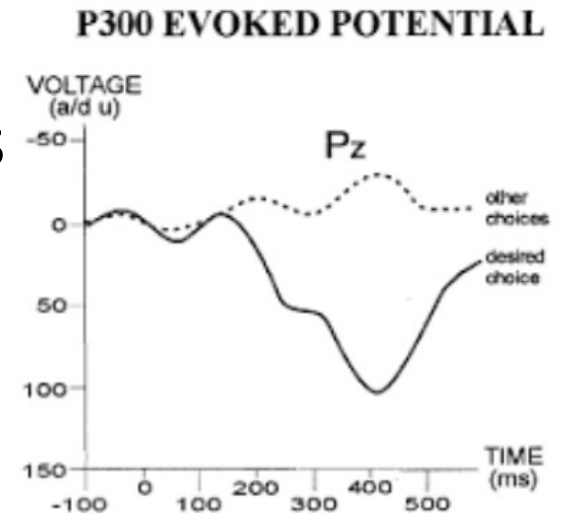
(positivity of EEG potential 300 ms after rare/unexpected stimulus)



P300 (EEG) speller: principle

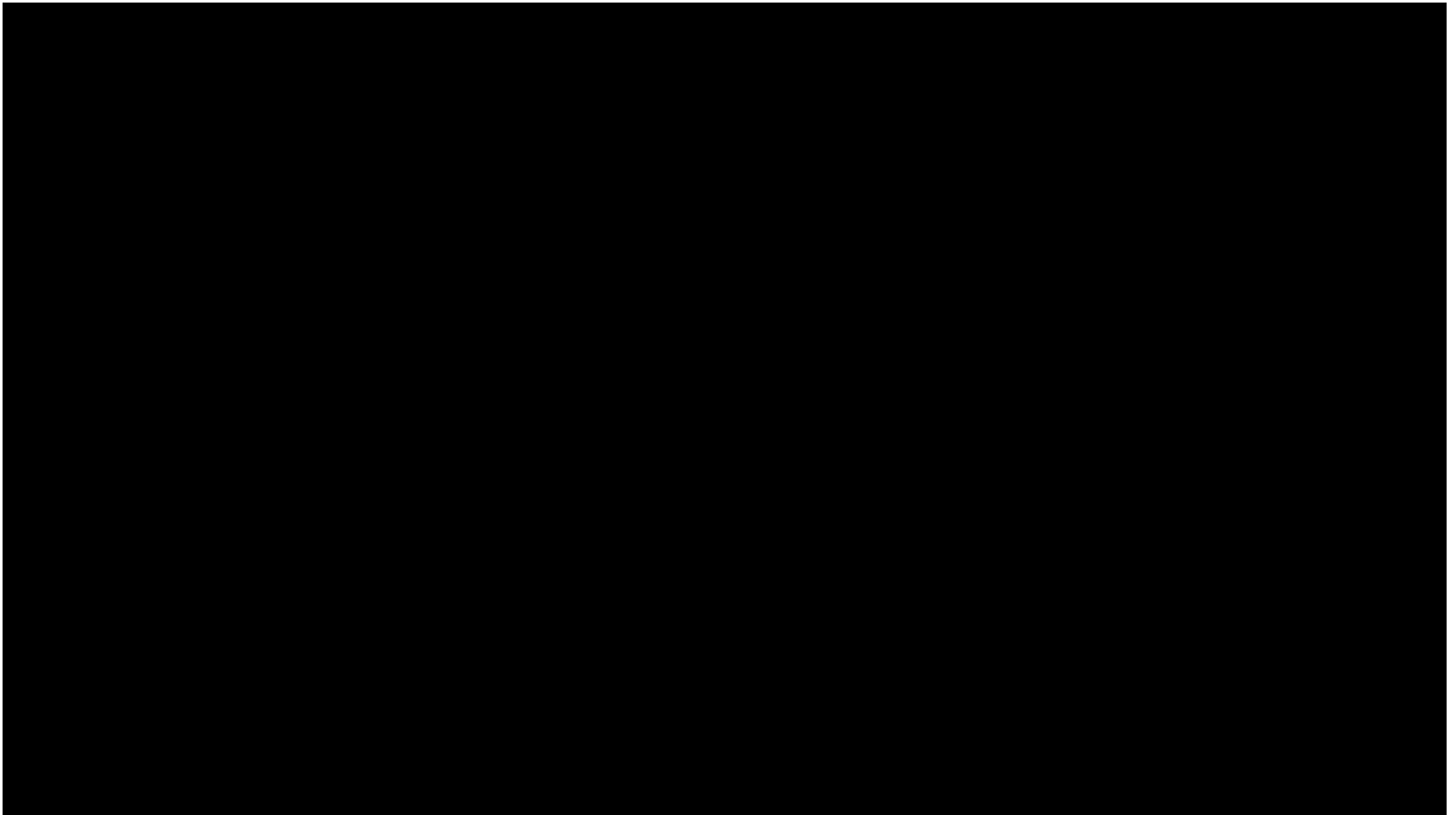
(positivity of EEG potential 300 ms after rare/unexpected stimulus)

- P300 component of EEG
- Discovered in the 60s
- Low probability (surprise) stimulus
- „oddball“ paradigm
- Pronounced peak
 - positivity
 - latency: 250 - 500 ms
- Parietal area of the brain
- Applications: P300 speller
 - speed cca 10 letters/min



SSVEP (EEG) BMI: example 1

(SSVEP, steady state visual evoked potential)



SSVEP (EEG) BMI: example 2

(SSVEP, steady state visual evoked potential)

A Lower Limb Exoskeleton Control Based on Steady State Visual Evoked Potential

No-Sang Kwak, Klaus-Robert Müller and Seong-Whan Lee

Department of Brain and Cognitive Engineering, Korea University

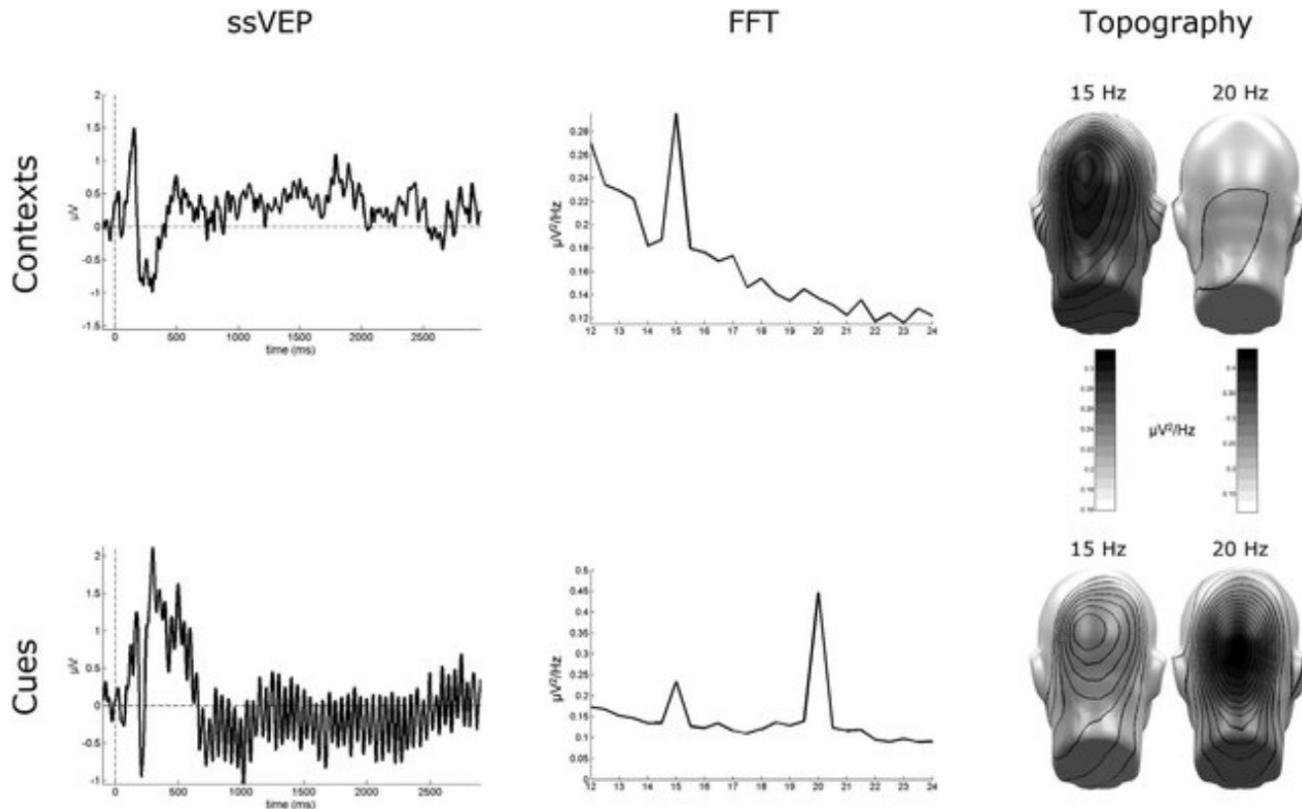


Pattern Recognition Laboratory

SSVEP (EEG) BMI: principle

(SSVEP, steady state visual evoked potential)

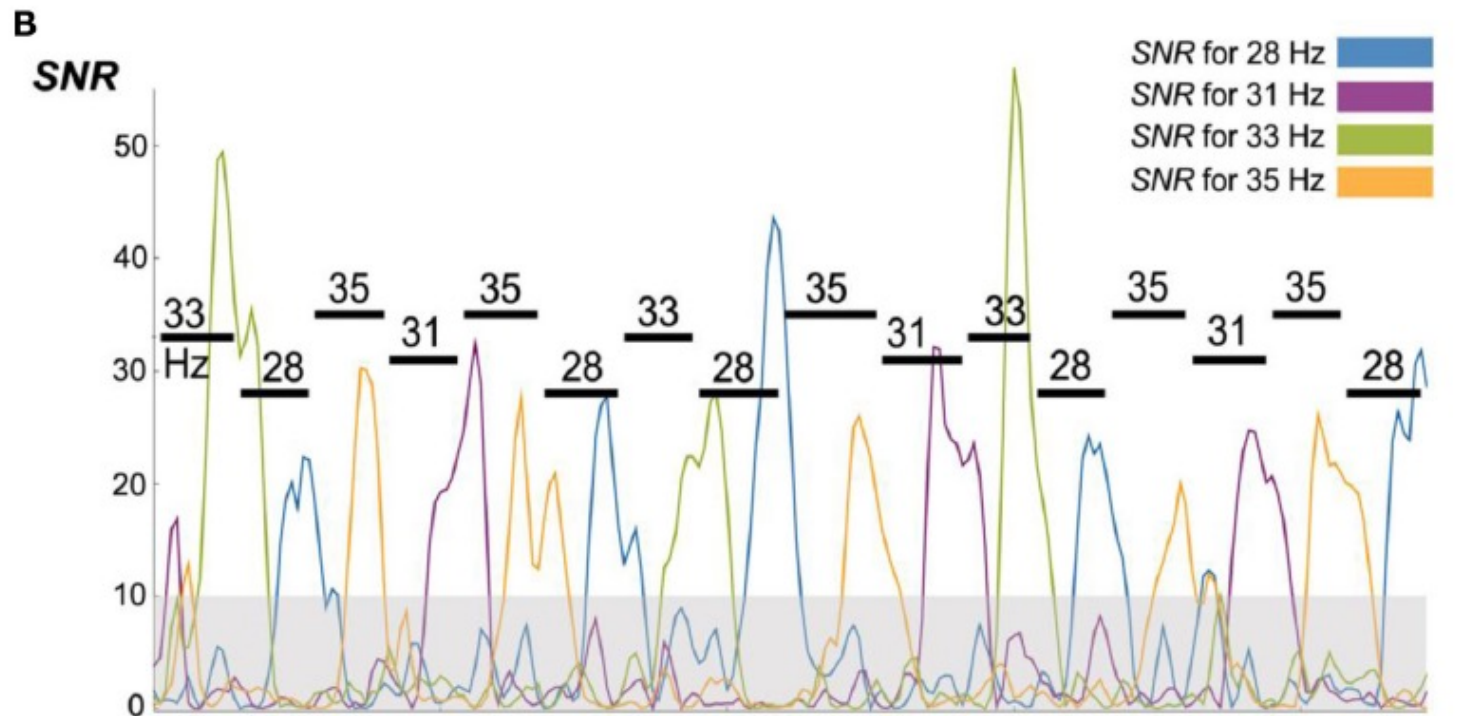
- Voluntary choice of focus on stimulus
- Stimuli flickering at different frequencies
- Signal = „resonant frequency“ in visual cortex



SSVEP (EEG) BMI: principle

(SSVEP, steady state visual evoked potential)

- Voluntary choice of focus on stimulus
- Stimuli flickering at different frequencies
- Signal = „resonant frequency“ in visual cortex



SCP (EEG) BMI

(SCP, slow cortical potentials)

LIEBER-HERR-BIRBAUMER-

HOFFENTLICH-KOMMEN-SIE-MICH-BESUCHEN,-WENN-DIESER-BRIEF-SIE-ERREICHT-HAT-.ICH-DANKE-IHNEN-UND-IHREM-TEAM-UND-BESONDERS-FRAU-KÜBLER-SEHR-HERZLICH,-DENN-SIE-ALLE-HABEN-MICH-ZUM-ABC-SCHÜTZEN-GEMACHT,-DER-OFT-DIE-RICHTIGEN-BUCHSTABEN-TRIFFT.FRAU-KÜBLER-IST-EINE-MOTIVATIONSKÜNSTLERIN.OHNE-SIE-WÄRE-DIESER-BRIEF-NICHT-ZUSTANDE-GEKOMMEN.-ER-MUSS-GEFEIERT-WERDEN.-DAZU-MÖCHTE-ICH-SIE-UND-IHR-TEAM-HERZLICH-EINLADEN-.EINE-GELEGENHEIT-FINDET-SICH-HOFFENTLICH-BALD.

MIT-BESTEN-GRÜSSEN-
IHR-HANS-PETER-SALZMANN



Movement-related spatial patterns, EEG BMI: example 1

(ERS / ERD, event related synchronization / desynchronization)

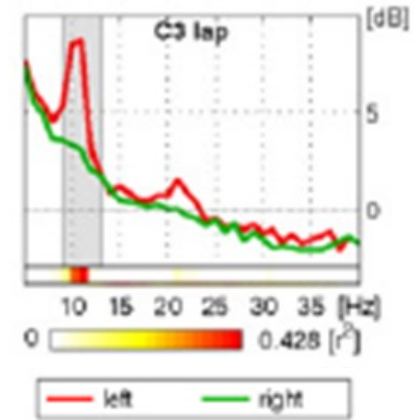
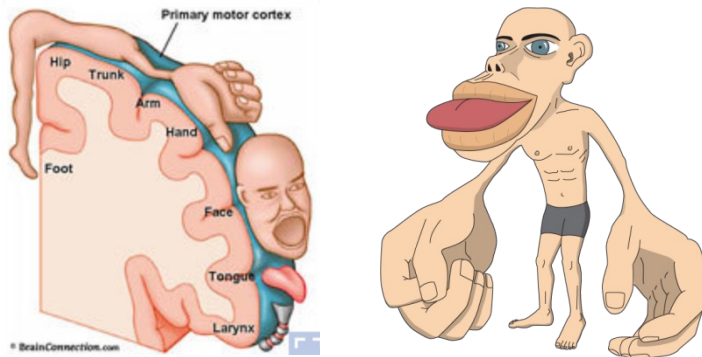


Movement-related spatial patterns, EEG BMI: example 2

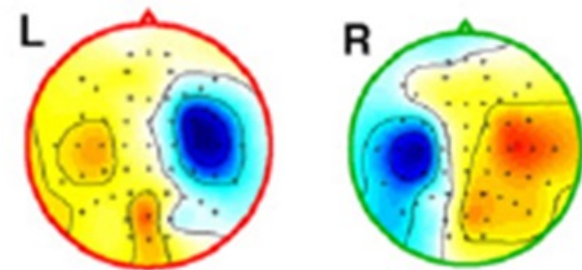
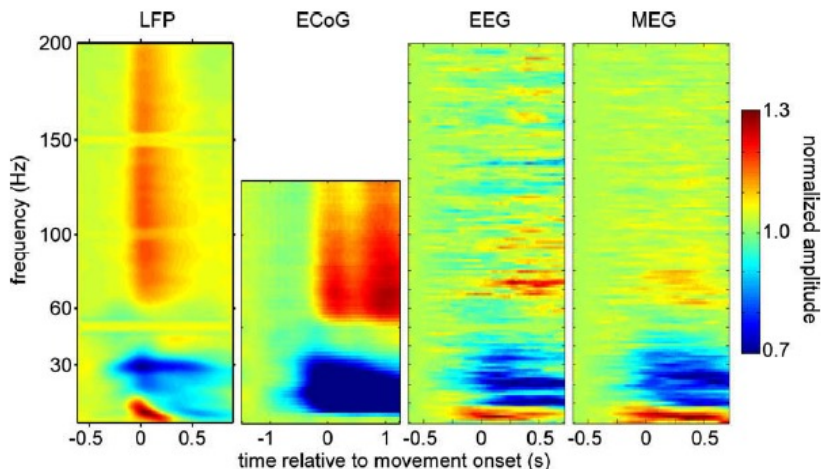


Movement-related spatial patterns, EEG BMI: principle

(ERS / ERD, event related synchronization / desynchronization)



Reprezentace těla v mozku: homunkulus



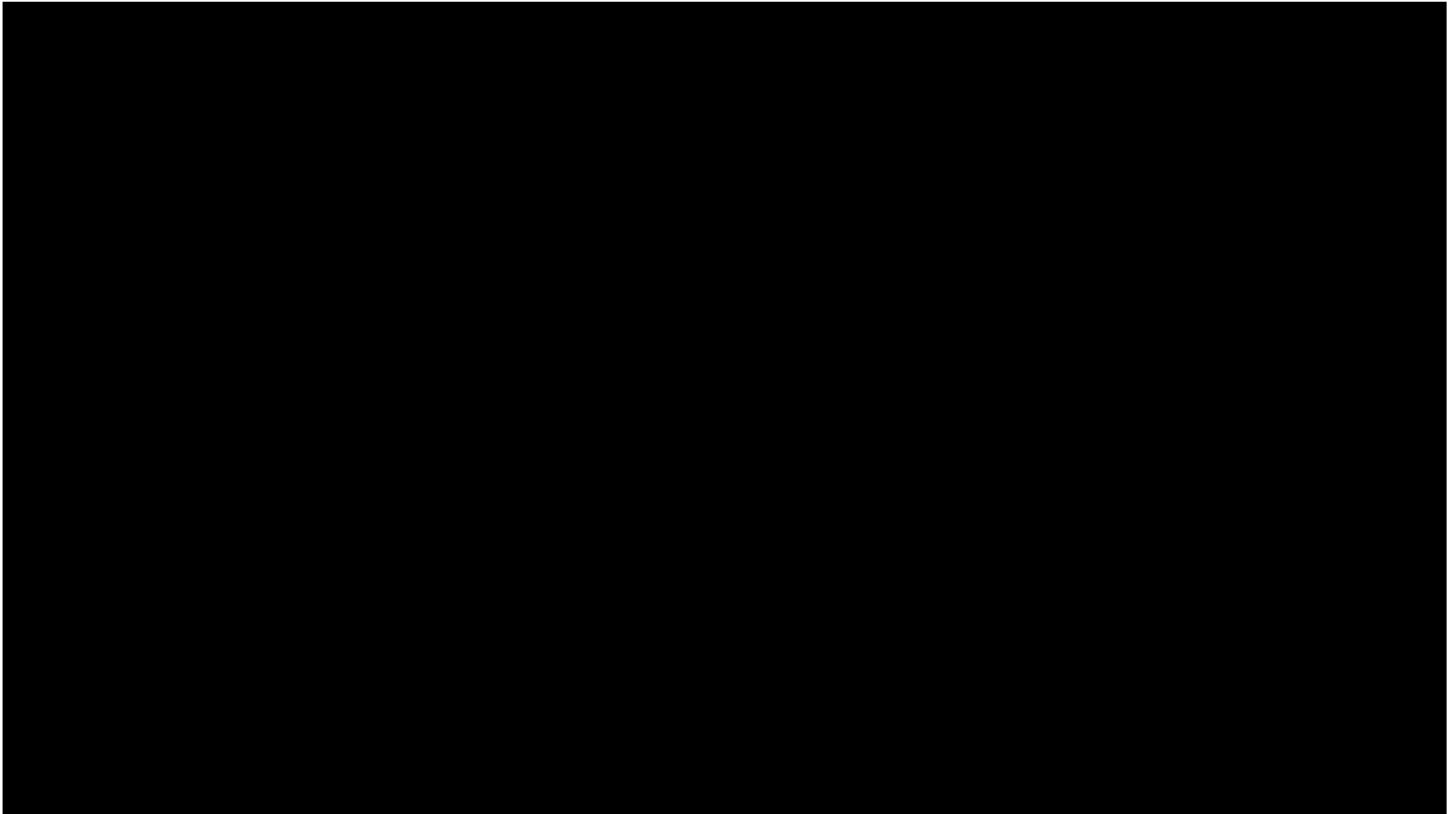
Blankertz et al. (2007) NeuroImage

Waldert et al. (2009) J Neurophysiol Paris

Biomimetic BMI (single neurons): example 1



Biomimetic BMI (single neurons): example 2

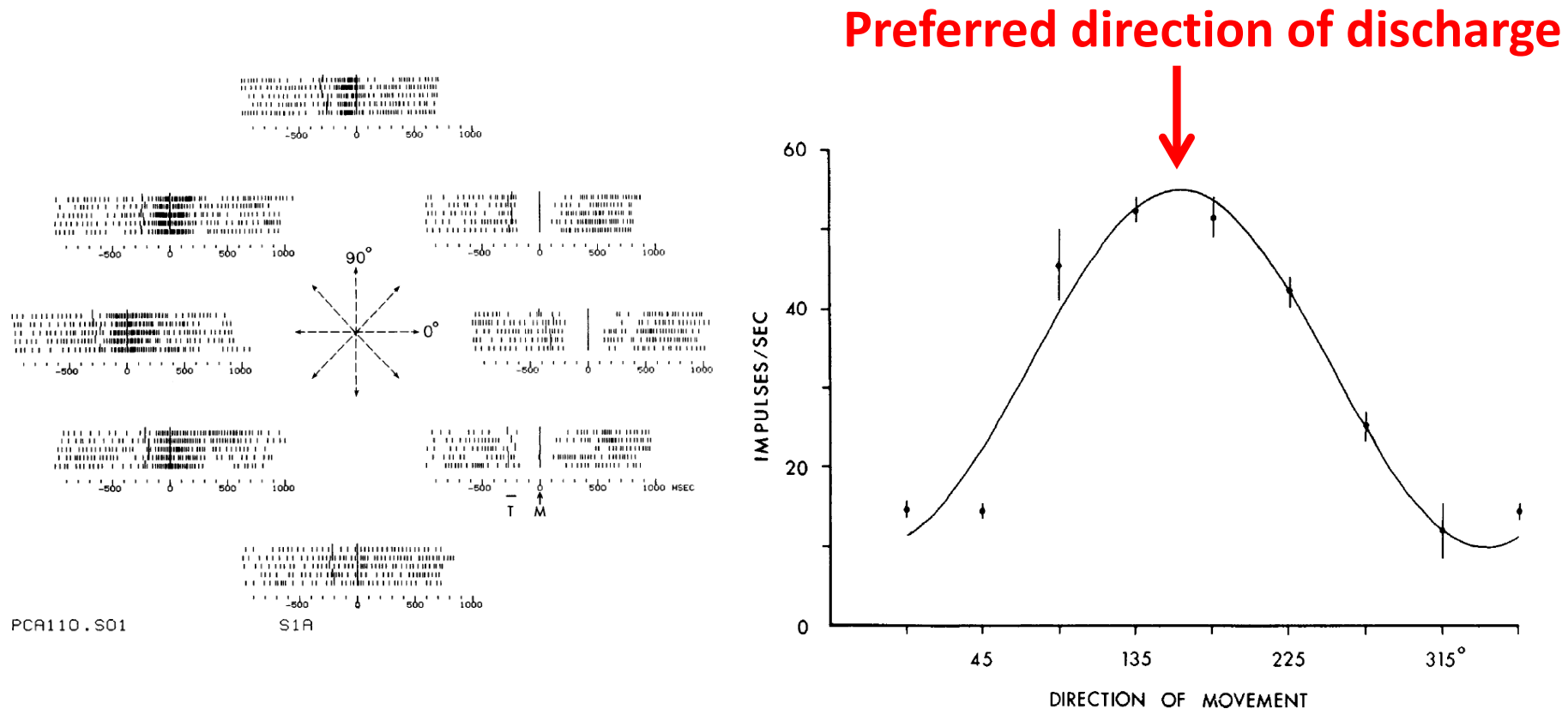


Biomimetic BMI (single neurons): example 3



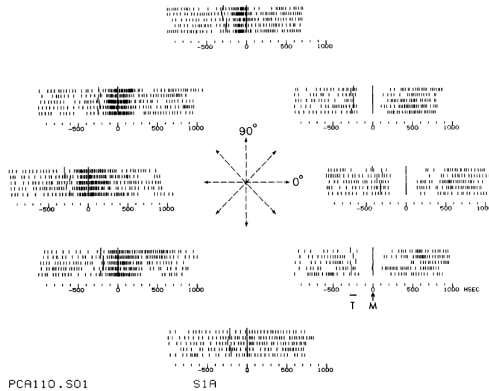
Biomimetic BMI (single neurons): principle

Directional „cosine tuning“ of motor cortex neurons

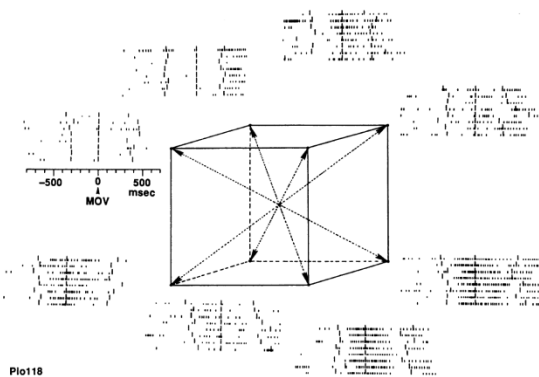


Biomimetic BMI (single neurons): principle

Decoding model for movement direction
= sum of neuronal population along preferred directions



Georgopoulos et al. (1982) J Neurosci

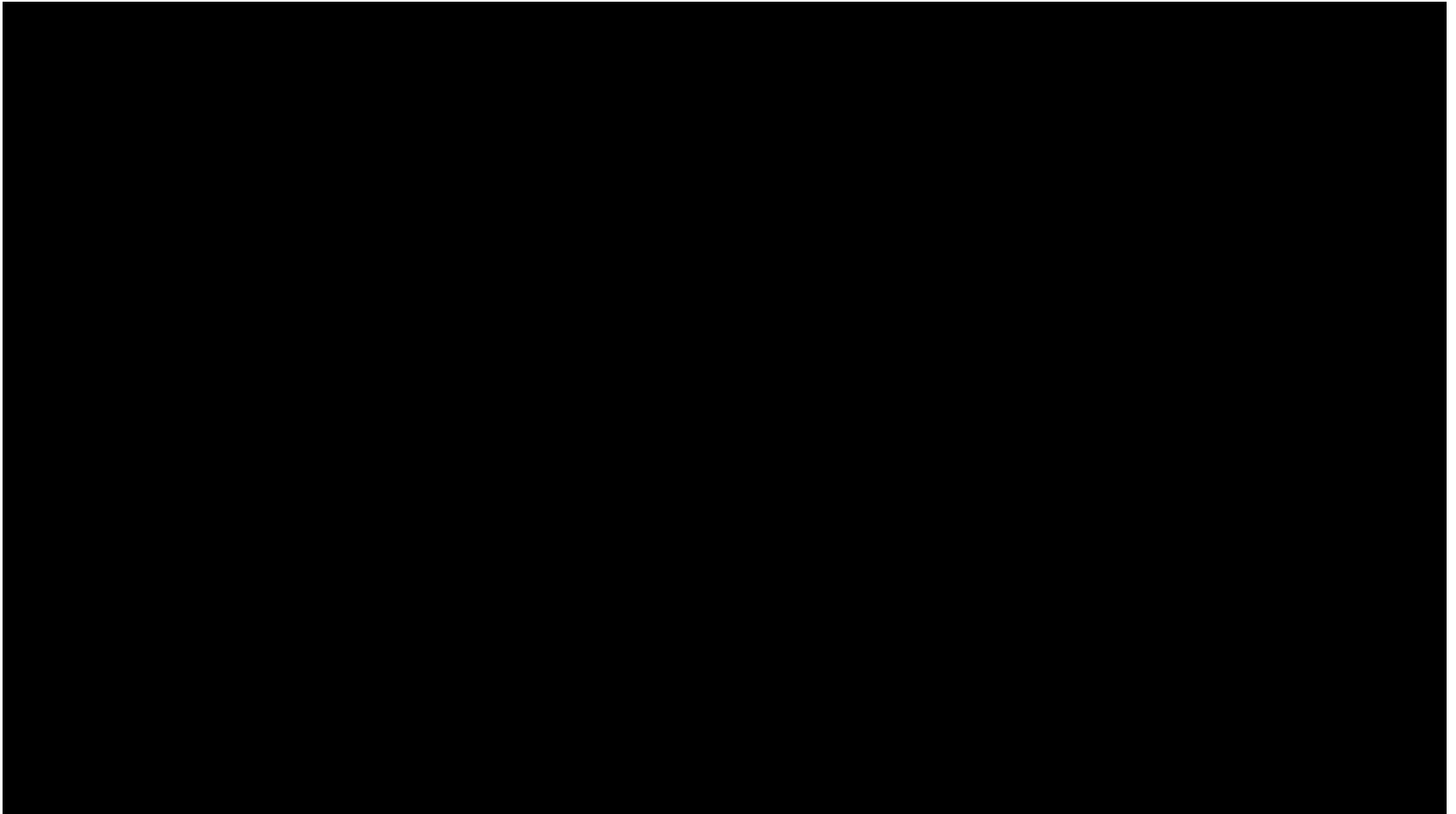


Georgopoulos et al. (1986) Science

$$P(M) = \sum_{n=1}^N r_n(M) \Phi_n$$

- P ~ predicted movement direction
- M ~ intended movement direction
- r_n ~ discharge of n -th neuron
- Φ_n ~ preferred direction of n -th neuron
- N ~ number of neurons

BMI (single neurons): with sense of touch – example 1



BMI (single neurons): with sense of touch – example 2

ARAT

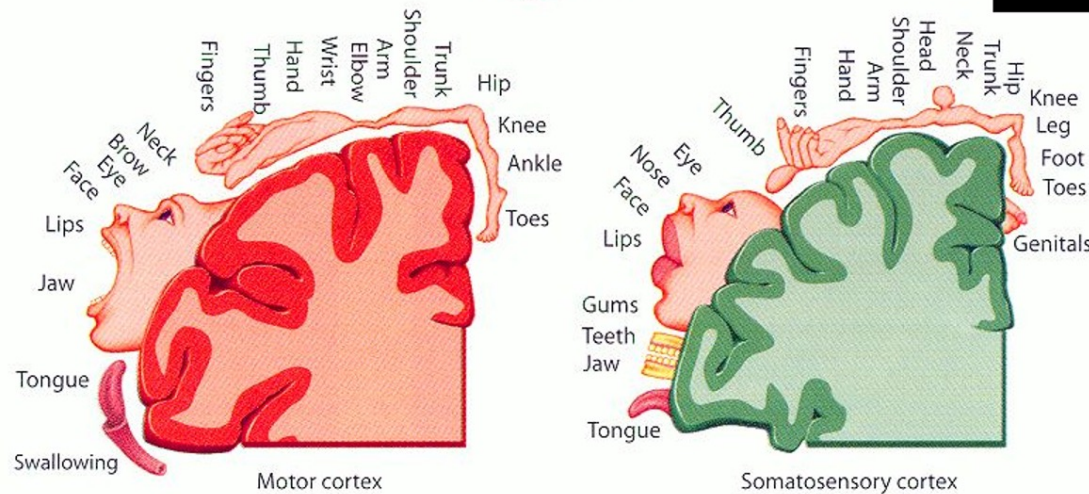
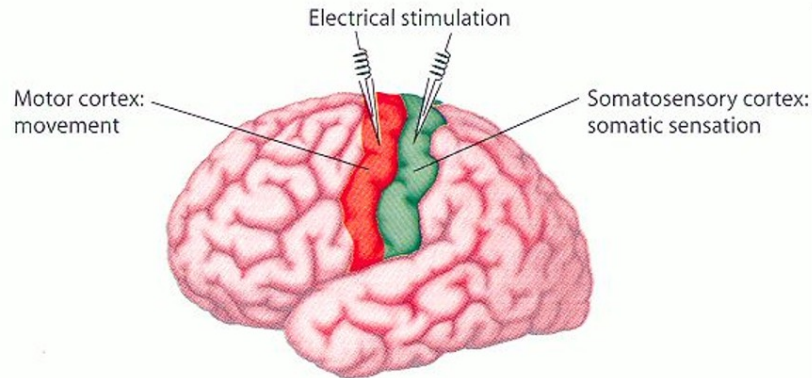
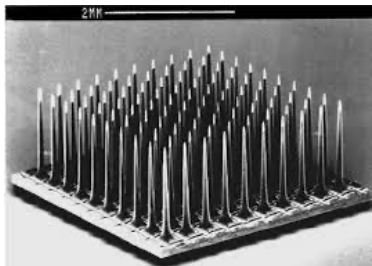
Fastest trial comparison for each object with and without ICMS feedback

University of Pittsburgh

BMI (single neurons): with sense of touch



Modified from Elston (2003)

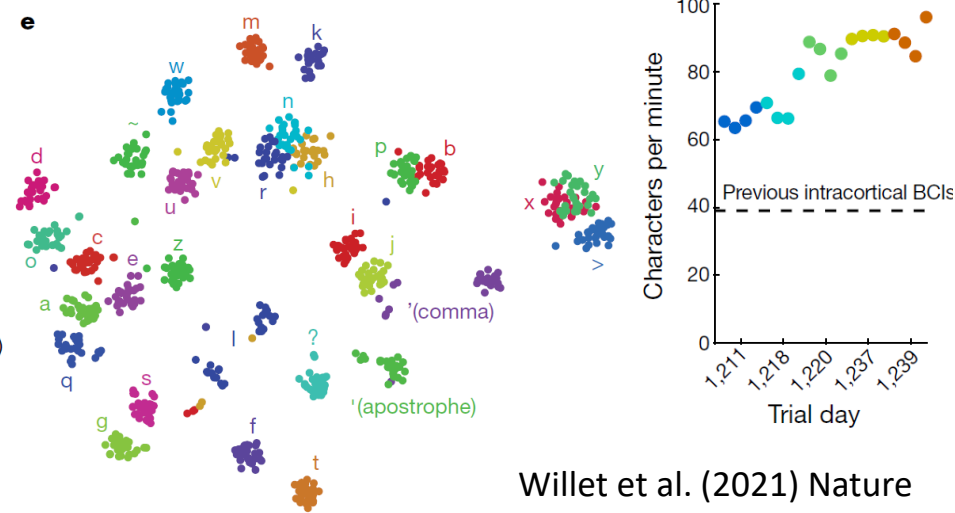
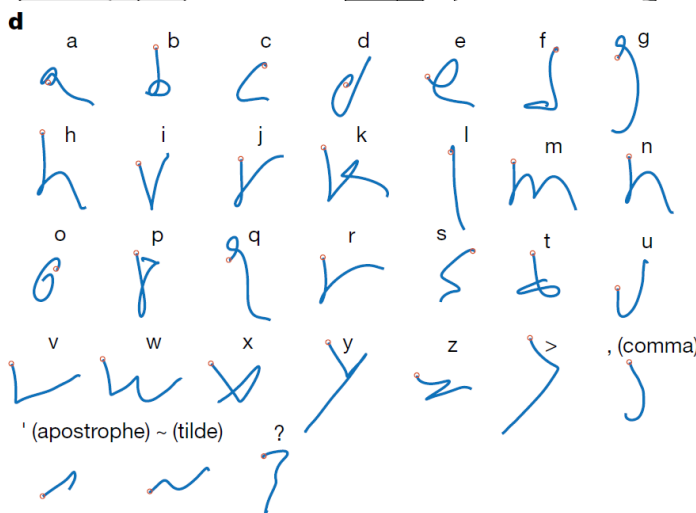
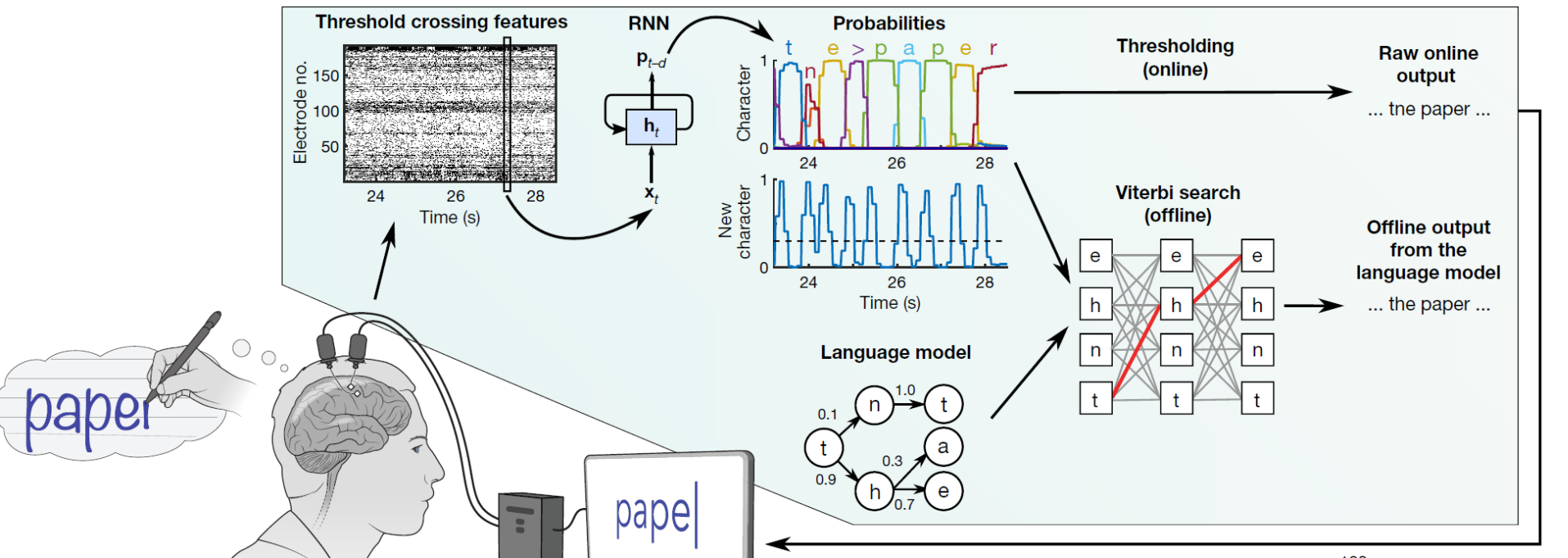


*motorický a
sensitive
homunkulus
jsou si velmi
podobní (velké
tváře, jazyk,
ruce; motorický
homunkulus
nemá genitál)

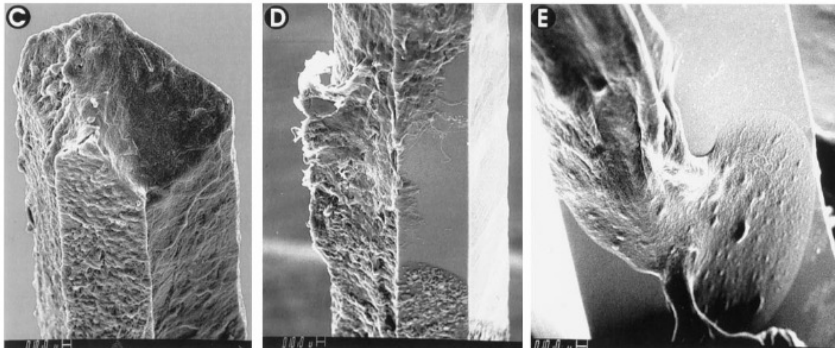
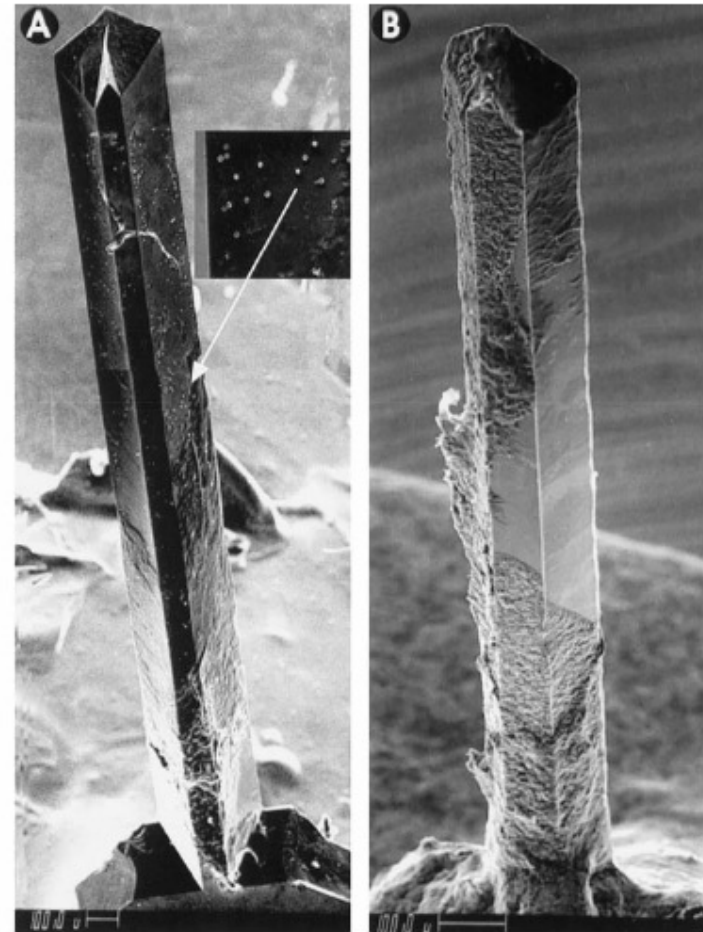
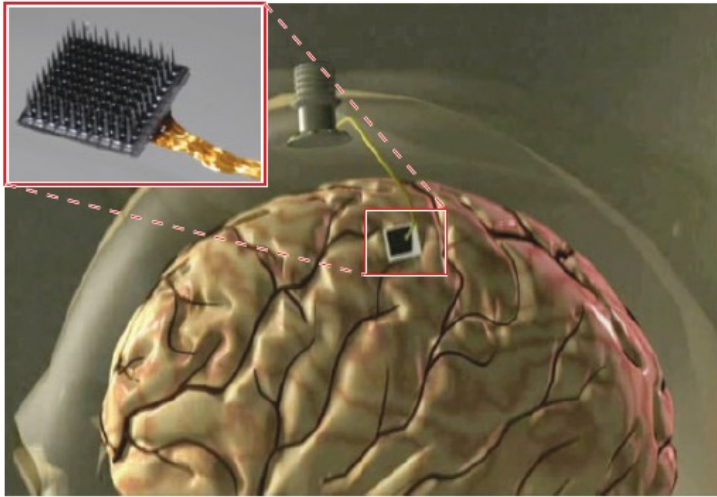
BCI (single neurons): text writing example



BCI (single neurons): text writing principle



Problem: myelination of micro-electrodes

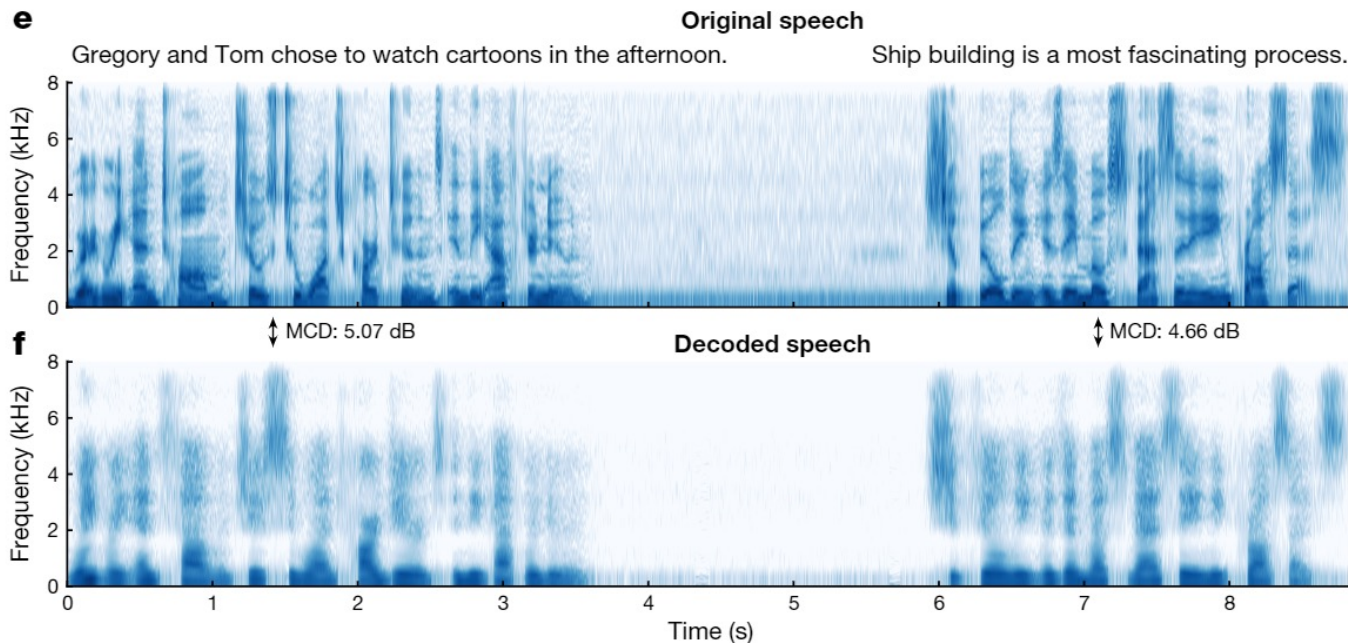
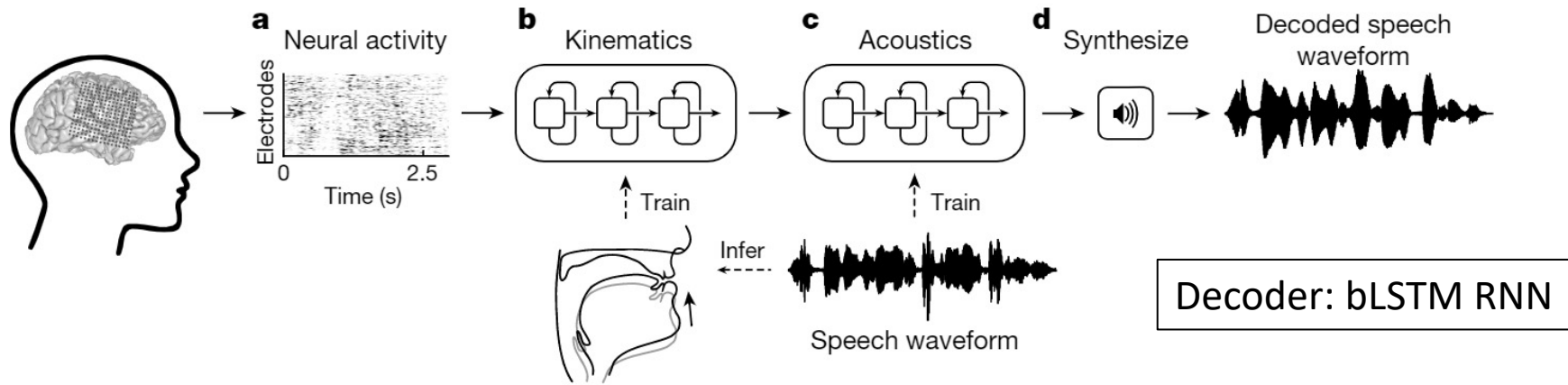


after 2 and 6 weeks after implantation

BMI: Speech synthesis of spoken sentences from ECoG



BMI: Speech synthesis of spoken sentences from ECoG



BMI: Speech synthesis of spoken sentences from ECoG

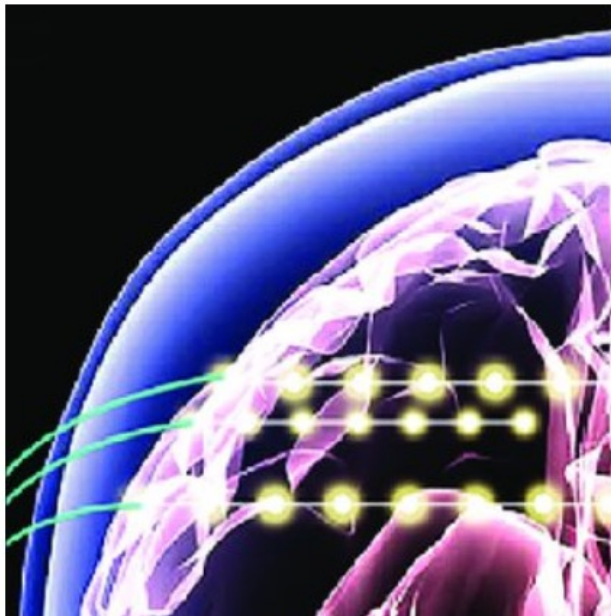
- We designed a recurrent neural network that decoded cortical signals with an explicit intermediate representation of the articulatory dynamics to synthesize audible speech.
- **STAGE 1:** a bLSTM RNN decodes **articulatory kinematic features** from continuous neural activity (Fig. 1a, b)
 - high-gamma amplitude envelope and low frequency component
 - from vSMC, STG, IFG
- **STAGE 2:** a separate bLSTM, decodes **acoustic features** (pitch, mel-frequency cepstral coefficients (MFCCs), ...) from the decoded articulatory features (Fig. 1c)
- **The audio signal** is then synthesized from the decoded acoustic features (Fig. 1d).
- To integrate the two stages of the decoder, stage 2 (articulation-to-acoustics) was trained directly on output of stage 1 (brain-to-articulation) so that it not only learns the transformation from kinematics to sound, but also corrects articulatory estimation errors made in stage 1.

„Our“ BMI research
(Prof. Tonio Ball, Freiburg)

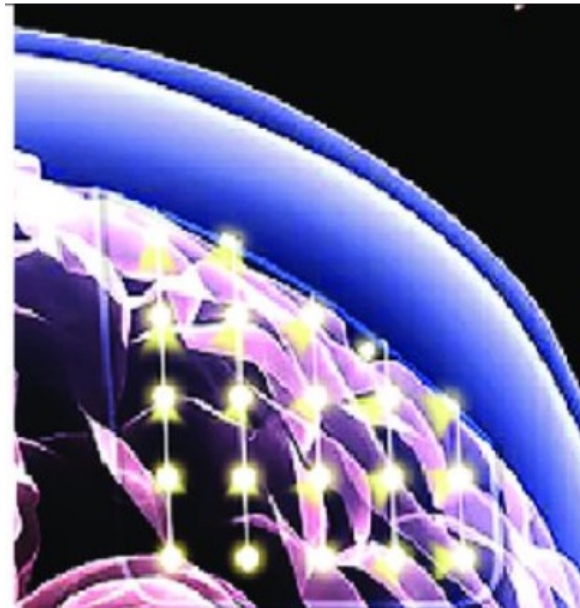
Intracranial EEG (iEEG)

- Invasive
- Signal quality is superior to scalp EEG
- Patients with epilepsy
- Cognitive experiments during video-EEG monitoring

sEEG (stereo-EEG)

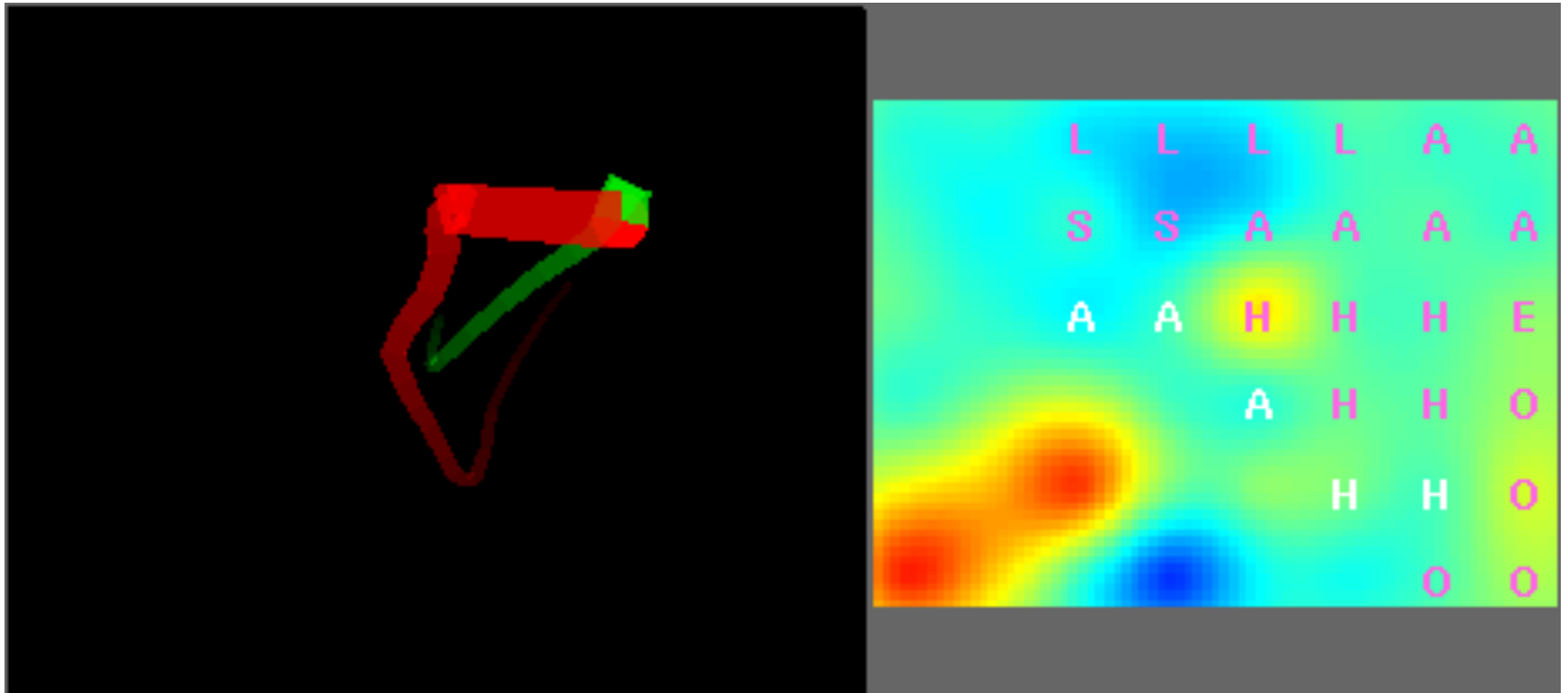


ECoG (electrocorticography)



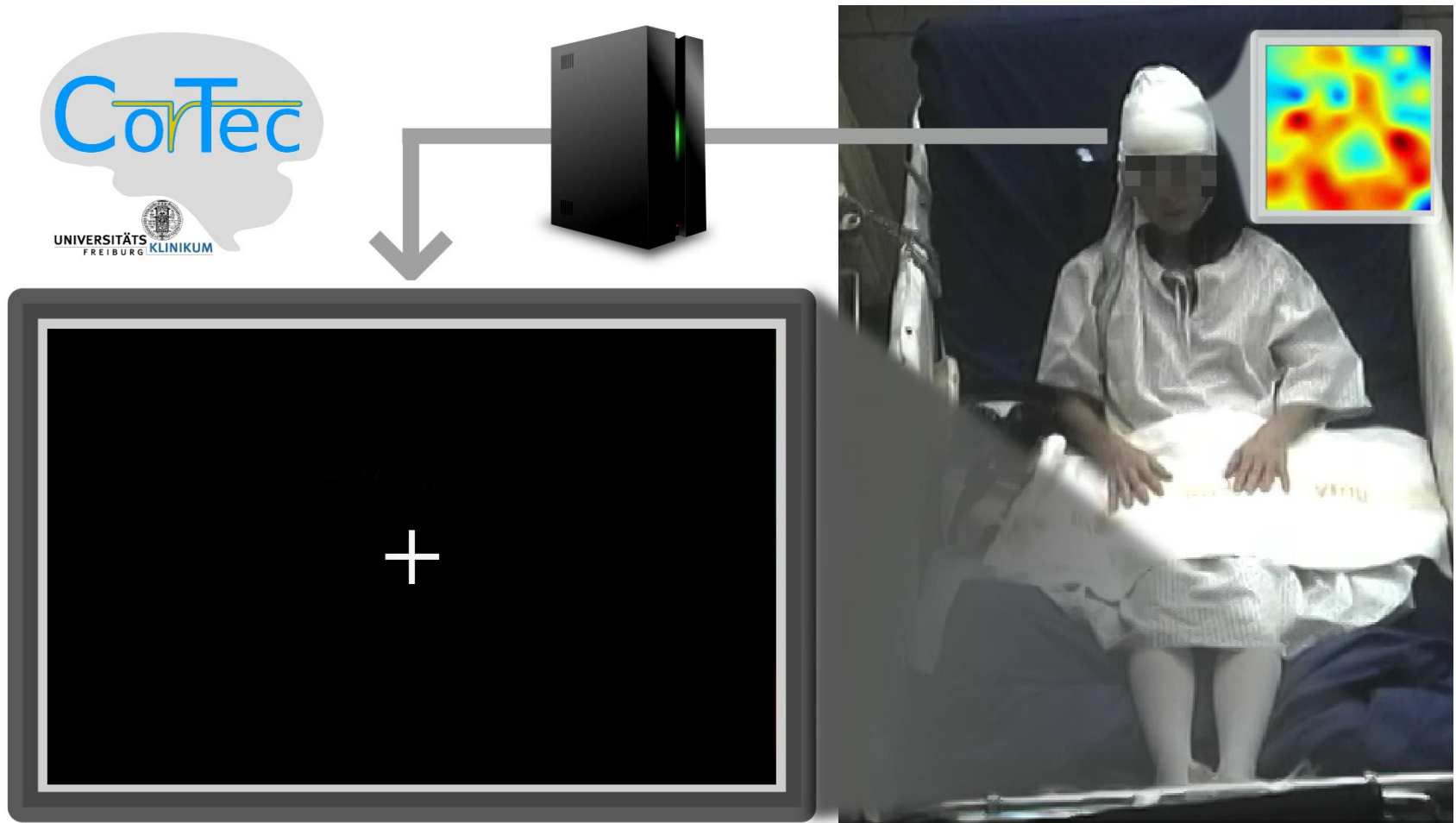
Biomimetic BMI (ECoG): example 1

(electrocorticography)



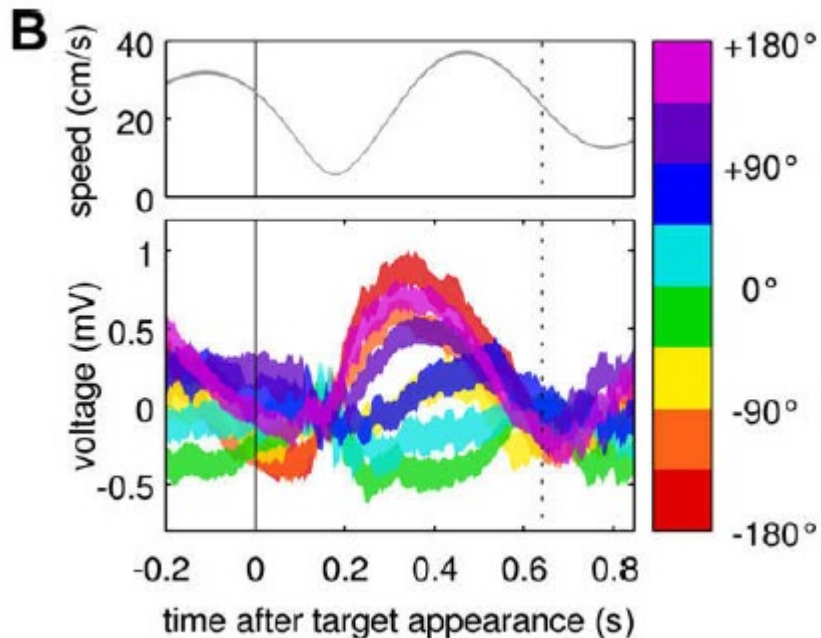
Biomimetic BMI (ECoG): example 2

(electrocorticography)



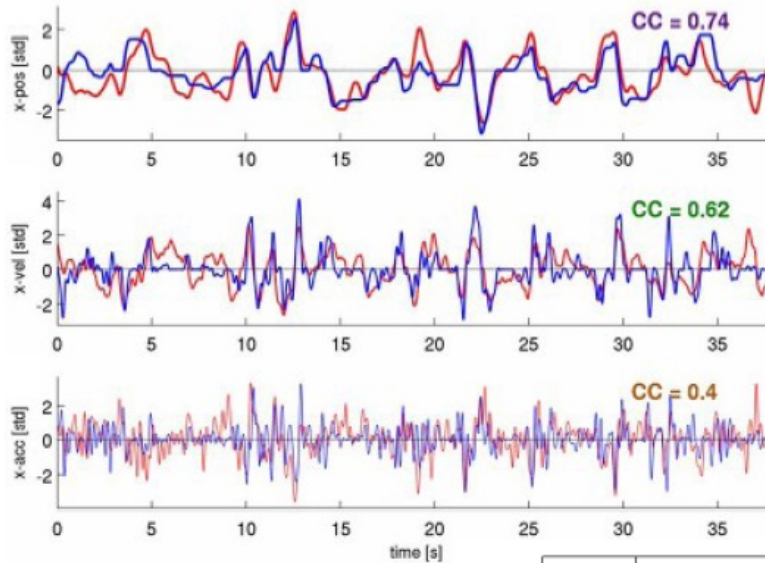
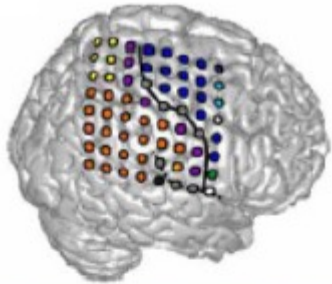
Biomimetic BMI (ECoG): principle

(electrocorticography)

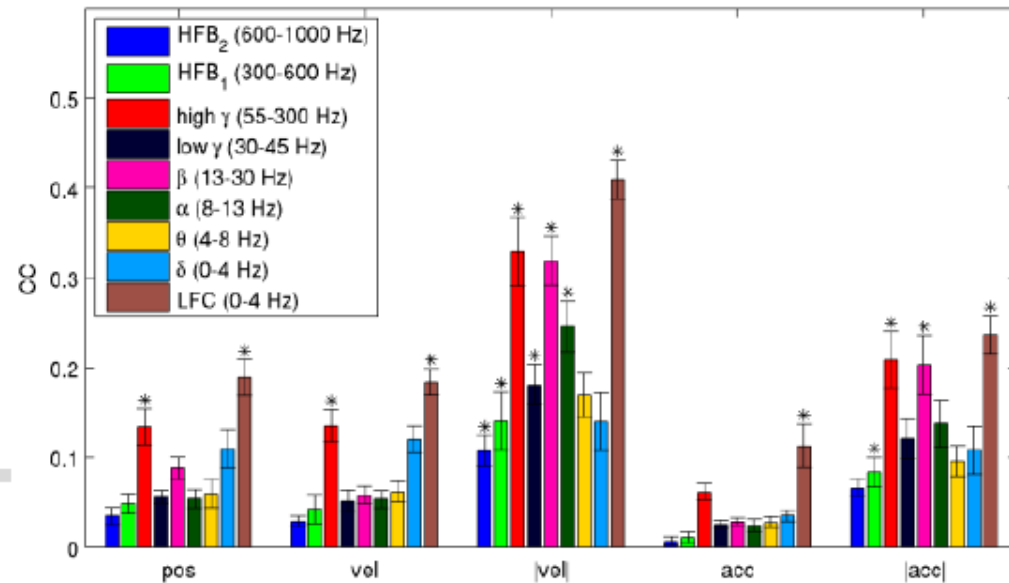


- Decoder: example 1
 - Kalman filter
- Decoder: example 2
 - LDA (linear discriminant analysis)

Biomimetic BMI (ECoG): “my own” results

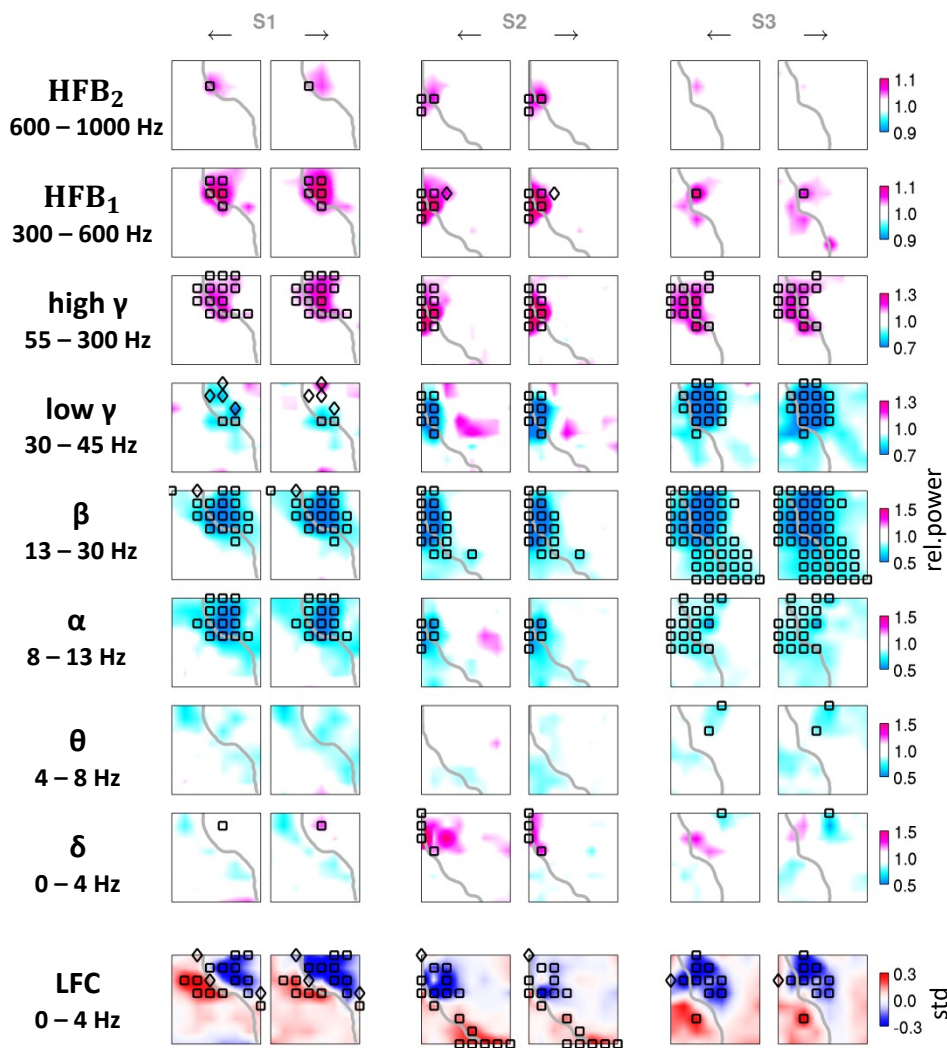


- Decoder:
 - multiple linear regression

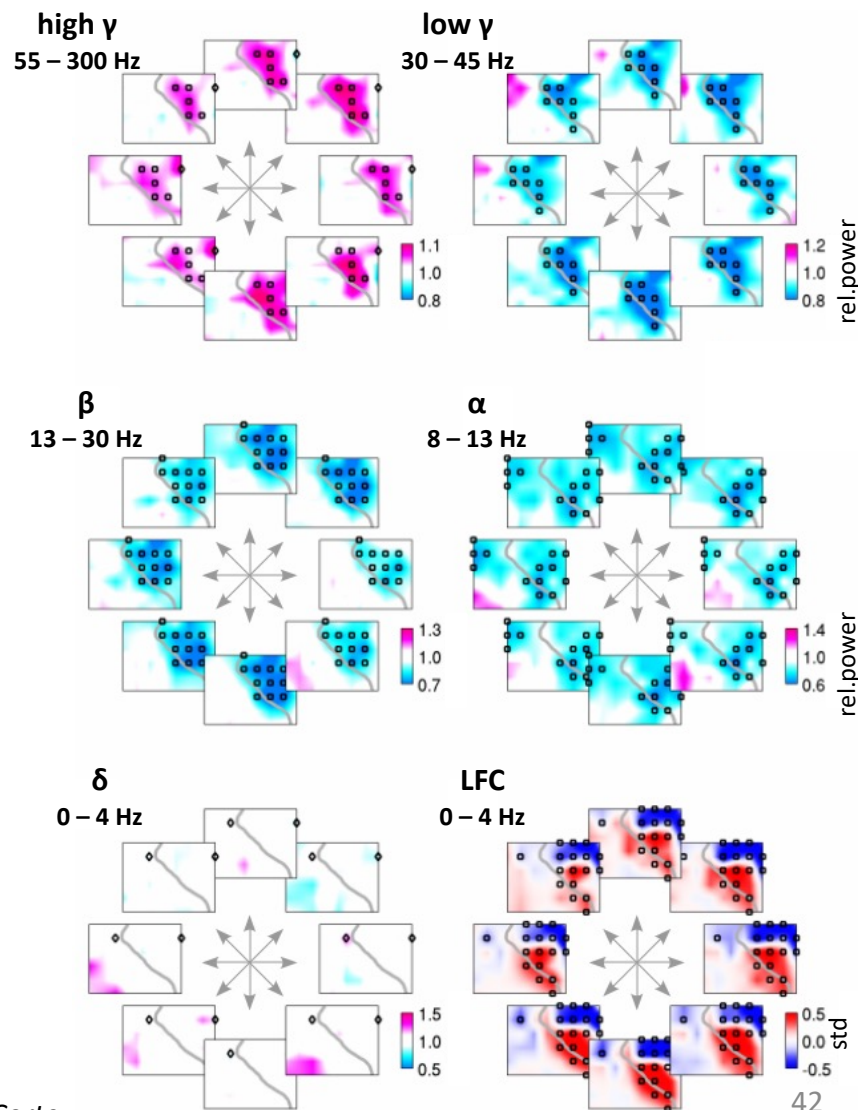


Tuning of ECoG to different movement directions

1-D control task



2-D control task



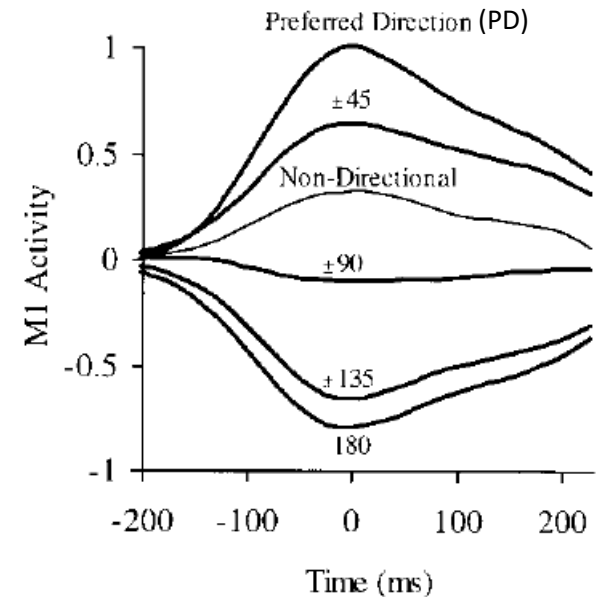
Movement speed correlates with motor-cortical activation.

Velocity tuning of single-unit activity (SUA)

- ECoG
 - strong speed tuning
 - weak directional tuning
- SUA
 - strong directional tuning
(e.g. *Georgopoulos et al. 1982*)
 - weak speed tuning
(e.g. *Moran and Schwartz, 1999*)

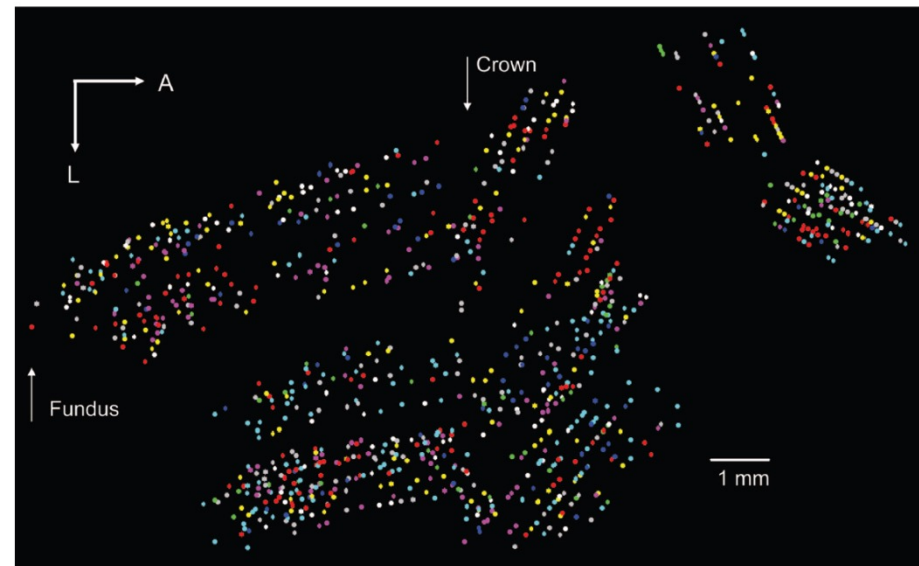
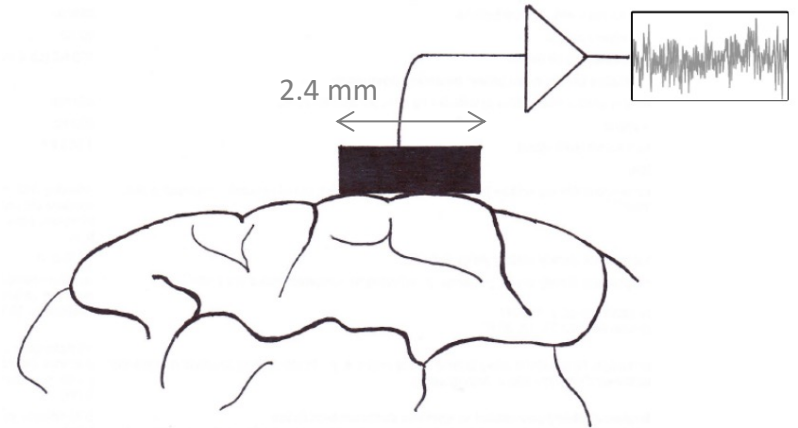


Modified from
Elston (2003)



Model of neuronal population activity

- Mimics the activity of a recorded ECoG electrode
- Assumptions
 - spatial sum of firing rates of underlying SUA
(Waldert *et al.*, 2009)
 - random distribution of PDs on a mm scale
(e.g. Georgopoulos *et al.*, 2007)
 - discharge activity as a function of movement velocity
(Moran and Schwartz, 1999)



Model of neuronal population activity

SNR of directional and speed tuning

$$P_N(\varphi, s) = \sum_{n=1}^N d_n(\varphi, s)$$
$$= \sum_{n=1}^N [S_n \cdot s + V_n \cdot s \cdot \cos(\varphi - PD_n) + \varepsilon_n]$$

$P_N \sim$ population activity of N neurons
 $d_n \sim$ discharge of n -th neuron
 $\varphi \sim$ direction
 $s \sim$ speed

Moran and Schwartz (1999)

Model of neuronal population activity

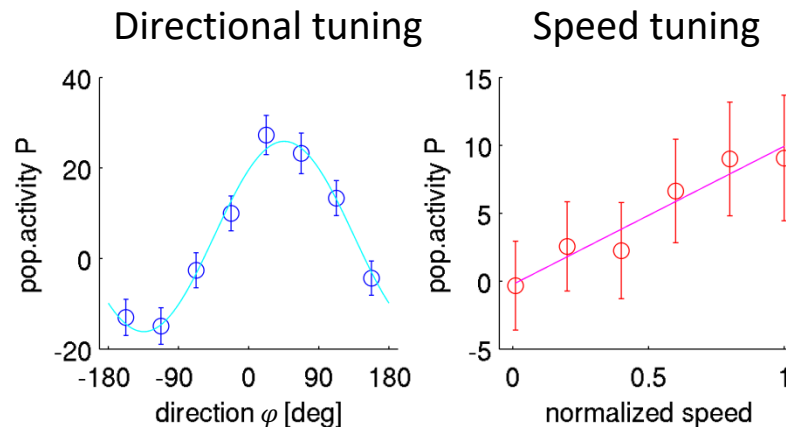
SNR of directional and speed tuning

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$P_N \sim$ population activity of N neurons
 $d_n \sim$ discharge of n -th neuron
 $\varphi \sim$ direction
 $s \sim$ speed

Moran and Schwartz (1999)

Example $P_N(\varphi, s)$
 $N = 1000$ neurons



$$SNR = \frac{var_{tuning}}{var_{trials}}$$

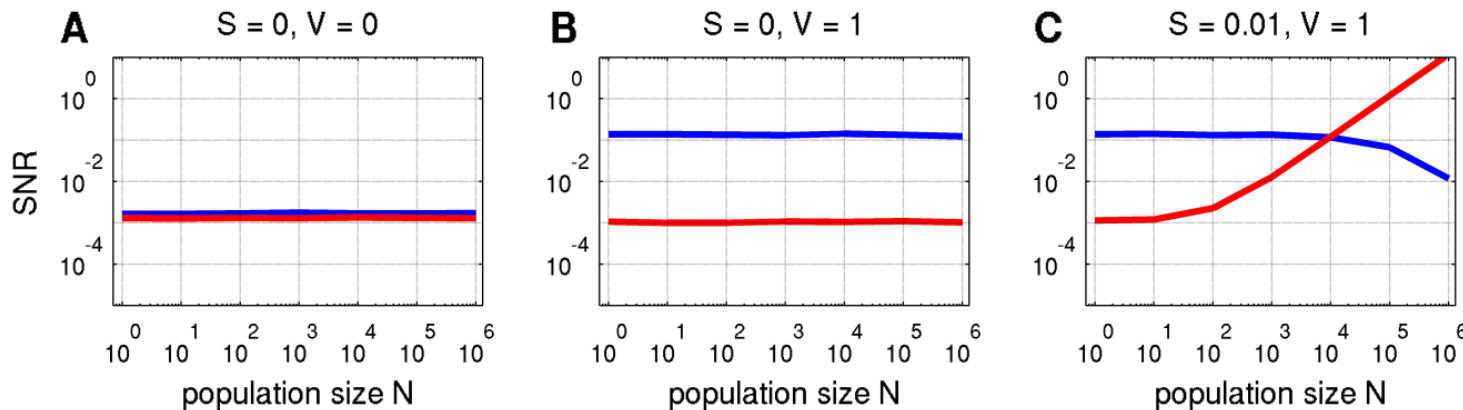
Model of neuronal population activity

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 $s \sim$ speed

Moran and Schwartz (1999)



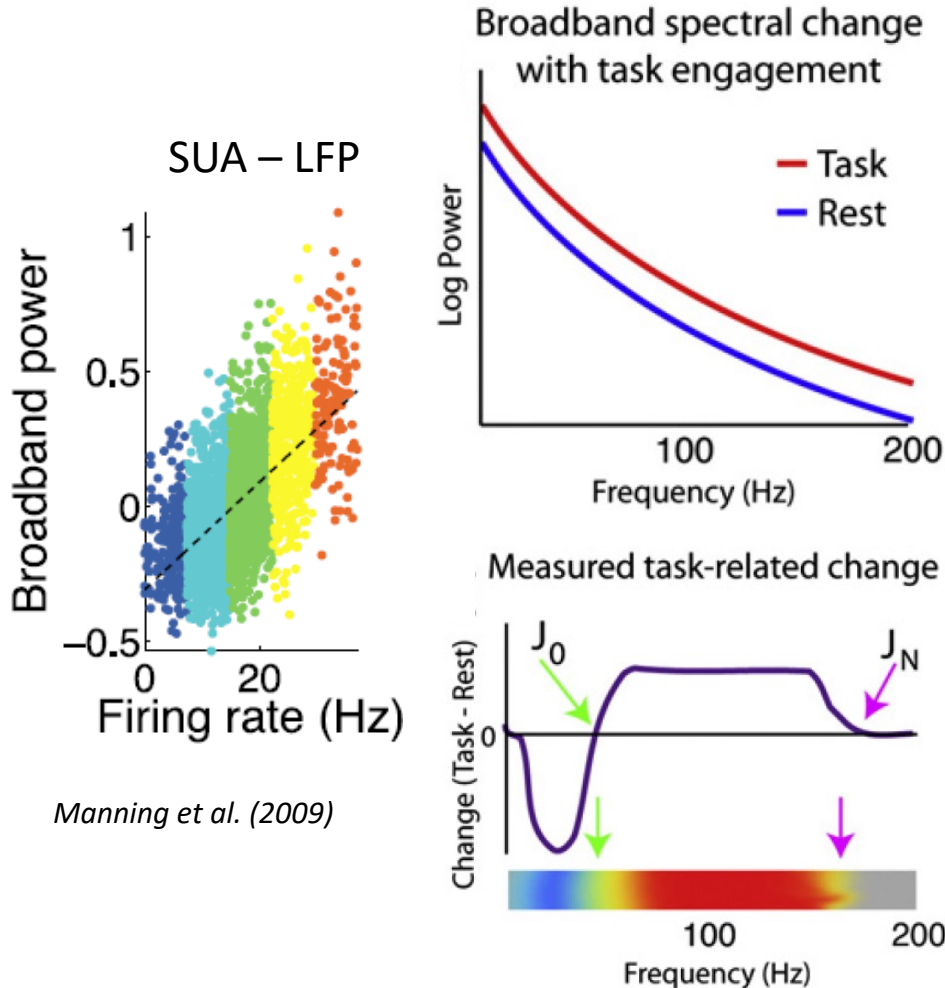
Hammer et al. (2016)

directional tuning
speed tuning

Neuronal population activity
is consistent with robust
speed representation.

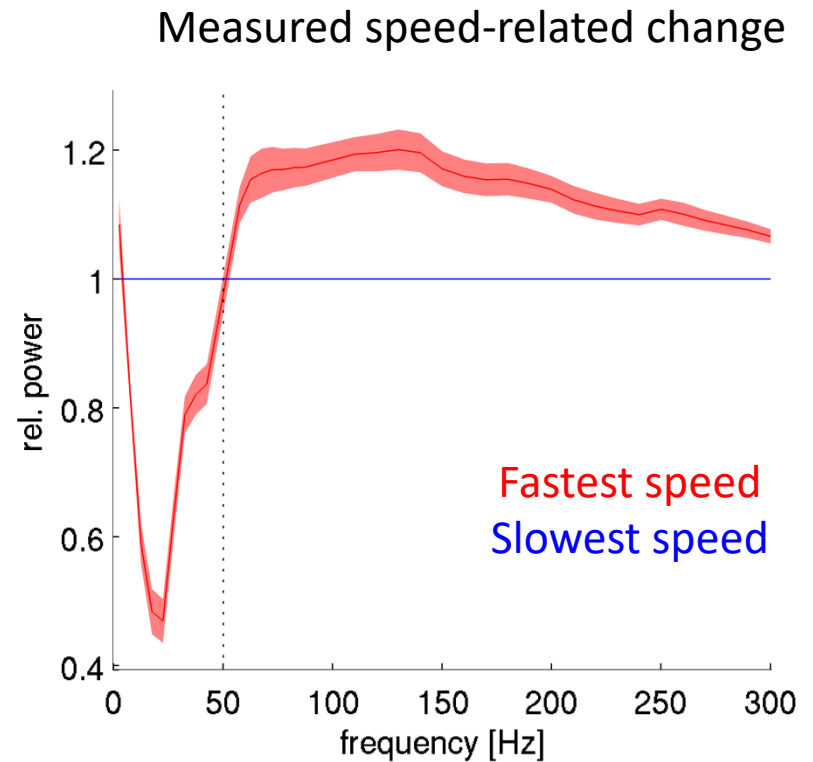
Neuronal population activity
increases with speed.

Why do we see speed-related power increase up to 1 kHz ?



Manning et al. (2009)

Miller et al. (2014)

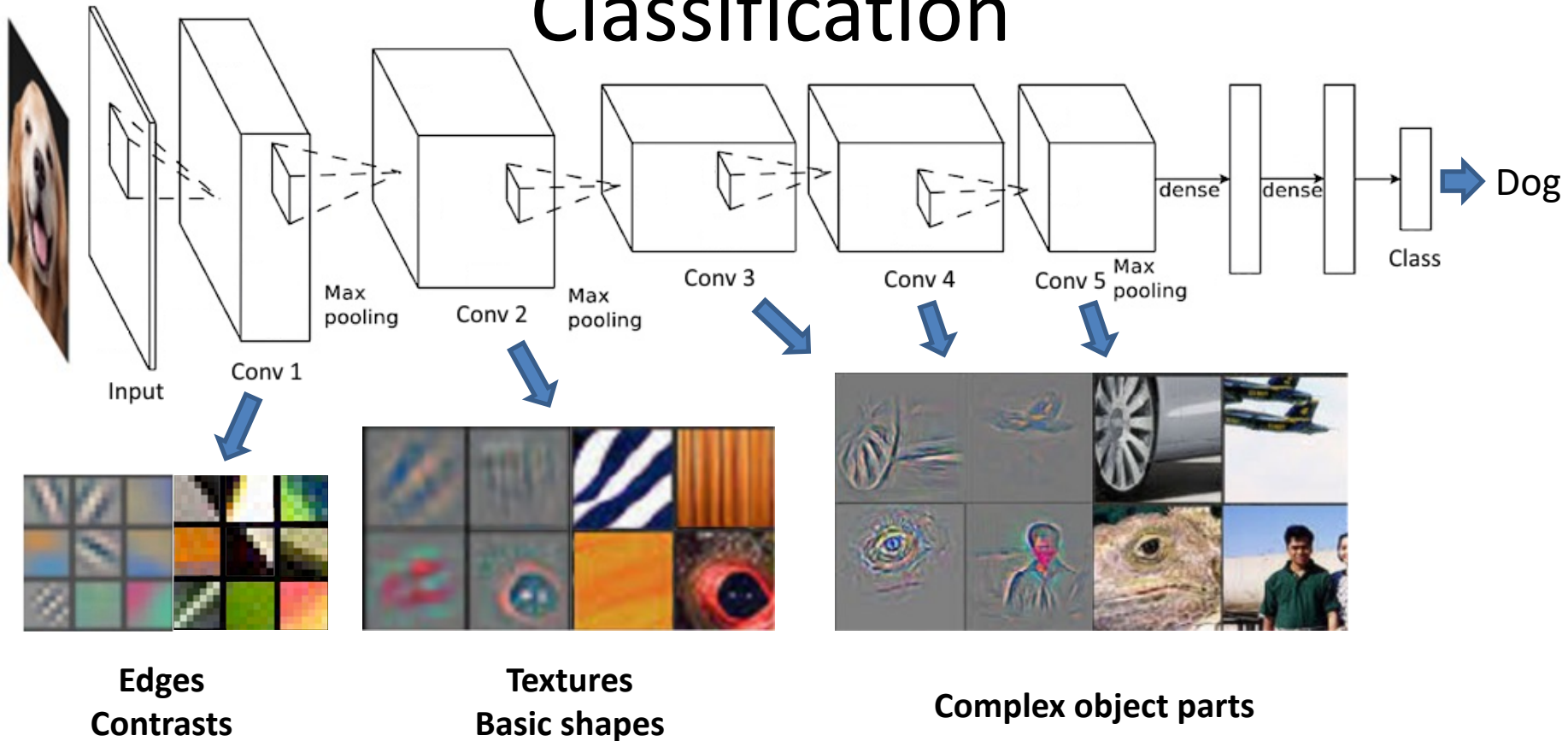


Hammer et al. (2016)

Deep learning in BMI

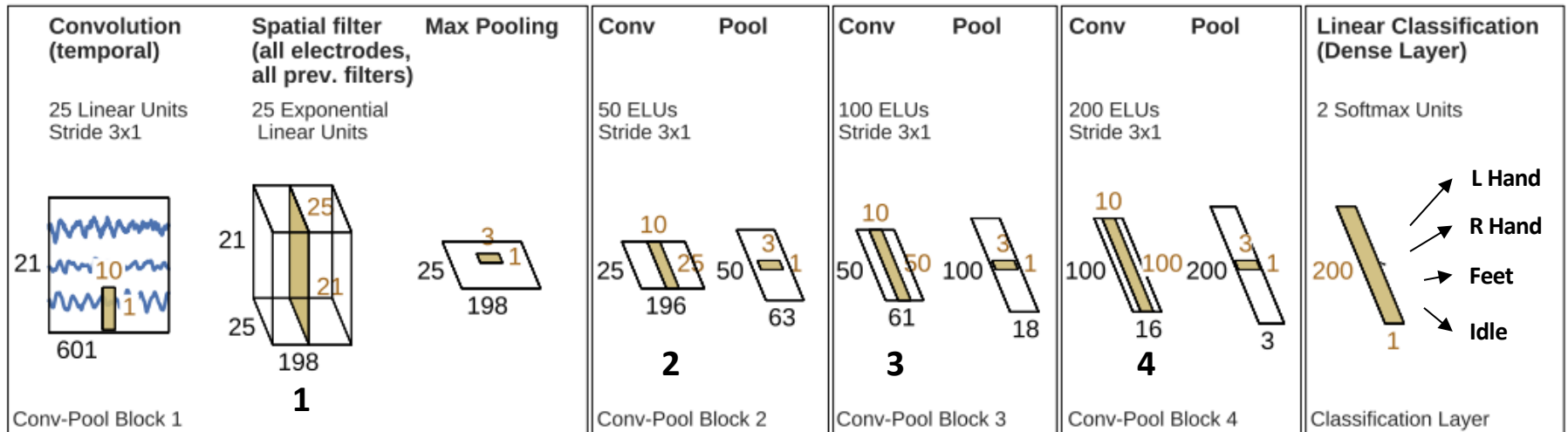
- Deep artificial neural networks
 - CNN (convolutional neural networks)
 - RNN (recurrent neural networks), ...
- Recent breakthroughs in hard machine learning problems
 - Computer vision
 - Language processing
 - ...
- + Super-human performance
- + Capable of *end-to-end* learning
- + No need for feature engineering
- - Particularly dark „black box“ algorithm
- - Requires large datasets
- Useful in BMI research ?

Intermediate Representations in ConvNets Trained for Image Classification



Krizhevsky et al. 2012
Zeiler et al. 2013

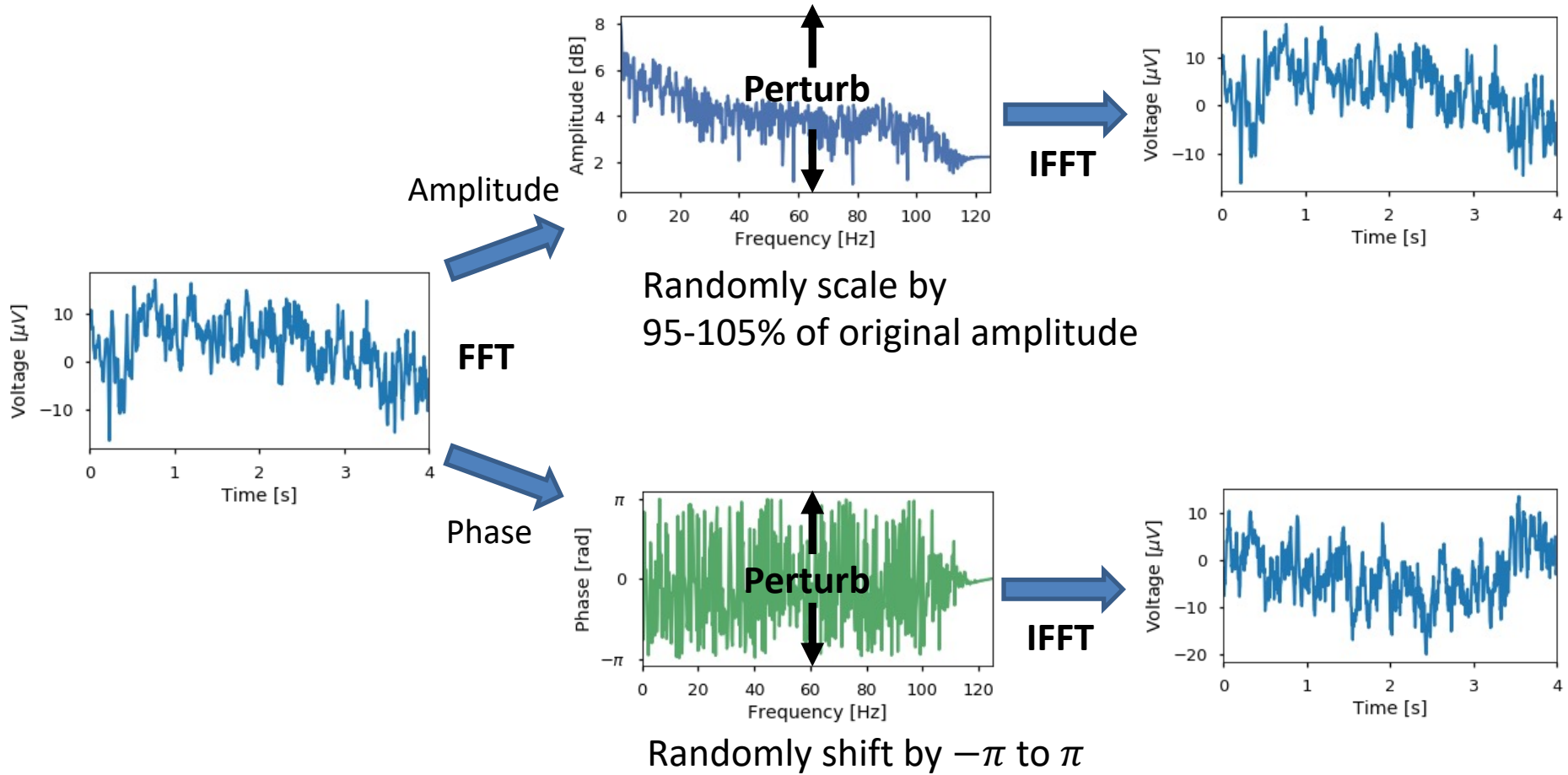
Deep4: CNN for EEG (classification problem)



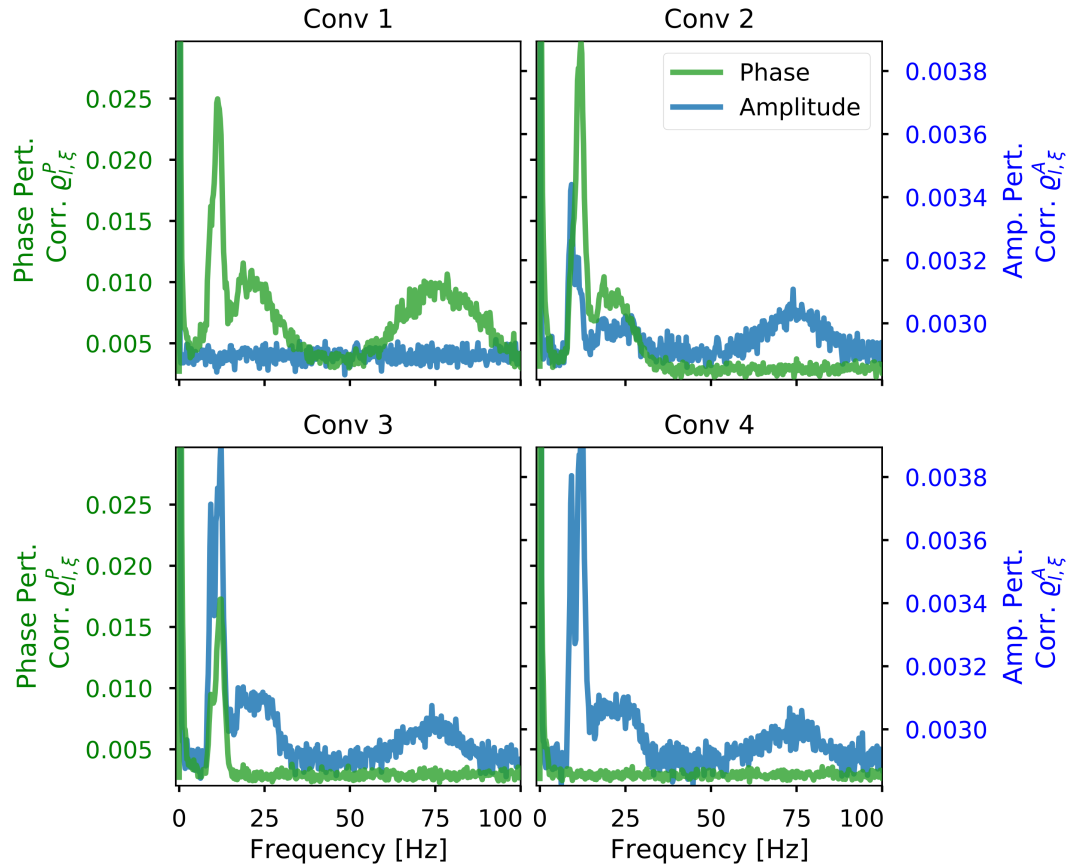
Schirrmeister et al. 2017

Investigate learned filters of convolutional layers: 1 2 3 4

Visualization by Perturbation

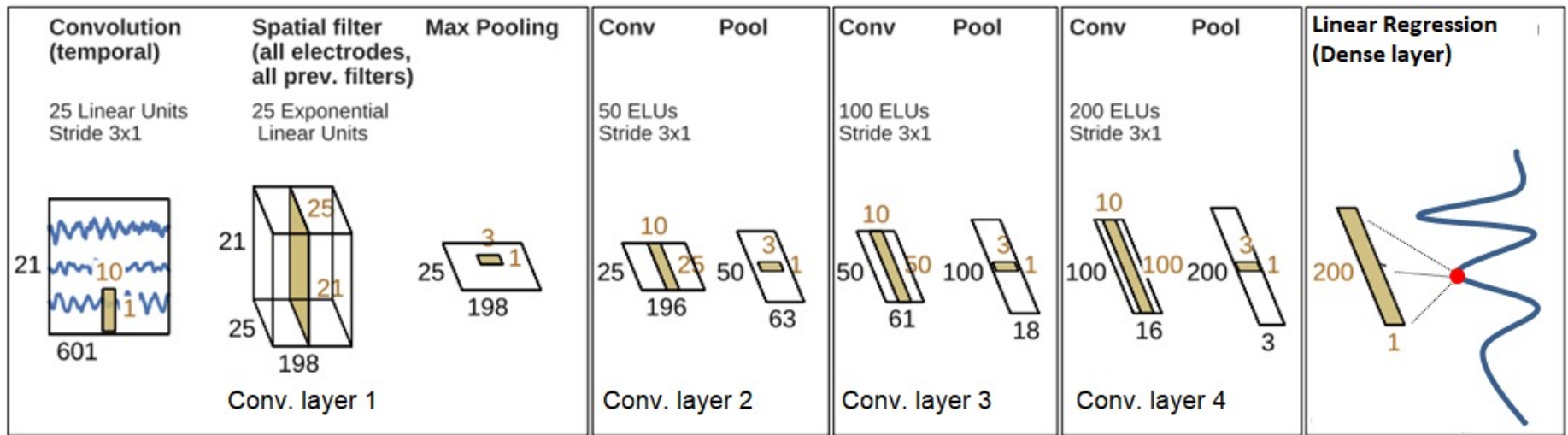


Perturbation Results



Hartmann et al. 2018

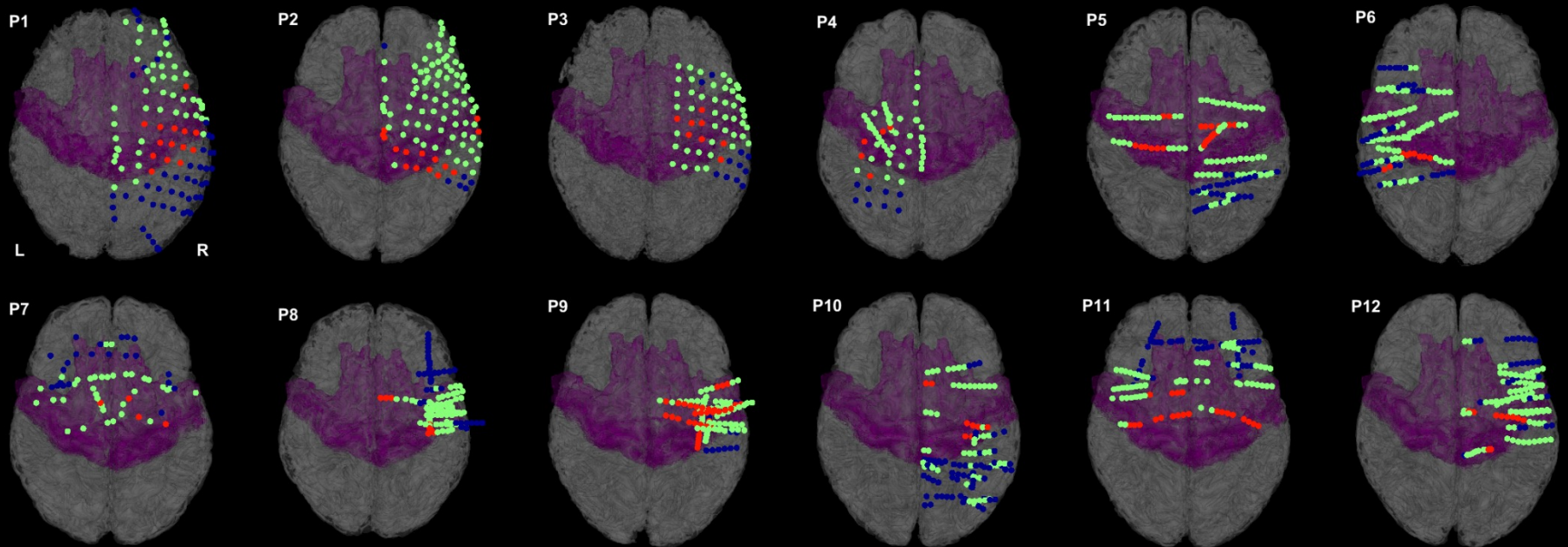
Deep4: CNN for EEG (regression problem)



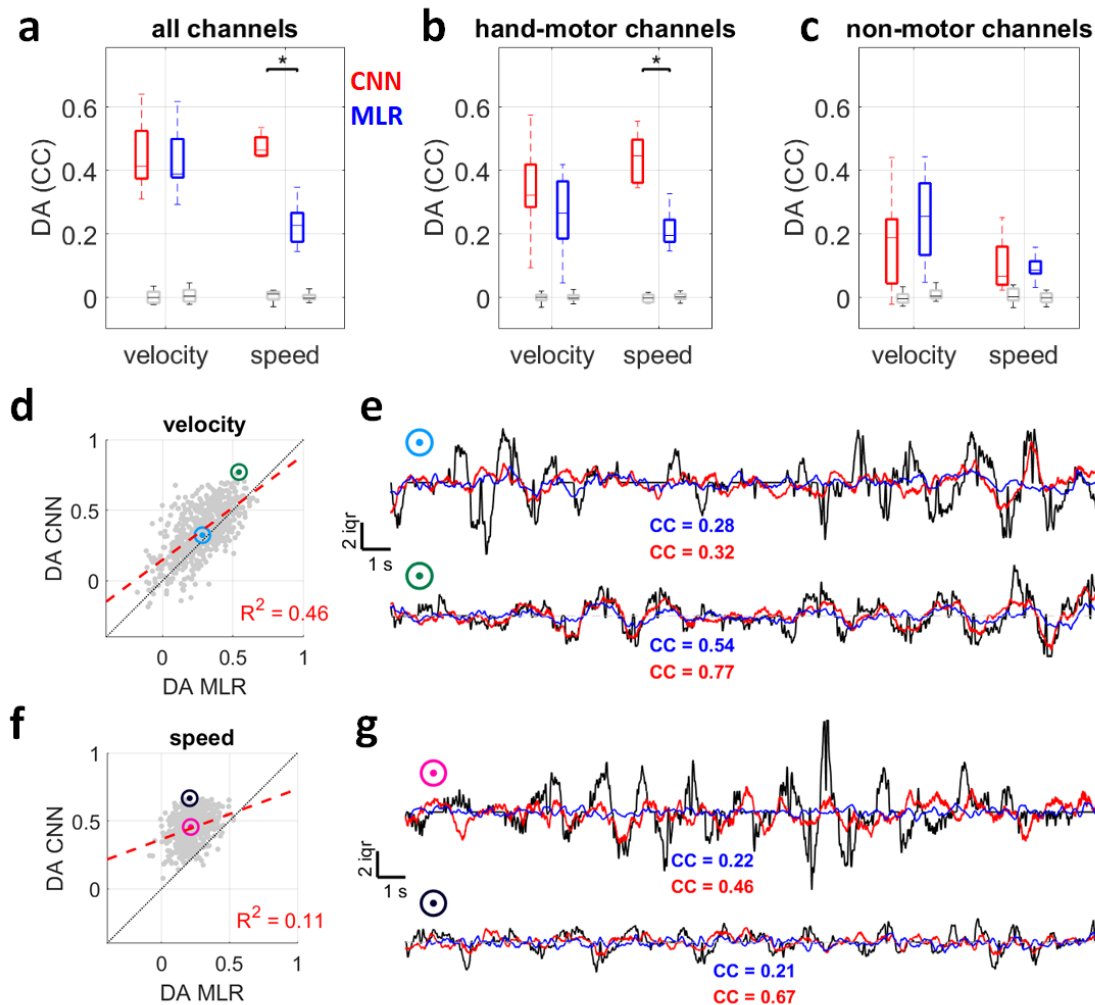
Hammer et al. 2019 – in prep.

Investigate learned filters of
convolutional layers: 1 2 3 4

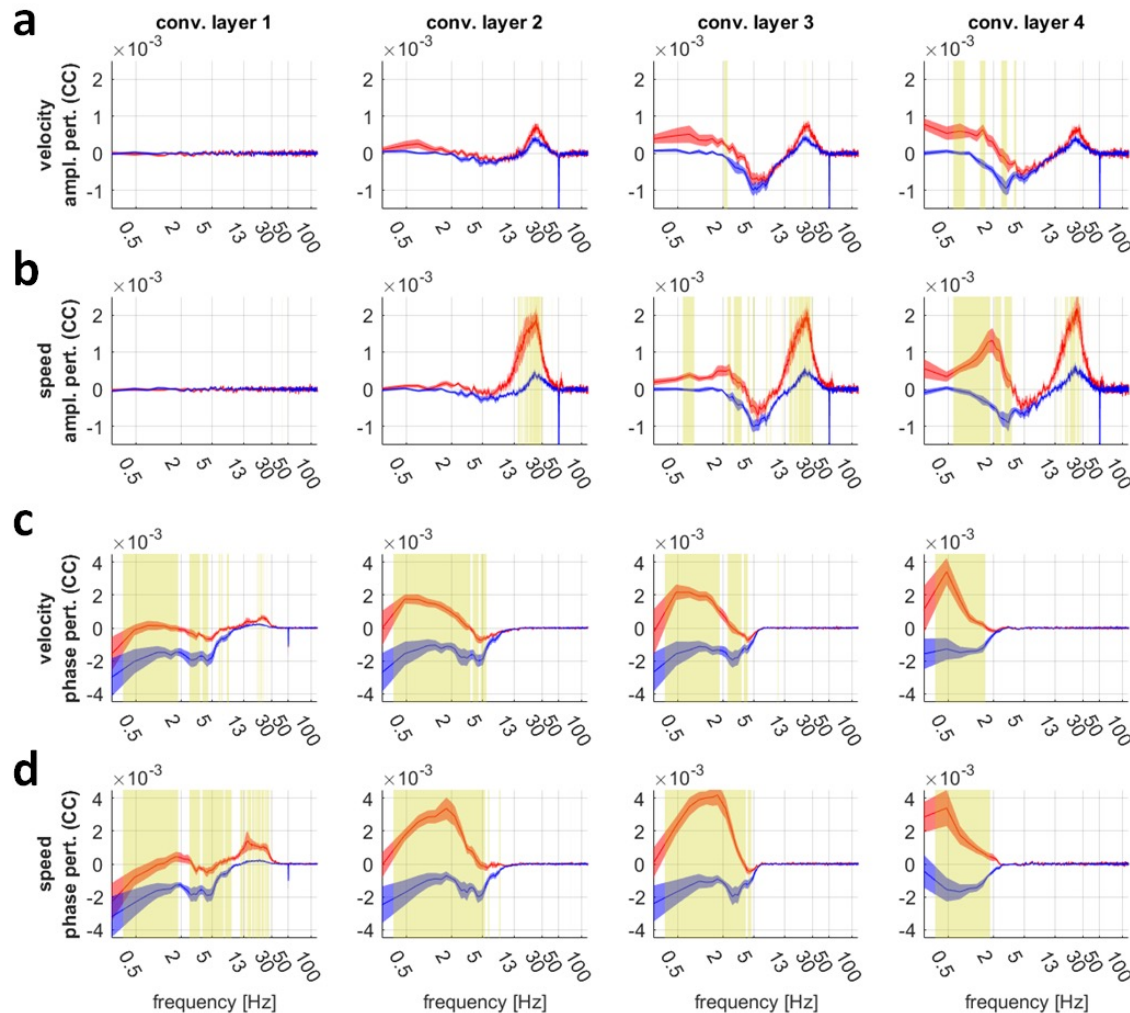
12 epilepsy patients with intracranial EEG implantations in motor cortex



Convolutional neural networks outperform multiple linear regression



Network sensitivity to amplitude and phase perturbations



Motor-cortex channels
Non-motor channels

Deep learning for iEEG decoding

- Convolutional neural networks (CNNs) are capable of *end-to-end* learning to decode movement from intracranial EEG.
- CNNs outperformed MLR and extracted information from motor cortex.
- CNNs learned low-frequency phase and beta-band amplitude information.
- Different CNN filters specialized for different features.

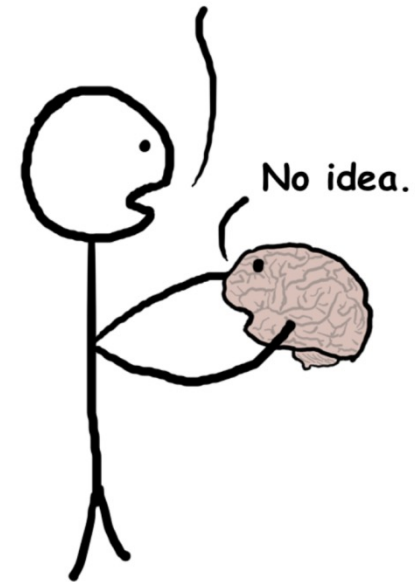
BMI usage

- Movement restoration
 - Paralyzed patients
- Neurorehabilitation
 - Patients after stroke
- Sensory restoration
 - Hearing: cochlear implants
 - Vision: retina / visual implants
- Brain stimulation
 - deep brain stimulation: Parkinson patients, depression, ...
 - epilepsy: seizure detection and stimulation
- Entertainment (gaming), ...
- Ethical issues!

Would you like to join our research?

- jirihammer@gmail.com
- Project, diploma thesis, PhD
 - ČVUT: doc. Daniel Novák, FEL
 - ČVUT: Dr. Radek Janča, katedra teorie obvodů, FEL
 - 2. LF UK: Prof. Petr Marusič
- Topics: closed-loop (with feedback) BCI
 - interdisciplinary (bioengineering, medicine, machine learning, stat. data analysis, hardware communication, software implementation, ...)
 - using iEEG
 - cooperation with
 - University of Freiburg (DE): Prof. Ball
 - University of Grenoble (FR): Prof. Bastin

How do you work?



Acknowledgements

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 - Martin Völker
 - Andreas Schultze-Bonhage
 - ...
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 - Petr Marusič
 - Adam Kalina
 - Pavel Čelakovský
 - Přemysl Jiruška
 - Pavel Kršek
 - ...

... a vám za pozornost

