## Nodules and mammography

Jan Kybic

2020

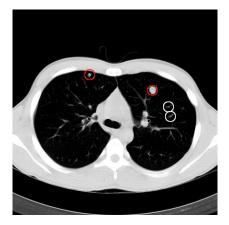
Murphy et al: A large-scale evaluation of automatic pulmonary nodule detection in chest CT using localfeatures and k-nearest-neighbor classification

Key points

- Nodule (pre-cancer) detection
- Handcrafted features, simple classifier

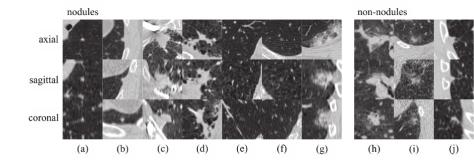
#### Pulmonary nodules

- small bright spots on thoraci CT (often round but not always)
- mostly benign but some may lead to cancer
- $\blacktriangleright$  earlier detection  $\rightarrow$  better prognosis



Martin Dolejší

## Nodule examples



#### Nelson trial data

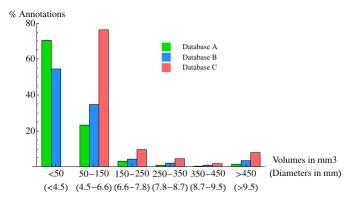
- ▶  $512 \times 512$  pixels,  $306 \sim 860$  slices
- two observers to mark nodules
- small nodules (diameter < 3mm) may not be marked</p>
- if several scans per patient the earliest chosen
- $\blacktriangleright$  TP = within 7 pixels
- Datasets: A all scans, B all scans with at least one big nodule, C - only big nodules

#### Table 1

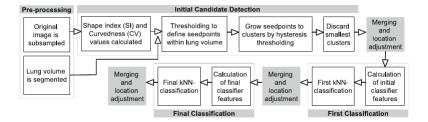
Statistics on the number of scans in the three databases.

	А	В	С
#Scans before checks	1588	1158	1158
#Scans with lung segmentation failures	53	37	37
#Scans after removing failures	1535	1121	1121
#Scans in training set	722	580	580
#Scans in test set	813	541	541
#Nodules in final training set	1369	1763	760
#Nodules in final test set	1525	1688	768

## Size distribution

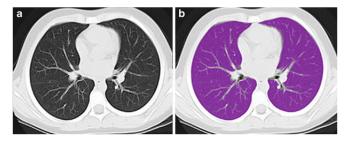


#### Flowchart



### Preprocessing

- downsampling to  $256 \times 256$
- Iung segmentation



from Jill Stein et al. DOI: 10.1007/s00247-016-3686-8

#### Shape index and curvedness

$$ext{SI} = rac{2}{\pi} \arctan\left(rac{k_1+k_2}{k_1-k_2}
ight)$$
 $ext{CV} = \sqrt{k_1^2+k_2^2}$ 

Principal curvatures  $k_1, k_2$ 

- minimum and maximum curvatures of the isosurface
- can be calculated from Hesssian with  $\sigma = 1$

#### Shape index

1 local maximum = bright blob, 0.5 bright tubular structure, 0 saddle/flat...

## Seed point detection

#### Cluster formation

#### Table 2

Initial seed thresholds.

Value	Upper threshold	Lower threshold
SI	1	0.8 (near pleural surface)
CV	1	0.9 (elsewhere) 0.3

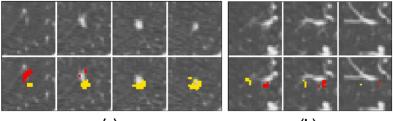
#### Table 3

Hysteresis thresholds.

Value Upper threshold		Lower threshold	
SI	1	0.7 (near pleural surface)	
CV	1.3	0.2	

- Cluster merging (distance < voxels). Small objects (<15 voxels) discarded.
- Candidate location = highest locally averaged intensity

# Merging examples



(a)

(b)

Successive axial slices. (a) TP, (b) FP.

## False positive reduction

- Classify candidates
- ► *k*-NN classifier
- Two stages (15 and 50 features)
- Final stage on full resolution images
- Feature selection (Sequential forward floating selection)
- Operating point: sensitivity 90%

## Training set generation

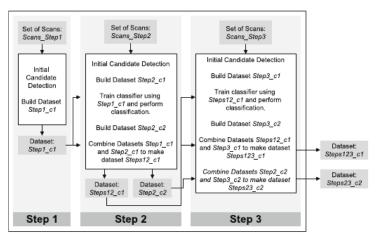


Fig. 4. Generation of training sets.

Subsample N class, N:P ratio 3:1, preserving pdf.

# Features (1)

#### Table 4

The features calculated for the first kNN classifier. See text in Section 2.3.2.

ID	Description			
Features of the	Features of the voxel cluster			
a1	Cluster size (number of voxels)			
a2	Compactness1, ClusterSize			
a3	Compactness2, ClasterSize max dim*			
a4	Ratio max_dim:min_dim			
a5	Ratio max_dim:med_dim			
a6	Ratio Amed: Amax where Amax, Amed and Amin are the eigenvalues for the eigenvectors of the clu			
a7	Ratio Amin: Amax			
a8	Sphericity, mun_chister_voxels_in_sphere_S vot_sphere_S where sphere_S is a sphere at the candidate location with r			
a9	Ratio Sphericity:r			
Features of vox	Features of voxels in spherical kernels at the candidate location			
a10-a18	On grey-values over spherical kernels K: Average, Median, Standard-Deviation			



#### Table 5

The features calculated for the final kNN classifier. See text in Section 2.3.3

ID	Description	Notes
Features of the voxel cluste	27	
b1-b9	Features a1-a9 as described in Table 4	
b19	min_dim = min_(dim_i)	dim <sub>i</sub> = width in di
b20	$max_dim = max_i(dim_i)$	dim <sub>i</sub> = width in di
Features of voxels in spher	ical kernels at the candidate location	
b10-b18	Features a10-a18 as described in Table 4	
b21-b26	On grey-values over spherical kernels K: Min, Max	Halfsizes of K: 1 (
b27-b36	On SI over spherical kernels K: Average, Median, Std-Dev, Min, Max	Halfsizes of K: 3 (
b37-b46	On CV over spherical kernels K: Average, Median, Std-Dev, Min, Max	Halfsizes of K: 3 (
Features calculated on ran	domly chosen points on a spherical surface around the candidate location.	
b47-b76	Features of Gradient orientation values: Average(Avg), Median,	30 points on sphe
	Max, Min, Std-Dev, Coefficient of	b66), 50 points or
	Variation, Ratio Max:Min, Ratio Std-Dev:Median, Ratio	
	Median:Avg, Ratio Median:Max	
b77-b106	Features of Gradient magnitude values: Average(Avg), Median,	30 points on sphe
	Max, Min, Std-Dev, Coefficient of Variation, Ratio Max:Min, Ratio	b96), 50
	Std-Dev:Median, Ratio Median:Avg, Ratio Median:Max	points on sphere
Features of voxels in the co	indidate segmentation	
b107-b115	Features a1-a9 as described in Table 4 but calculated this time ov	er the segmented v
b116	min_dim = min_(dim_i)	
b117	$max_dim = max_i(dim_i)$	
b118-b122	On grey-values over segmented voxels: Average, Median, Std-Dev,	Min, Max
b123-b127	On SI of segmented voxels: Average, Median, Std-Dev, Min, Max	
b128-b132	On CV of segmented voxels: Average, Median, Std-Dev, Min, Max	
b133	Ratio Num segmented voxels: Num ROI voxels	
b134	Ratio {Distance from candidate location to the farthest point in th {Number of voxels in the segmentation}	e segmentation}:
Other features		
b135	Posterior probability of being a true nodule from the first classical	tion step

### Results

#### Table 7

Results for experiments on database A.

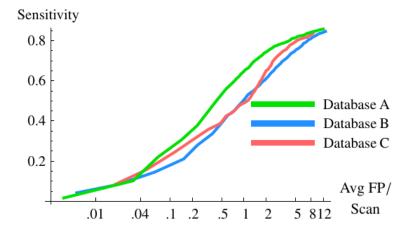
Number of Scans Number of annotations	813 1525	
	Sensitivity	FP per scan
After initial candidate detection After first classification After final classification	97.2% 92.3%	649.0 77.3
<ul> <li>At around 4 FP per scan</li> </ul>	80.0%	4.2

#### Table 9

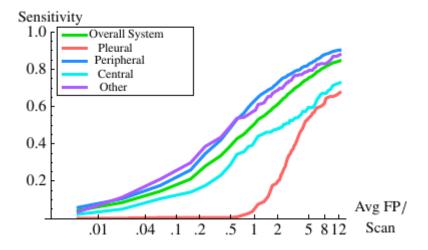
Results for experiments on database C.

Number of scans Number of annotations	541 768	
	Sensitivity	FP per scan
After initial candidate detection	98.2%	752.1
After first classification After final classification	92.2%	51.2
– At around 4 FP per scan	77.7%	4.2

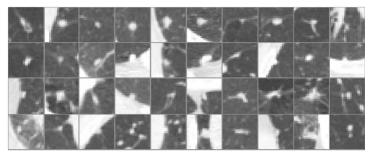
## FROC curve



# FROC by location

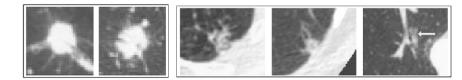


## Example nodules

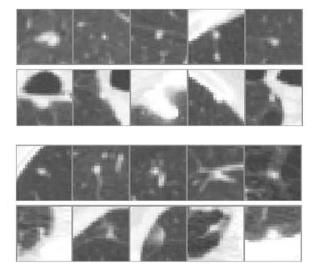


top row - easy detections (p>0.9), bottom row - not detected (p<0.35)

# Missed nodules



# False positives



Setio et al: Pulmonary Nodule Detection in CT Images: False Positive Reduction Using Multi-View Convolutional Networks. IEEE TMI 2016

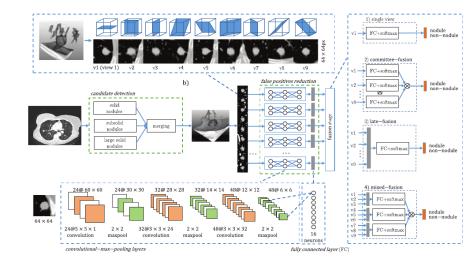
#### Key points

- Nodule detection from 3D CT
- Candidate detection (by 3 specialized detection)
- CNN for FP reduction
- $\blacktriangleright$  2D patches/planes + fusion

#### Datasets

- LIDC 1018 scans, 888 retained (ignore thick-slice cases), 4 observers
- ANODE09 55 scans, 2 observers,
- DLCST 612 scans, 2 observers, 898 nodules
- considered nodules > 3mm

#### Flowchart



#### Candidate detection

- Solid nodules Murphy's detector (shape index, curvedness, thresholding, clustering)
- Subsolid nodules (pure and part-solid ground-glass) thresholding, morphological opening, connected components, segmentation
- Large nodules (>10mm, possibly attached to pleura) lung segmentation, rolling-ball segmentation smoothing, density thresholding, multi-scale morphological opening

1/100001

DETECTION SENSITIVITY OF CANDIDATE DETECTION ALGORITHMS

Total number of CT scans: 888

Total number of nodules: 1,186

Candidate detection	Detected nodules	Sensitivity (%)	False Positives (FPs)	FPs per scan
Solid	1,016	85.7	292,413	329.3
Subsolid	428	36.1	255,027	287.2
Large solid	377	31.8	41,816	47.1
Combined set	1,120	94.4	543,160	611.7
Reduced set	1,106	93.3	239,041	269.2

## Patch classification

#### Patch extraction

 $\blacktriangleright~50\times50mm,~64\times64pixels,$  nine planes CNNs

- ▶ 3 convolutional layers, 3 max-pooling layers
- testing 1 s per scan on a GPU

# Fusion

#### Committee fusion

- FC layer + softmax + product rule
- each stream trained separately

#### Late fusion

- concatenate FC layer outputs
- FC layer + softmax

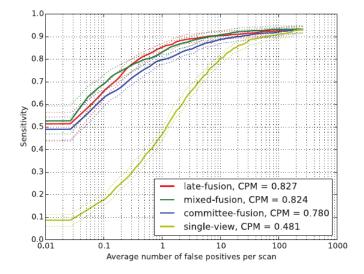
#### Mixed fusion

- group 9 patches into 3 groups of orthogonal views
- contenate within group (as in late fusion)
- FC layer + softmax + product rule (as in committee fusion)

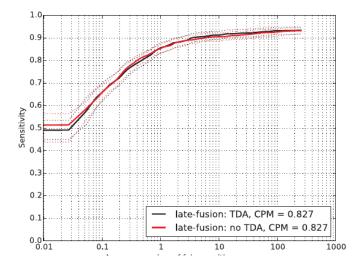
# Training

- Negative training data pruning
  - preliminary classification by existing algorithms
  - eliminate candidates with low nodule probability
- 5-fold cross-validation on LIDC (3/5 training, 1/5 validation, 1/5 testing)
- cross-entropy error
- RMSprop
- random initialization
- dropout regularization
- augmentation of nodules (shift, scaling)
- random upsampling of nodules for training
- test-data augmentation (scaling)

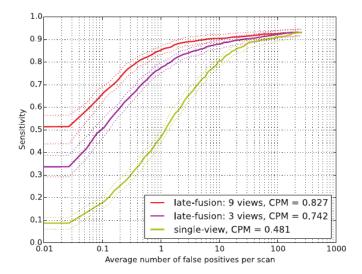
## FROC fusion



#### FROC test augmentation



## FROC number of views



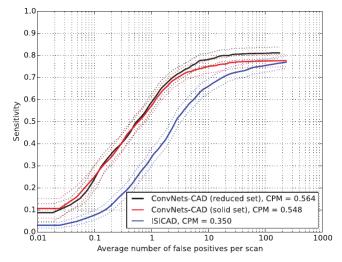
## LIDC results

#### TABLE III

PERFORMANCE BENCHMARK OF CONVNETS CONFIGURATIONS ON LIDC-IDRI DATASET. THE BEST SCORE FOR EACH PERFORMANCE METRIC IS MARKED IN BOLD. FOR COMPARISON PURPOSES, THE PERFORMANCE OF THE COMBINED ALGORITHMS [3], [5], [27] IS INCLUDED

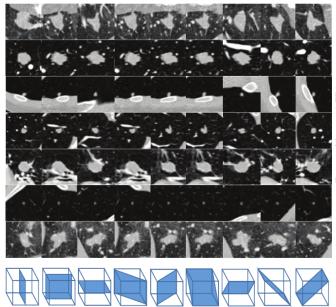
Configuration	Number of views	AUC	СРМ
combined algorithms	-	0.969	0.573
single-view	1	0.969	0.481
committee-fusion	3	0.981	0.696
	9	0.987	0.780
late-fusion	3	0.987	0.742
	9	0.993	0.827
mixed-fusion	3*3	0.996	0.824

## DLCST results



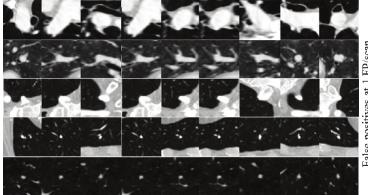
sensitivity 76.5% at 6 FPs/scan, which is 94% of the true candidate nodules

# True positives



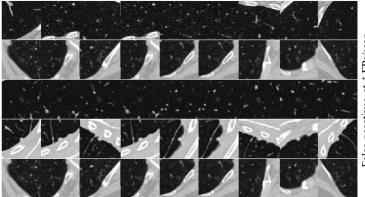
Irue positives at 1 FP/scan

# False positives



False positives at 1 FP/scan

# False negatives



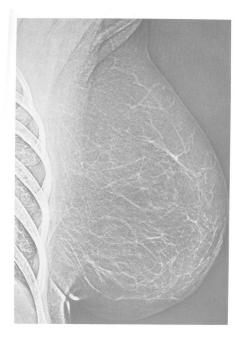
False negatives at 4 FPs/scan

Kooi: Large scale deep learning for computer aided detection of mammographic lesions. MIA 2017

#### Key points

- detect lesions from mammographs
- candidate detection learned
- classification to reduce FPs
- combine deep and manual features

# Mammography



#### Data overview

#### Table 1

Overview of the data. Pos refers to the amount of malignant lesions and neg to the amount of normals.

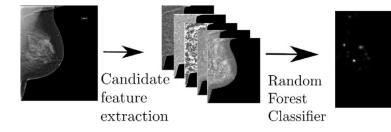
	Cases		Exams		Images		Candidates	
	Pos	Neg	Pos	Neg	Pos	Neg	Pos	Neg
Train	296	6433	358	11,780	634	39,872	634	213,450
Valid.	35	710	42	1247	85	4218	85	19,460
Test	124	2064	124	5317	271	18,182	271	180,777

### Candidate detection

5 features based on Gaussian derivative kernels

- center of mass
- size
- spiculation (spikes or points)
- random forest classifier
- training data
  - positive samples from annotated lesions
  - negative samples randomly
- test time apply RF to all pixels

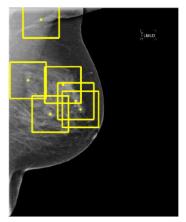
# Candidate detection examples



## Patches for CNN



(a) Illustration of segmentations for the reference system.



(b) Illustration of extracted patches for the CNN.

# Baseline (classical system)

mass segmentation by dynamic programming in polar coordinates

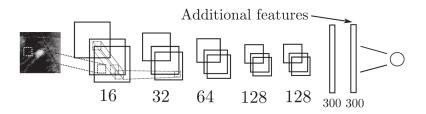
#### 74 features:

- candidate detector features,
- contrast features,
- texture features,
- geometry features
- context features (rest of the breast)
- patient features

RF classifier (also tested SVM, gradient boosted tree, MLPs)

### CNN

- ReLU
- Binary cross-entropy loss
- Data augmentation (scale, translation, flip)
- scaled-down VGG model (6 layers with 3 × 3 kernels, 2 × 2 max-pooling), FC layer with 300 neurons
- learned features also extracted and a classifier trained
- positive samples randomly oversampled
- deep networks tried but did not improve the results



### Feature importance

#### Table 3

Overview of results of the CNN combined with individual feature sets.

Feature group added to CNN	AUC	CI
CNN Only	0.929	[0.897, 0.938]
Candidate detector	0.938	[0.919, 0.955]
Contrast	0.931	[0.91, 0.949]
Texture	0.933	[0.912, 0.950]
Geometry	0.928	[0.907, 0.946]
Location	0.933	[0.913, 0.950]
Context	0.934	[0.914, 0.952]
Patient	0.929	[0.908, 0.947]
All	0.941	[0.922, 0.958]

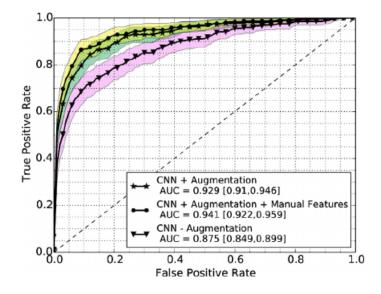
#### Dataset size importance

#### Table 4

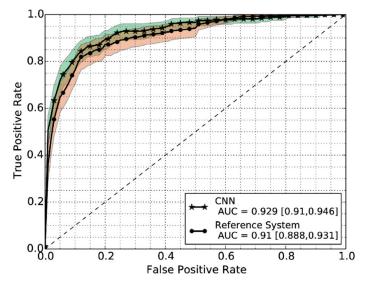
AUC values obtained when training the network on subsets of malignant lesions in the training set, keeping the same amount of normals.

Data Augmentation	60%	All
With	0.842	0.929
Without	0.685	0.875

#### Augmentation importance

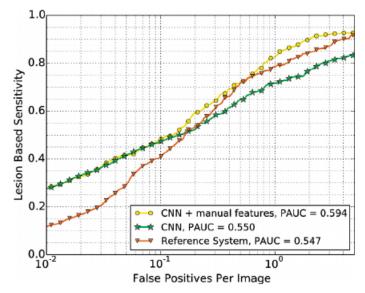


### CNN versus baseline



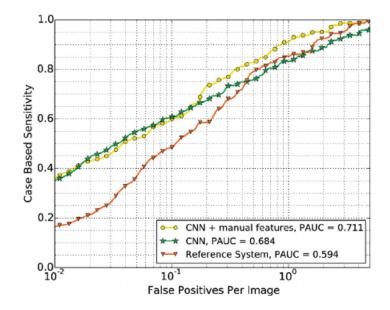
excluding context, location, patient information

# CNN versus baseline

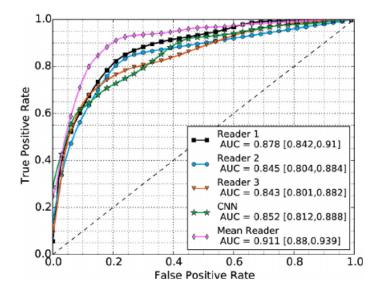


including context, location, patient information

#### CNN versus baseline Case FROC

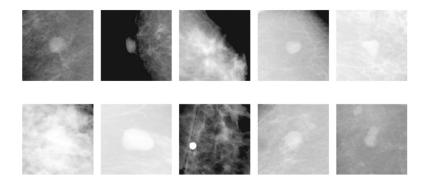


#### CNN versus human readers

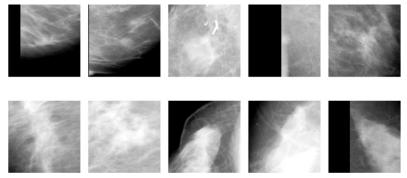


no significant difference between CNN and any readers difference with mean of readers significant

# False positives



### False negatives



#### mostly very large lesions