Nodules and mammography

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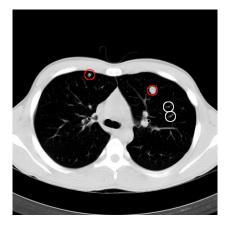
Murphy et al: A large-scale evaluation of automatic pulmonary nodule detection in chest CT using local features and k-nearest-neighbor classification

Key points

- Nodule (pre-cancer) detection
- ► Handcrafted features, simple classifier

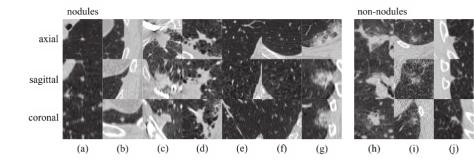
Pulmonary nodules

- small bright spots on chest CT (often round but not always)
- mostly benign but some may lead to cancer
- \blacktriangleright earlier detection \rightarrow better prognosis



Martin Dolejší

Nodule examples



Nelson trial data

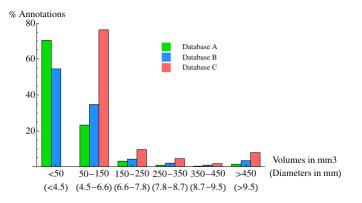
- ▶ 512×512 pixels, $306 \sim 860$ slices
- two observers to mark nodules
- small nodules (diameter < 3mm) may not be marked</p>
- if several scans per patient the earliest chosen
- \blacktriangleright TP = within 7 pixels
- Datasets: A all scans, B all scans with at least one big nodule, C - only big nodules

Table 1

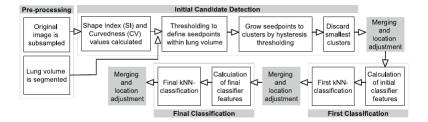
Statistics on the number of scans in the three databases.

	А	В	С
#Scans before checks	1588	1158	1158
#Scans with lung segmentation failures	53	37	37
#Scans after removing failures	1535	1121	1121
#Scans in training set	722	580	580
#Scans in test set	813	541	541
#Nodules in final training set	1369	1763	760
#Nodules in final test set	1525	1688	768

Size distribution



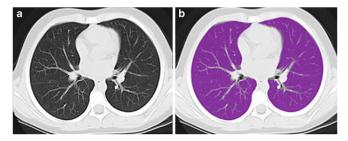
Flowchart



Preprocessing

• downsampling to 256×256

lung segmentation by registration with normal templates



from Jill Stein et al. DOI: 10.1007/s00247-016-3686-8

Shape index and curvedness

$$SI = \frac{2}{\pi} \arctan\left(\frac{k_1 + k_2}{k_1 - k_2}\right)$$
$$CV = \sqrt{k_1^2 + k_2^2}$$

Principal curvatures k_1, k_2

- minimum and maximum curvatures of the isosurface
- eigenvalues of the Hesssian with $\sigma = 1$

Shape index

1 local maximum = bright blob, 0.5 bright tubular structure, 0 saddle/flat...

Seed point detection

Cluster formation

Table 2

Initial seed thresholds.

Value	Upper threshold	Lower threshold
SI	1	0.8 (near pleural surface)
		0.9 (elsewhere)
CV	1	0.3

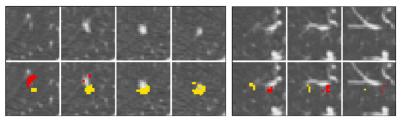
Table 3

Hysteresis thresholds.

Value	Upper threshold	Lower threshold	
SI	1	0.7 (near pleural surface)	
CV	1.3	0.2	

- Cluster merging (distance < 3 and 7 voxels). Small objects (<15 voxels) discarded.
- Candidate location = highest locally averaged intensity

Merging examples



(a)

(b)

Successive axial slices. (a) TP, (b) FP. Red/yellow — structures to be merged

False positive reduction

- Classify candidates
- ► *k*-NN classifier
- Two stages (15 and 50 features)
- Final stage on full resolution images
- Feature selection (Sequential forward floating selection)
- Operating point: sensitivity 90%

Training set generation

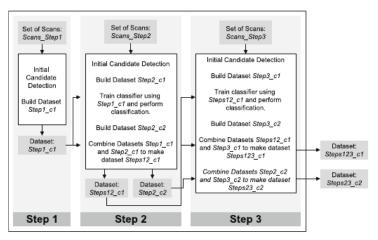


Fig. 4. Generation of training sets.

Subsample N class, N:P ratio 3:1, preserving pdf.

Features (1)

Table 4

The features calculated for the first kNN classifier. See text in Section 2.3.2.

ID	Description			
Features of the	Features of the voxel cluster			
a1	Cluster size (number of voxels)			
a2	Compactness1, ClusterSize			
a3	Compactness2, ClasterSize max dim*			
a4	Ratio max_dim:min_dim			
a5	Ratio max_dim:med_dim			
a6	Ratio Amed: Amax where Amax, Amed and Amin are the eigenvalues for the eigenvectors of the clu			
a7	Ratio Amin: Amax			
a8	Sphericity, mun_chister_voxels_in_sphere_S vot_sphere_S where sphere_S is a sphere at the candidate location with r			
a9	Ratio Sphericity:r			
Features of vox	Features of voxels in spherical kernels at the candidate location			
a10-a18	On grey-values over spherical kernels K: Average, Median, Standard-Deviation			



Table 5

The features calculated for the final kNN classifier. See text in Section 2.3.3

ID	Description	Notes			
Features of the voxel cluster	Features of the voxel cluster				
b1-b9	Features a1-a9 as described in Table 4				
b19	min_dim = min_(dim_i)	dim _i = width in di			
b20	max_dim = max_i(dim_i)	dim _i = width in di			
Features of voxels in spherical	kernels at the candidate location				
b10-b18	Features a10-a18 as described in Table 4				
b21-b26	On grey-values over spherical kernels K: Min, Max	Halfsizes of K: 1 (
b27-b36	On SI over spherical kernels K: Average, Median, Std-Dev, Min, Max	Halfsizes of K: 3 (
b37-b46	On CV over spherical kernels K: Average, Median, Std-Dev, Min, Max	Halfsizes of K: 3 (
Features calculated on random	ily chosen points on a spherical surface around the candidate location.				
b47-b76	Features of Gradient orientation values: Average(Avg), Median,	30 points on sphe			
	Max, Min, Std-Dev, Coefficient of	b66), 50 points or			
	Variation, Ratio Max:Min, Ratio Std-Dev:Median, Ratio				
	Median:Avg, Ratio Median:Max				
b77-b106	Features of Gradient magnitude values: Average(Avg), Median,	30 points on sphe			
	Max, Min, Std-Dev, Coefficient of Variation, Ratio Max:Min, Ratio	b96), 50			
	Std-Dev:Median, Ratio Median:Avg, Ratio Median:Max	points on sphere			
Features of voxels in the candi					
b107-b115	Features a1-a9 as described in Table 4 but calculated this time ow	er the segmented v			
b116	$min_dim = min_i(dim_i)$				
b117	$max_dim = max_i(dim_i)$				
b118-b122	On grey-values over segmented voxels: Average, Median, Std-Dev,	Min, Max			
b123-b127	On SI of segmented voxels: Average, Median, Std-Dev, Min, Max				
b128-b132 b133	On CV of segmented voxels: Average, Median, Std-Dev, Min, Max				
b134	Ratio Num segmented voxels: Num ROI voxels Ratio {Distance from candidate location to the farthest point in th	a componiation):			
1111	{Number of voxels in the segmentation}	e segmentation).			
Other features					
b135 Posterior probability of being a true nodule from the first classication step					
	reaction probability of being a true noture from the first classical	ion step			

Results

Table 7

Results for experiments on database A.

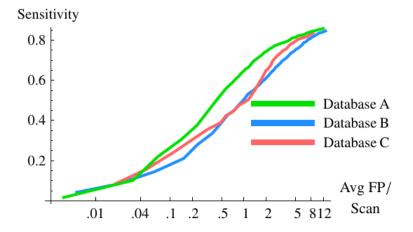
Number of Scans Number of annotations	813 1525	
	Sensitivity	FP per scan
After initial candidate detection After first classification After final classification	97.2% 92.3%	649.0 77.3
 At around 4 FP per scan 	80.0%	4.2

Table 9

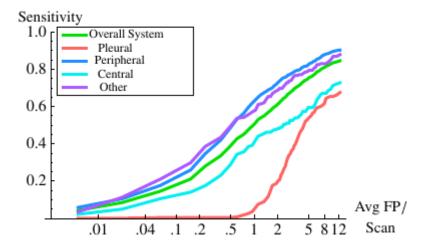
Results for experiments on database C.

Number of scans Number of annotations	541 768	
	Sensitivity	FP per scan
After initial candidate detection	98.2%	752.1
After first classification After final classification	92.2%	51.2
– At around 4 FP per scan	77.7%	4.2

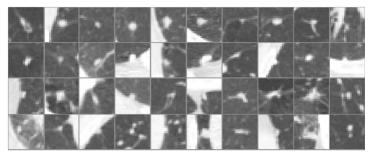
FROC curve



FROC by location

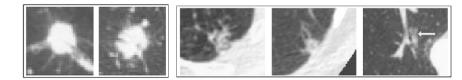


Example nodules

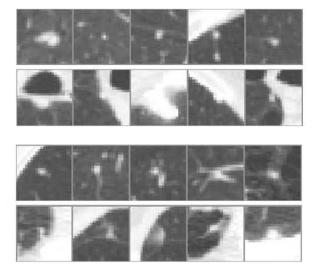


top row - easy detections (p>0.9), bottom row - not detected (p<0.35)

Missed nodules



False positives



Setio et al: Pulmonary Nodule Detection in CT Images: False Positive Reduction Using Multi-View Convolutional Networks. IEEE TMI 2016

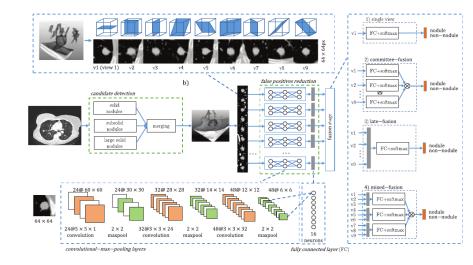
Key points

- Nodule detection from 3D CT
- Candidate detection (by 3 specialized detectors)
- CNN for FP reduction
- \blacktriangleright 2D patches/planes + fusion

Datasets

- LIDC 1018 scans, 888 retained (ignore thick-slice cases), 4 observers
- ANODE09 55 scans, 2 observers,
- DLCST 612 scans, 2 observers, 898 nodules
- considered nodules > 3mm

Flowchart



Candidate detection

- Solid nodules Murphy's detector (shape index, curvedness, thresholding, clustering)
- Subsolid nodules (pure and part-solid ground-glass) thresholding, morphological opening, connected components, segmentation
- Large nodules (>10mm, possibly attached to pleura) lung segmentation, rolling-ball segmentation smoothing, density thresholding, multi-scale morphological opening

11100001

DETECTION SENSITIVITY OF CANDIDATE DETECTION ALGORITHMS

Total number of CT scans: 888

Total number of nodules: 1,186

Candidate detection	Detected nodules	Sensitivity (%)	False Positives (FPs)	FPs per scan
Solid	1,016	85.7	292,413	329.3
Subsolid	428	36.1	255,027	287.2
Large solid	377	31.8	41,816	47.1
Combined set	1,120	94.4	543,160	611.7
Reduced set	1,106	93.3	239,041	269.2

Patch classification

Patch extraction

 $\blacktriangleright~50\times50mm,~64\times64pixels,$ nine planes CNNs

- ▶ 3 convolutional layers, 3 max-pooling layers
- testing 1 s per scan on a GPU

Fusion

Committee fusion

- FC layer + softmax + product rule
- each stream trained separately

Late fusion

- concatenate FC layer outputs
- FC layer + softmax

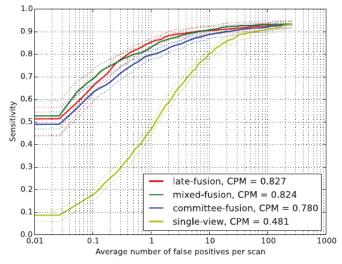
Mixed fusion

- group 9 patches into 3 groups of orthogonal views
- contenate within group (as in late fusion)
- FC layer + softmax + product rule (as in committee fusion)

Training

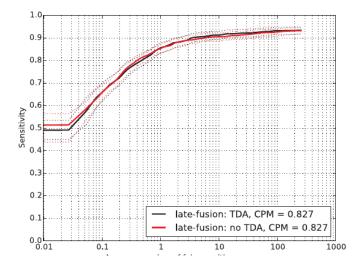
- Negative training data pruning
 - preliminary classification by existing algorithms
 - eliminate candidates with low nodule probability
- 5-fold cross-validation on LIDC (3/5 training, 1/5 validation, 1/5 testing)
- cross-entropy error
- RMSprop optimizer
- random initialization
- dropout regularization
- augmentation of nodules (shift, scaling)
- random upsampling of nodules for training
- test-data augmentation (scaling)

FROC fusion

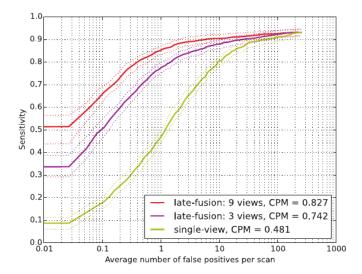


CPM (competition performance metric) = average sensitivity at 1/8,1/4,...,4,8 FP/s

FROC test augmentation



FROC number of views



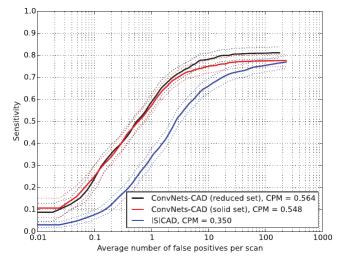
LIDC results

TABLE III

PERFORMANCE BENCHMARK OF CONVNETS CONFIGURATIONS ON LIDC-IDRI DATASET. THE BEST SCORE FOR EACH PERFORMANCE METRIC IS MARKED IN BOLD. FOR COMPARISON PURPOSES, THE PERFORMANCE OF THE COMBINED ALGORITHMS [3], [5], [27] IS INCLUDED

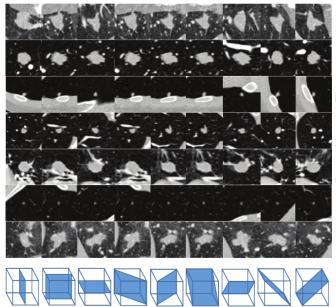
Configuration	Number of views	AUC	СРМ
combined algorithms	-	0.969	0.573
single-view	1	0.969	0.481
committee-fusion	3	0.981	0.696
	9	0.987	0.780
late-fusion	3	0.987	0.742
	9	0.993	0.827
mixed-fusion	3*3	0.996	0.824

DLCST results



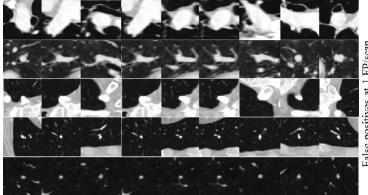
sensitivity 76.5% at 6 FPs/scan, which is 94% of the true candidate nodules

True positives



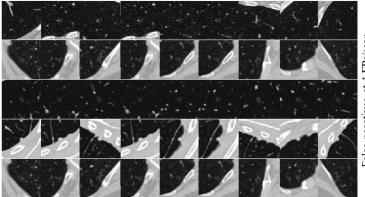
Irue positives at 1 FP/scan

False positives



False positives at 1 FP/scan

False negatives



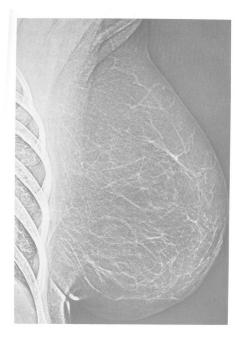
False negatives at 4 FPs/scan

Kooi: Large scale deep learning for computer aided detection of mammographic lesions. MIA 2017

Key points

- detect lesions from mammographs
- candidate detection learned
- classification to reduce FPs
- combine deep and manual features

Mammography



Data overview

Table 1

Overview of the data. Pos refers to the amount of malignant lesions and neg to the amount of normals.

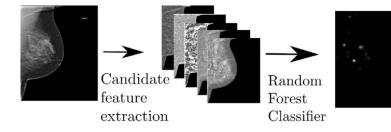
	Cases		Exams		Images		Candidates	
	Pos	Neg	Pos	Neg	Pos	Neg	Pos	Neg
Train	296	6433	358	11,780	634	39,872	634	213,450
Valid.	35	710	42	1247	85	4218	85	19,460
Test	124	2064	124	5317	271	18,182	271	180,777

Candidate detection

5 features based on Gaussian derivative kernels

- center of mass
- size
- spiculation (radiating lines)
- random forest classifier
- training data
 - positive samples from annotated lesions
 - negative samples randomly
- test time apply RF to all pixels

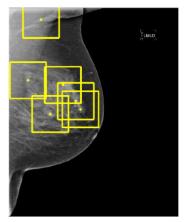
Candidate detection examples



Patches for CNN



(a) Illustration of segmentations for the reference system.



(b) Illustration of extracted patches for the CNN.

Baseline (classical system)

mass segmentation by dynamic programming in polar coordinates

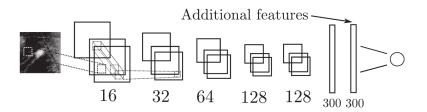
74 features:

- candidate detector features,
- contrast features,
- texture features,
- geometry features
- context features (rest of the breast)
- patient features

RF classifier (also tested SVM, gradient boosted tree, MLPs)

CNN

- ReLU
- Binary cross-entropy loss
- Data augmentation (scale, translation, flip)
- scaled-down VGG model (6 layers with 3 × 3 kernels, 2 × 2 max-pooling), FC layer with 300 neurons
- positive samples randomly oversampled
- deep networks tried but did not improve the results



Feature importance

Table 3

Overview of results of the CNN combined with individual feature sets.

Feature group added to CNN	AUC	CI
CNN Only	0.929	[0.897, 0.938]
Candidate detector	0.938	[0.919, 0.955]
Contrast	0.931	[0.91, 0.949]
Texture	0.933	[0.912, 0.950]
Geometry	0.928	[0.907, 0.946]
Location	0.933	[0.913, 0.950]
Context	0.934	[0.914, 0.952]
Patient	0.929	[0.908, 0.947]
All	0.941	[0.922, 0.958]

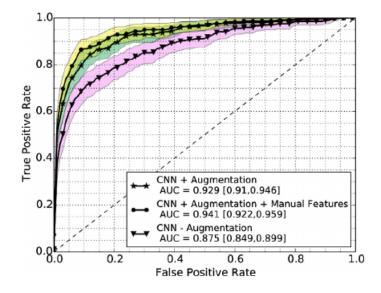
Dataset size importance

Table 4

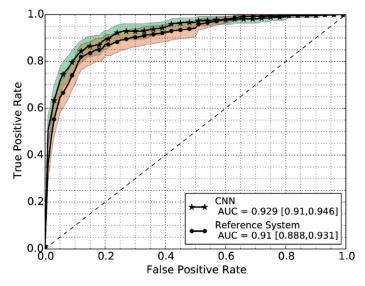
AUC values obtained when training the network on subsets of malignant lesions in the training set, keeping the same amount of normals.

Data Augmentation	60%	All
With	0.842	0.929
Without	0.685	0.875

Augmentation importance

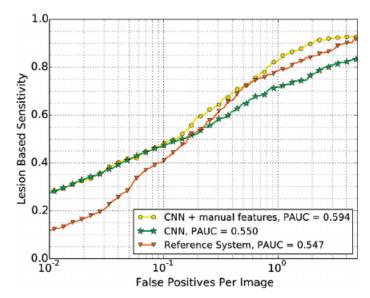


CNN versus baseline



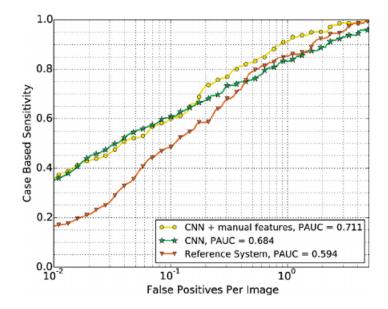
excluding context, location, patient information

CNN versus baseline

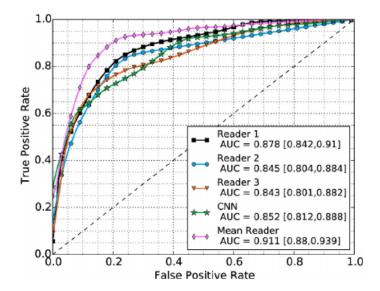


including context, location, patient information

CNN versus baseline Case FROC

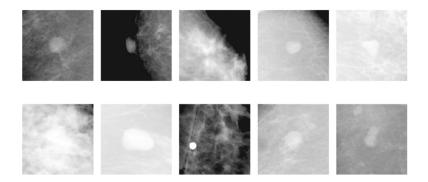


CNN versus human readers

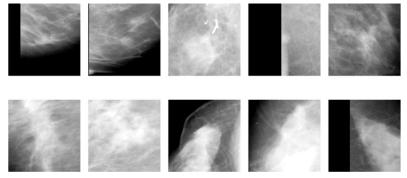


no significant difference between CNN and any readers difference with mean of readers significant

False positives



False negatives



mostly very large lesions, under-represented in the training set