

Magnetic resonance imaging

Part 1

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¹<http://www.cis.rit.edu/htbooks/mri/>

Introduction

MRI physics

Nuclear spin

Spectroscopy

Excitation

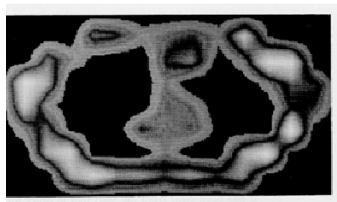
Relaxation

Bloch equation

First human MRI

MR přístroje

První obraz člověka (1977)



MRI scanner

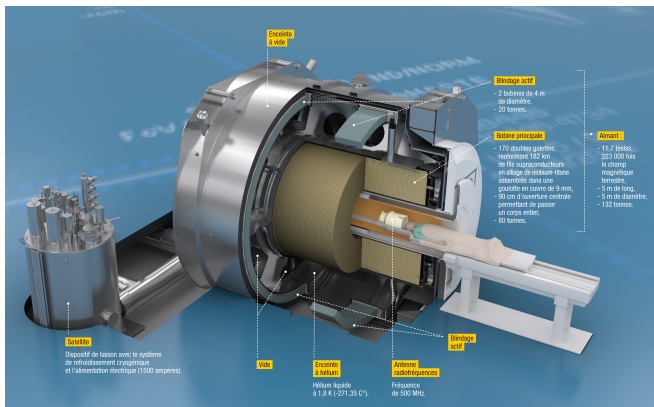
solenoid, closed-bore magnet



Permanentní magnety - architektura „OPEN“

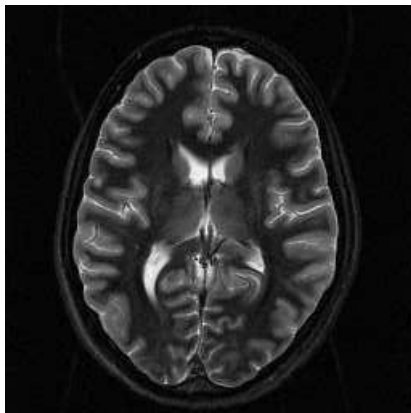


11.7T MRI



MRI – Example

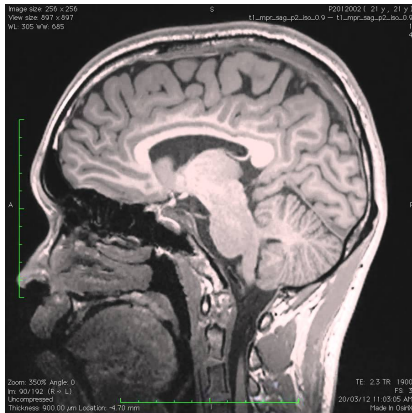
Brain slice:



all 3D

MRI – Example

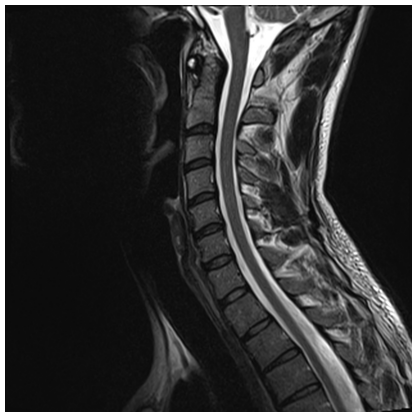
Brain slice:



all 3D

MRI – Example

Spine:



all 3D

MRI – Example



all 3D

MRI principles

1. Insert object (subject) into a strong magnetic field.
2. (Repeatedly) send a radio-frequency impuls.
3. Spins are excited and then relax to equilibrium.
4. Receive and record emitted radio-frequency waves.
5. Reconstruct image from data.
6. Remove the object (subject) from the magnetic field.

Brief history of MRI

- 1946 – Felix Bloch, Edward Purcell, independent discovery
- 1950–1970 — NMR, spectroscopic analysis
- 1971 — Raymond Damadian, tissue relaxation times differ
- 1973 — Hounsfield, CT (showed demand for medical imaging)
- 1973 — Paul Lauterbur, tomographic MRI (backprojection)
- 1975 — Richard Ernst, Fourier MRI
- 1977 — Peter Mansfield, echo-planar imaging (EPI), later 30 ms/slice

Brief history of MRI (2)

- 1980 — Edelstein, whole-body MRI (3D), 5 min/slice
- 1986 — whole-body MRI, 5 s/slice
- 1986 — MRI microscopy, resolution $10\ \mu\text{m}$
- 1987 — beating heart imaging
- 1987 — MRA angiography without contrast agents, blood flow
- 1992 — functional MRI, brain mapping

Nobel prizes

- 1952 — Felix Bloch, Edward Purcell, physics, discovery
- 1991 — Richard Ernst, chemistry, Fourier MRI
- 2003 — Paul Lauterbur, Peter Mansfield, medicine, MRI in medicine

Numbers related to MRI

- About 40000 MRI scanners worldwide
- About 20 examination per day per scanner
- 110 scanners in Czech Republic in 2018
- One scanner costs 10 ~ 100 mil. Kč (millions of EUR)
- One examination 5 ~ 20 tis. Kč (hundreds of EUR)

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Spin

- Human body: fat and water. 63 % hydrogen (10 % by mass)
- Hydrogen nucleus = proton.
- Proton has a property called a **spin** (besides a mass and charge), related to angular momentum.
- Non-zero spin particles behave like small magnets → MRI signal

Nuclear spin

- Free electrons, protons, and neutrons have a spin of 1/2
- Spins may pair and compensate
- Nuclear spin I is a multiple of 1/2
- $I \neq 0 \Rightarrow$ (small) magnet,

$$\text{magnetic moment } \boldsymbol{\mu} \quad \|\boldsymbol{\mu}\| = \gamma \hbar \sqrt{I(I+1)} \quad \left[\frac{\text{N} \cdot \text{m}}{\text{T}} \right]$$

$$\text{torque} \quad \boldsymbol{\tau} = \boldsymbol{\mu} \times \mathbf{B} \quad [\text{N} \cdot \text{m}]$$

γ — gyromagnetic constant $\left[\frac{\text{rad}}{\text{s} \cdot \text{T}} \right]$ or $\left[\frac{\text{MHz}}{\text{T}} \right]$

$\hbar = \frac{h}{2\pi}$ — reduced Planck constant

$$h \approx 6.626 \cdot 10^{-34} \text{ J} \cdot \text{s}$$

Isotopes useful for MRI

- Only unpaired spins ($I \neq 0$) are useful for MRI
- Total nuclear spin — no easy rule
- Even atomic number Z (number of protons) and even mass number A (total number of protons and neutrons) $\Rightarrow I = 0$ (^{12}C , ^{16}O)
- Most abundant isotopes for even Z have $I = 0$
- Isotopes with $I \neq 0$ are often
 - rare isotopes (1.11% for ^{13}C)
 - biologically rare elements
 - give small signal

Biological abundance of elements

(by count)

Element Abundance [%]

H	63	
O	26	main isotope ^{16}O with zero spin
C	9.4	main isotope ^{12}C with zero spin
N	1.5	
P	0.24	
Ca	0.22	
Na	0.041	

Abundance of MRI active isotopes

by count

Isotope	Abundance [%]
^1H	99.985
^2H	0.015
^{13}C	1.11
^{14}N	99.63
^{15}N	0.37
^{23}Na	100
^{31}P	100
^{39}K	93.1
^{43}Ca	0.145

Abundance of MRI active isotopes

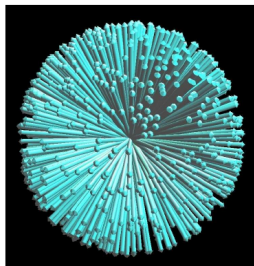
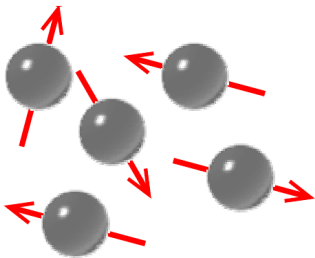
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Practical MRI exists for

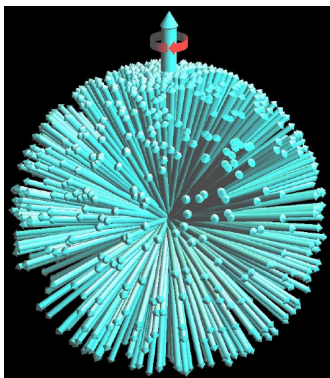
- ^1H — most often used, strongest signal, best quality
- ^{19}F , ^{23}Na , ^{31}P ... — mostly research

Spins in magnetic field



magnetic induction $B_0 = 0$, random orientation

Spins in magnetic field

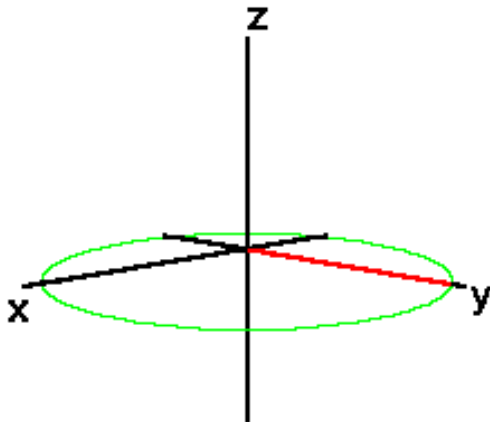


$B_0 \neq 0$ (around 0.1 ~ 10 T needed)

- Spin packet
- Spins will partially align (on the average)
- Macroscopically observable magnetisation $\mathbf{M} = \sum \mu$

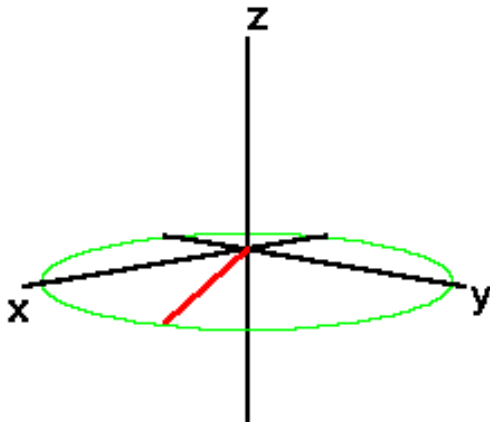
Precession

- For B_0 along z axis
- \mathbf{M} rotates around z axis
- $\boldsymbol{\tau} = \boldsymbol{\mu} \times \mathbf{B}$



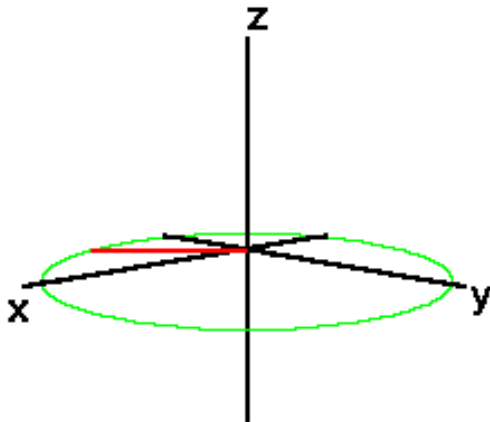
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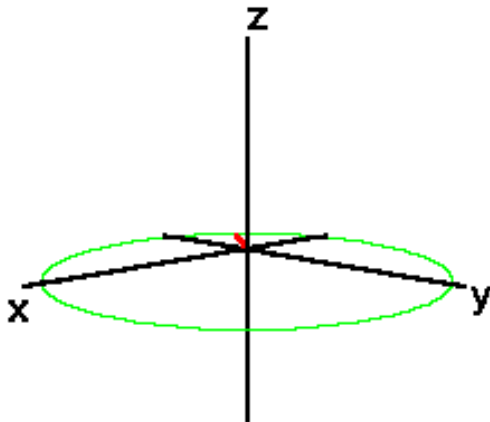
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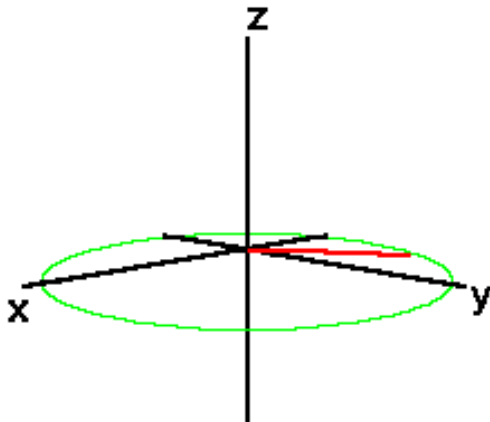
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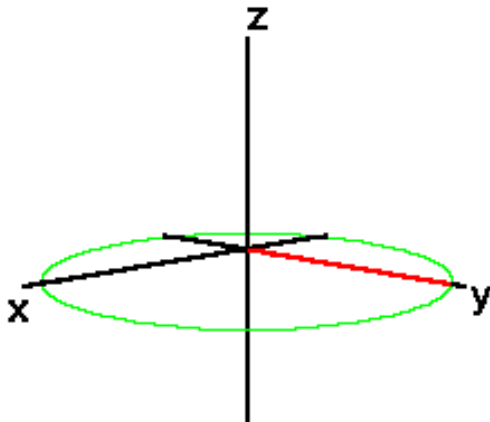
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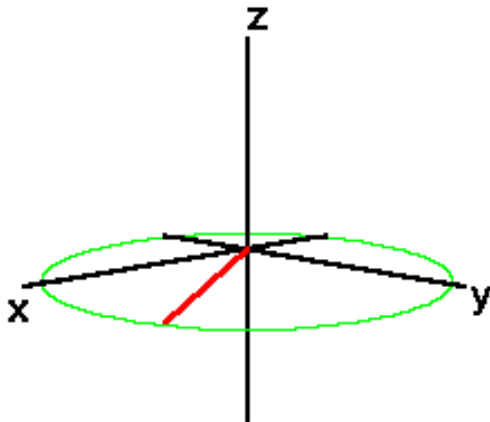
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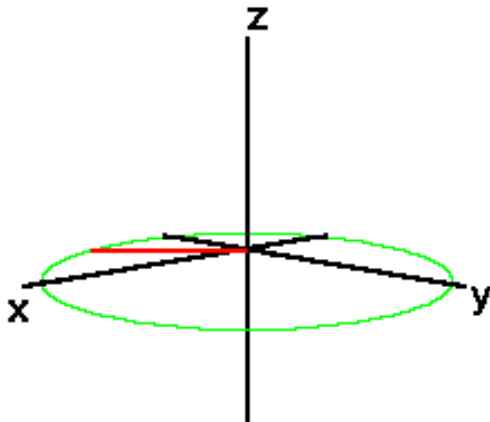
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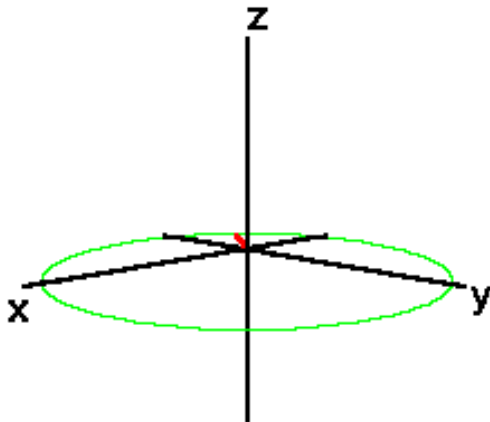
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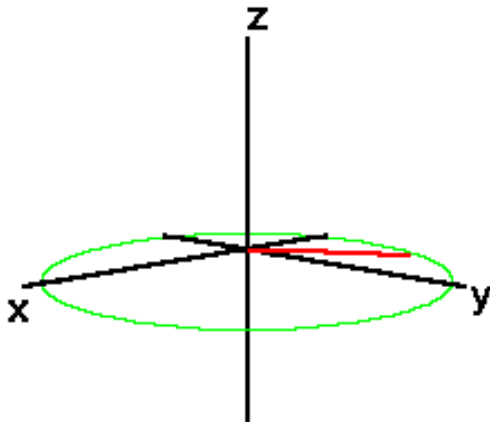
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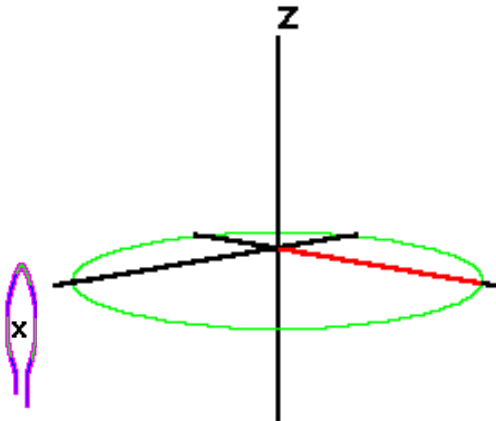
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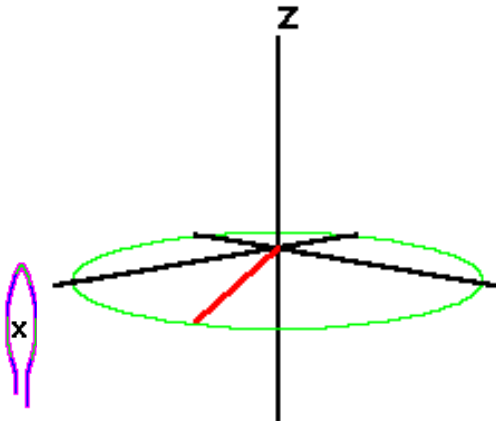
RF signal

Precession in the xy plane gives measurable RF signal.



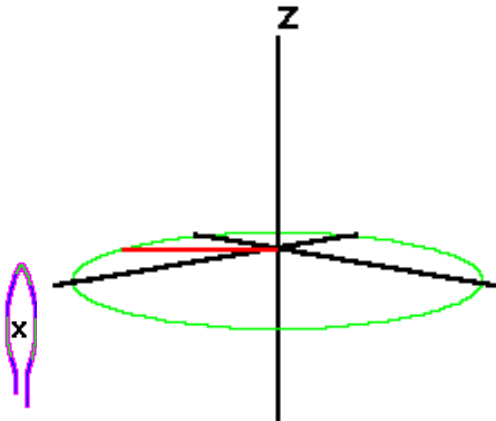
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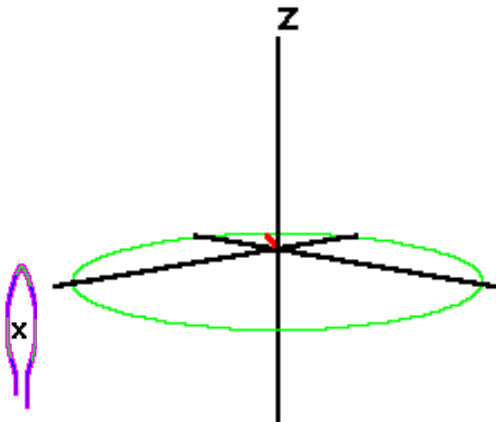
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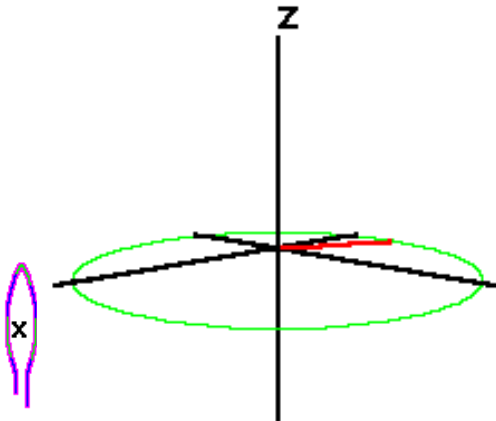
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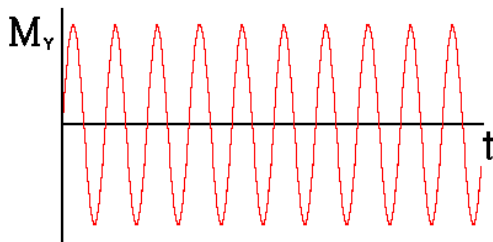
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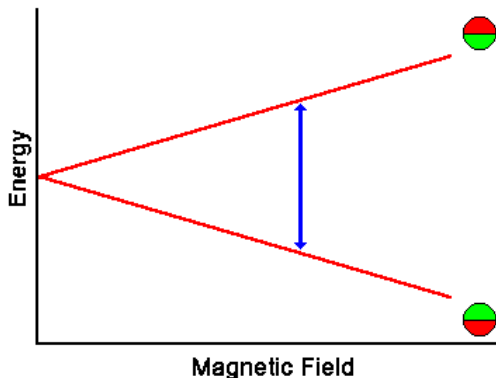


Larmor frequency

$$f = \gamma B$$

- B [Tesla] magnetic field intensity
- γ gyromagnetic constant
- Pro ^1H , $\gamma = 42.58 \text{ MHz/T}$
- f is a frequency of:
 - the precession
 - the received signal
 - the excitation signal

Energy diagram



$$f = \gamma B, \quad E_p = hf, \quad \Delta E \propto \gamma B$$

- low (parallel) and high (antiparallel) orientations
- For H , typically $f = 15 \sim 80$ MHz.
- Energy difference \sim signal amplitude

Boltzmann statistics

For a closed (non-quantum) system in thermal equilibrium:

- Number of low-energy spins N^-
- Number of high-energy spins N^+

$$\frac{N^-}{N^+} = e^{-\frac{\Delta E}{kT}}$$

Boltzmann constant $k = 1.3805 \cdot 10^{-23}$

Temperature T [K]

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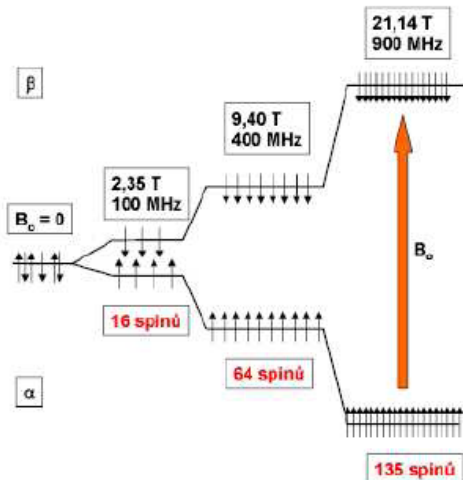
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Temperature T [K]

- MRI signal $\propto \|\mathbf{M}\| \propto N^- - N^+$
- low T , high $B \rightarrow$ high signal
- high T , low $B \rightarrow$ low signal

Boltzmann statistics example

Je-li stav β obsazen 10^6 spinů, stav α obsahuje $10^6 + \text{přebytek}$.



příklad ^1H :

$$f = 400 \text{ MHz}$$

$$B = 9.5 \text{ T}$$

$$\Delta E = 3.8 \cdot 10^{-5} \frac{\text{Kcal}}{\text{mol}}$$

$$\frac{N^-}{N^+} = 1.000064 \sim 64 \text{ ppm}$$

→ very low SNR in MRI.

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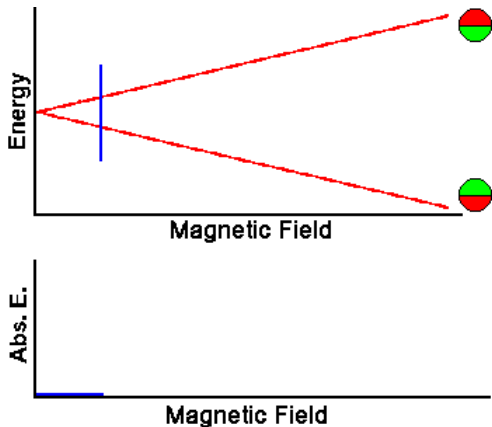
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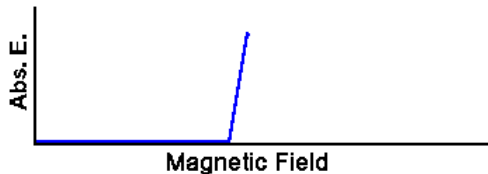
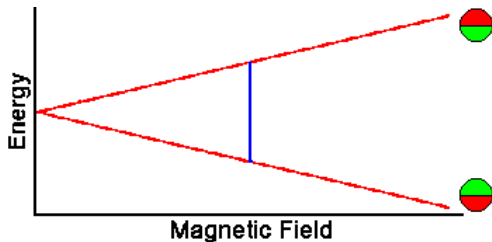
Continuous wave NMR (1)

- Constant frequency
- Variable magnetic field
- Measuring absorbed energy



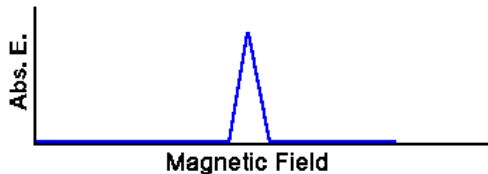
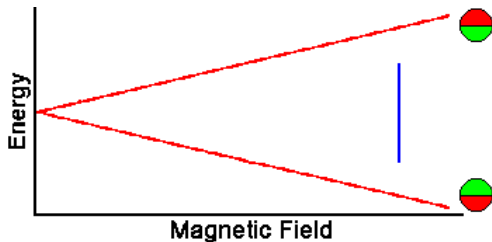
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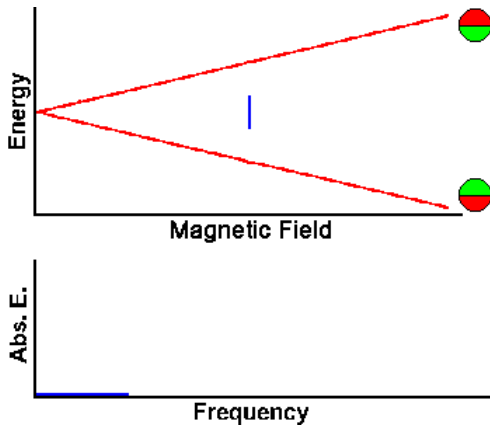
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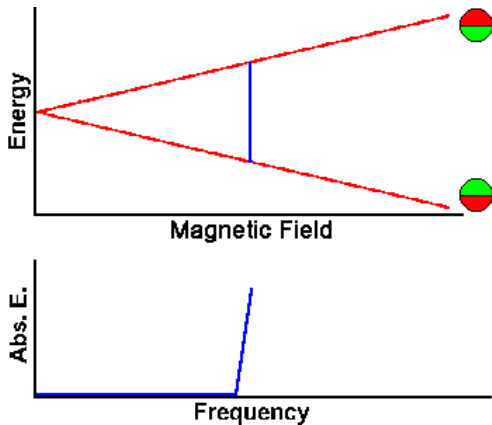
Continuous wave NMR (2)

- Constant magnetic field
- Variable frequency frekvence
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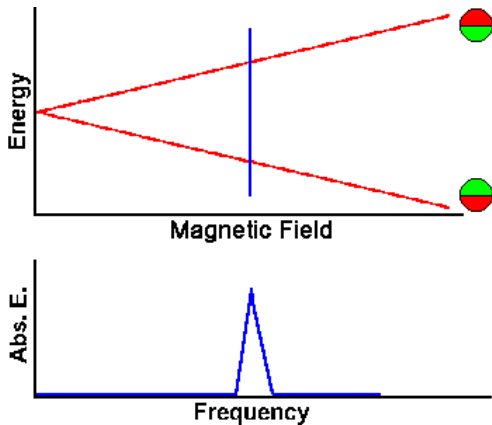
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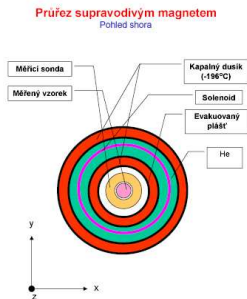


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NMR spektroskopie

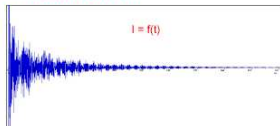


Fyzikální základy - pokračování

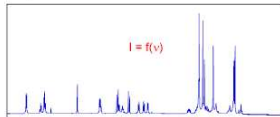
FID (pokračování)

- V reálném vzorku je mnoho spinových systémů, jejichž frekvence jsou odlišné od frekvence \mathbf{B}_1 (*carrier frequency*). Protože jsme efektivně excitovali všechny tyto spiny, dostaneme kombinaci signálů a různé frekvenci

Free Induction Decay (FID):



- Po zpracování Fourierovou transformací dostaneme:



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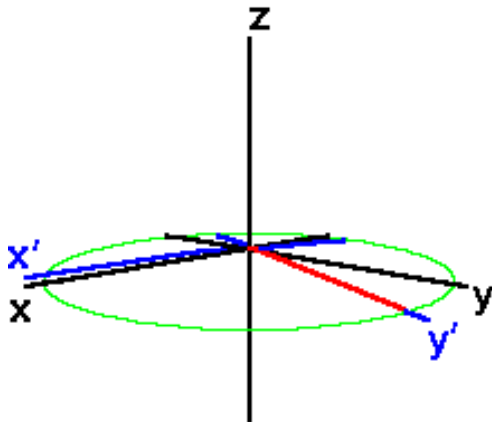
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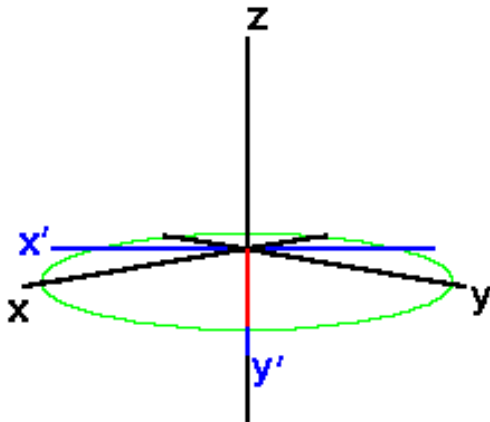
Rotating frame of reference

... rotates around z with Larmor frequency f



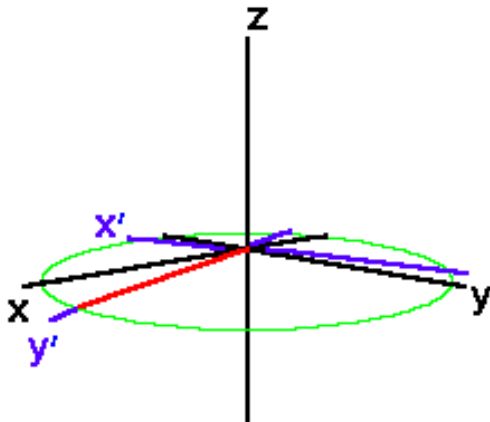
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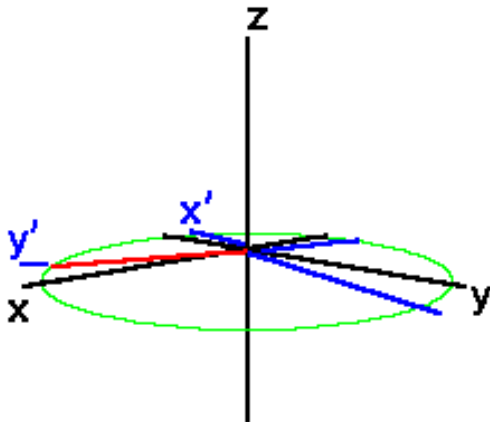
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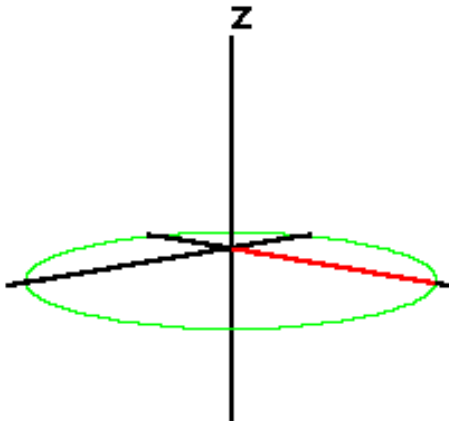
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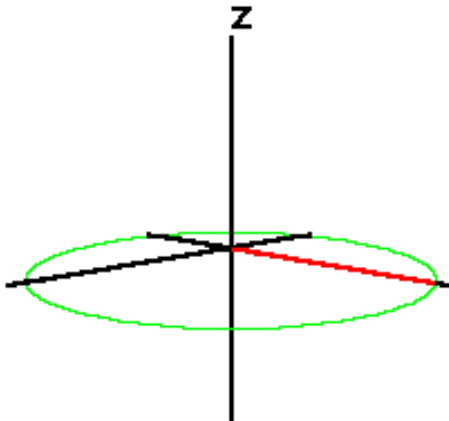
Rotating frame of reference (2)

μ rotating with frequency f appears stationary



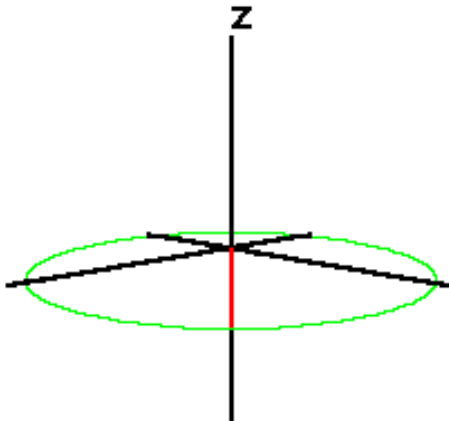
Rotating frame of reference (3)

μ rotating faster than f appears rotating in the same direction



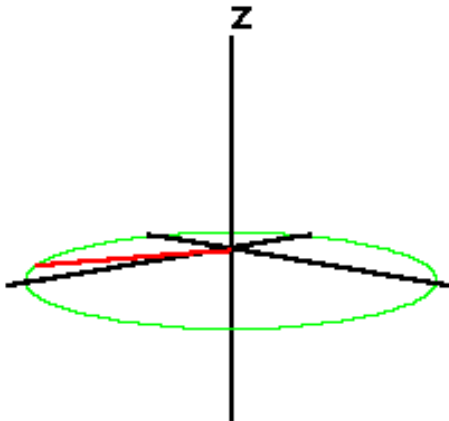
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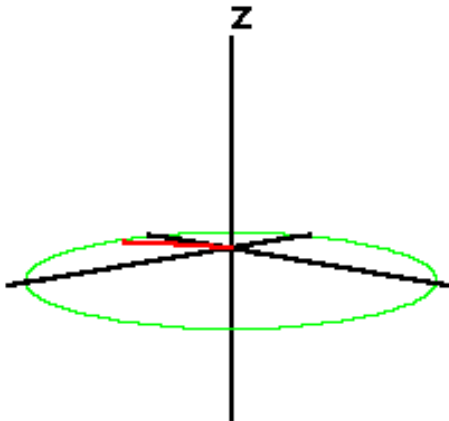
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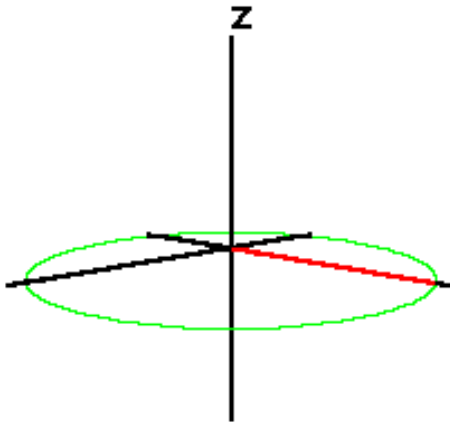
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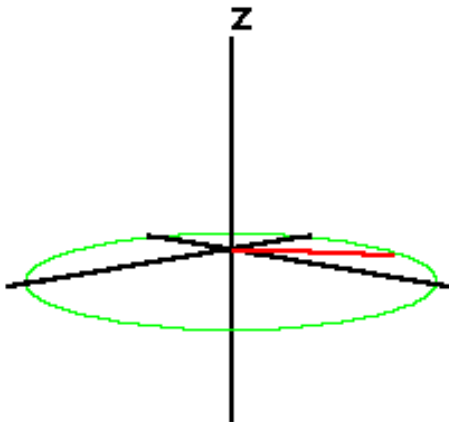
Rotating frame of reference (4)

μ rotating slower than f appears rotating in the opposite direction



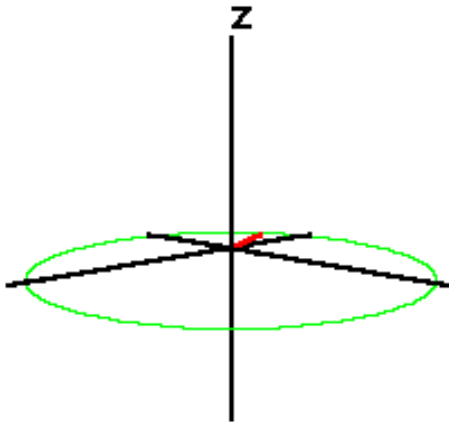
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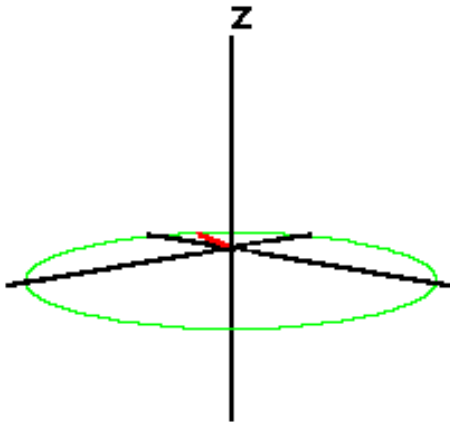
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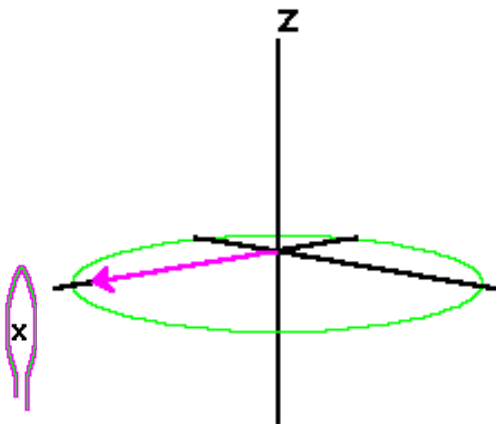
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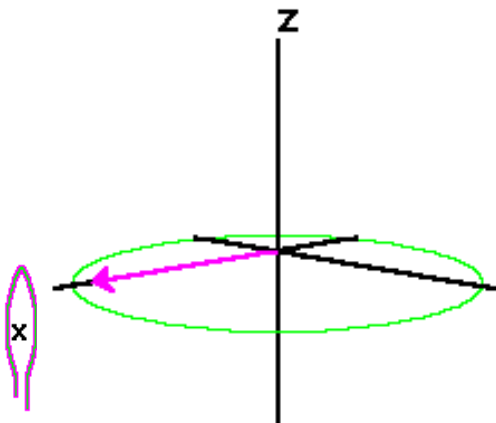
Electromagnetic excitation

- Coil around x axis creates magnetic field along x



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- Alternating current with frequency f creates alternating field \mathbf{B}_1



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- \mathbf{B}_1^- has frequency $2f$ there, far from the resonance, can be neglected.

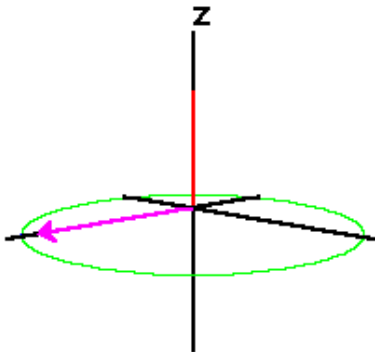
Electromagnetic excitation

- Coil around x axis creates magnetic field along x
- Alternating current with frequency f creates alternating field \mathbf{B}_1
- \mathbf{B}_1 can be decomposed to constant amplitude $\mathbf{B}_1^+ + \mathbf{B}_1^-$, rotating around z with frequency $\pm f$
- \mathbf{B}_1^+ is stationary in the rotating frame of reference.
- \mathbf{B}_1^- has frequency $2f$ there, far from the resonance, can be neglected.
- \rightarrow alternating field \mathbf{B}_1 will appear stationary along x' in the rotating frame of reference.

Magnetization vector flip (rotation)

- RF impuls at Larmor frequency f (*at resonance*), with amplitude B_1 and duration τ
- \rightarrow magnetization \mathbf{M} will turn around B_1 ($= x'$) by angle

$$\alpha = 2\pi\gamma\tau B_1 \quad \text{flip angle}$$

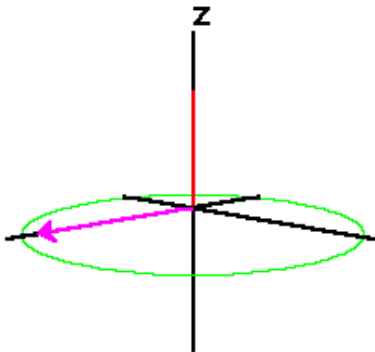


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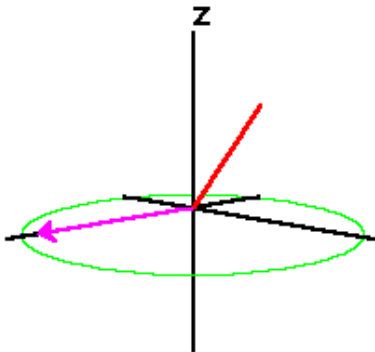


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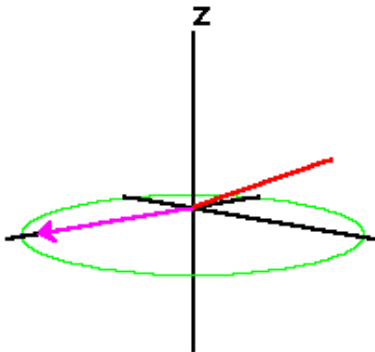


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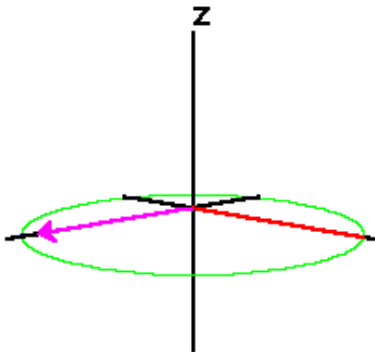


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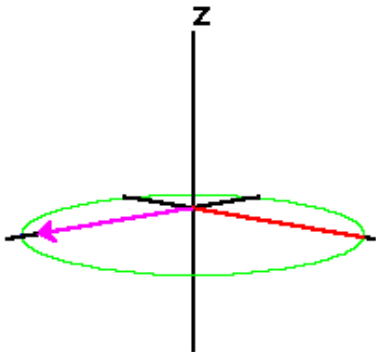


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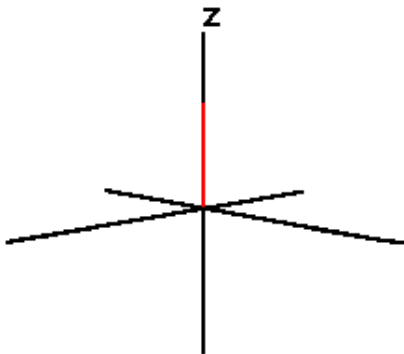
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- **90° impuls** — turns \mathbf{M} from z to y'
- **180° impuls** — turns \mathbf{M} from z to $-z'$



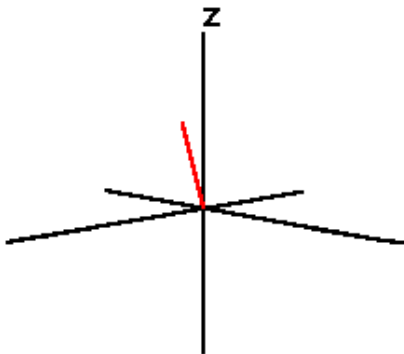
Magnetization vector flip (rotation)

- in the fixed coordinate system. . .



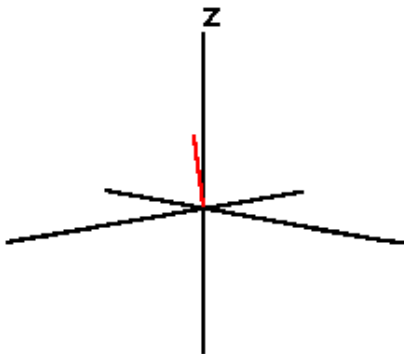
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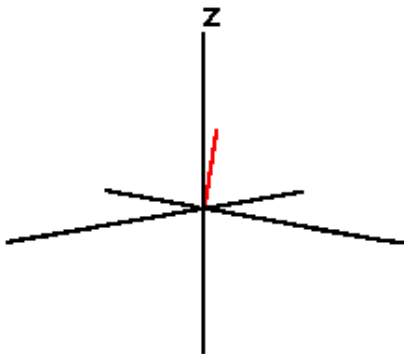
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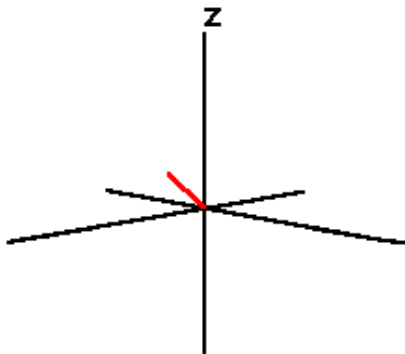
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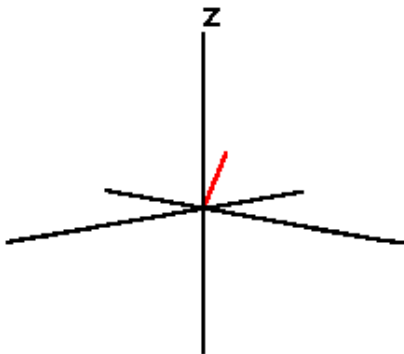
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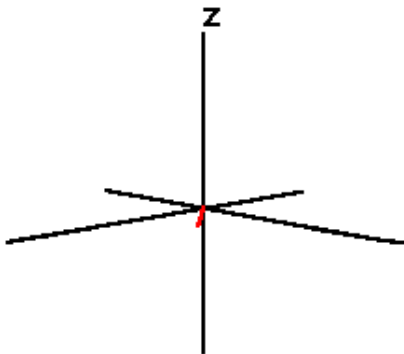
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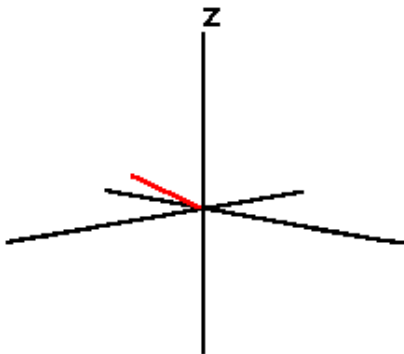
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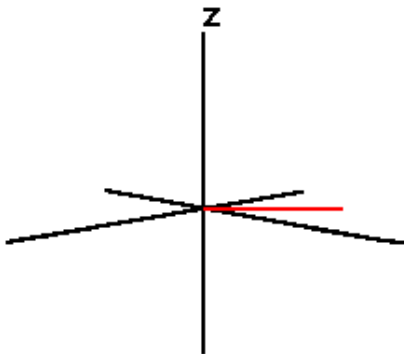
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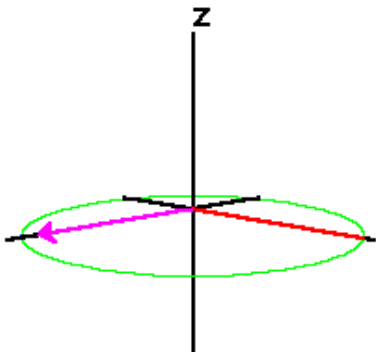
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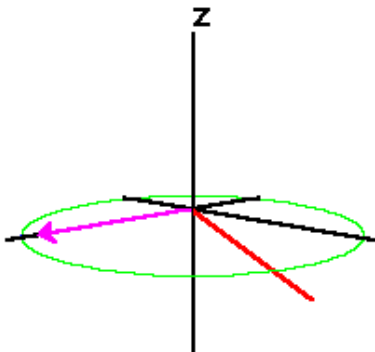
Magnetization vector flip (2)

- Magnetization is turned by angle α from any initial position
- e.g. 180° impuls for $\mathbf{M} \parallel y'$



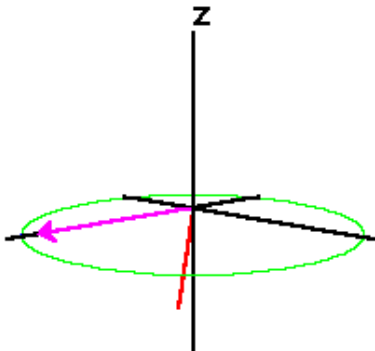
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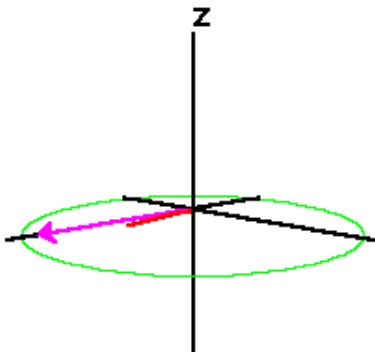
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Introduction

MRI physics

Nuclear spin

Spectroscopy

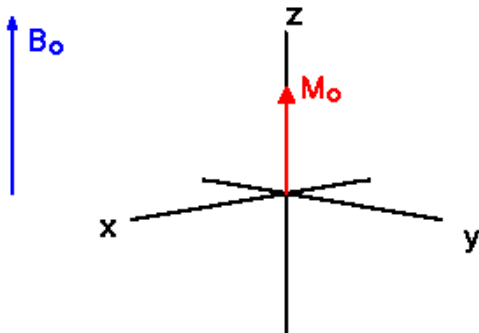
Excitation

Relaxation

Bloch equation

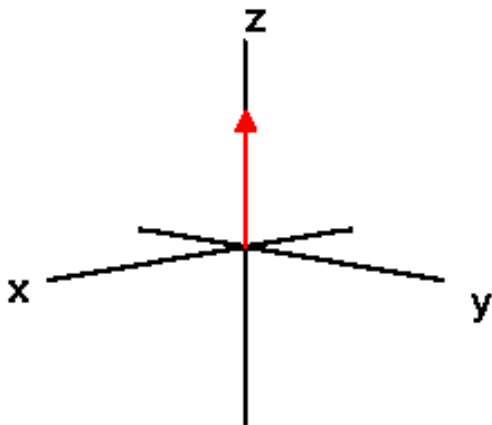
T_1 relaxation

- In equilibrium, $\mathbf{M} = M_0 \mathbf{e}_z$, $M_z = M_0$



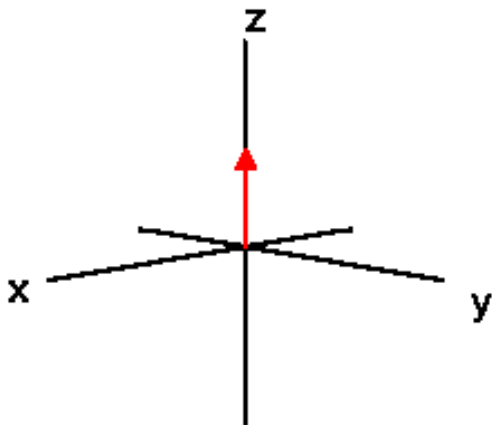
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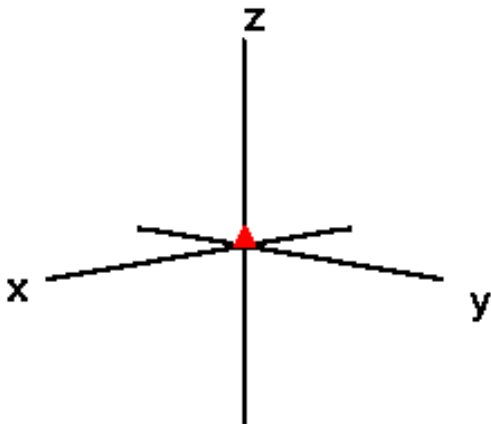
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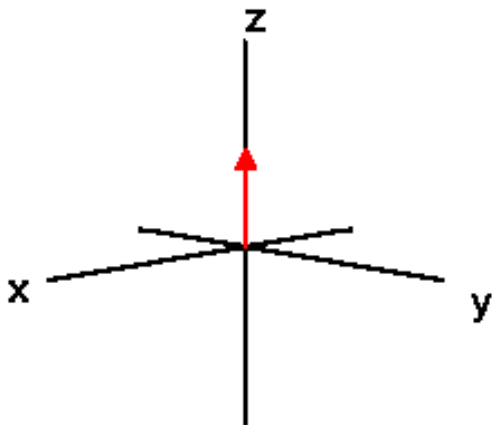
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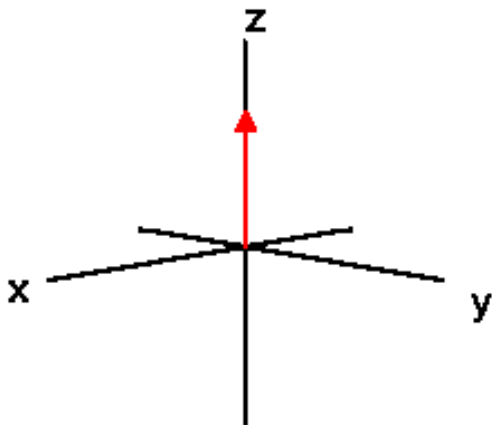
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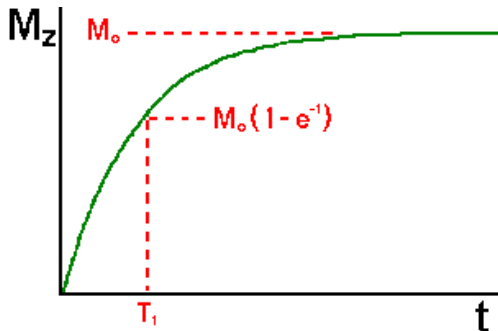
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T_1 relaxation (2)

After the pulse M_z returns to equilibrium.

$$M_z = M_0 \left(1 - e^{-\frac{t}{T_1}} \right)$$

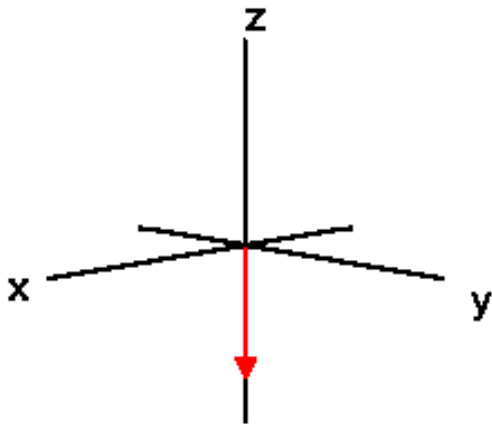


T_1 — spin-lattice relaxation time
(mřížková relaxační časová konstanta)
the energy is dissipated into the lattice as heat

T_1 relaxation (3)

A stronger/longer pulse may cause e.g. $M_z = -M_0$.

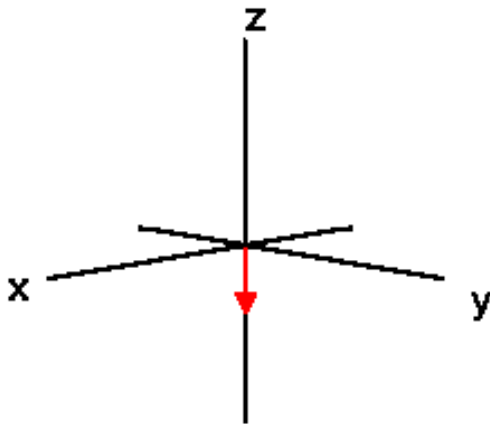
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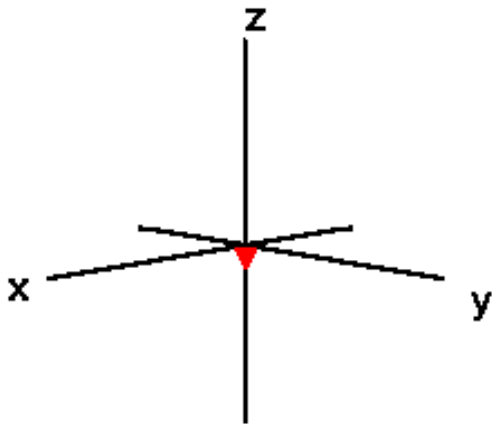
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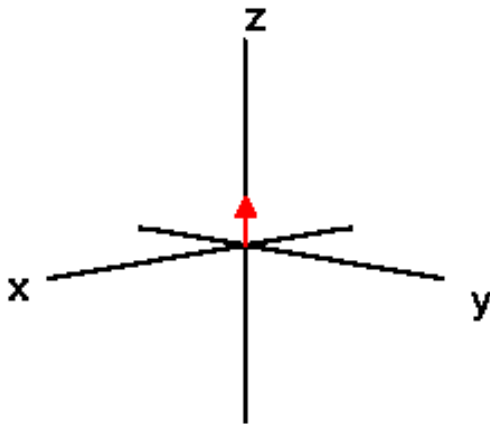
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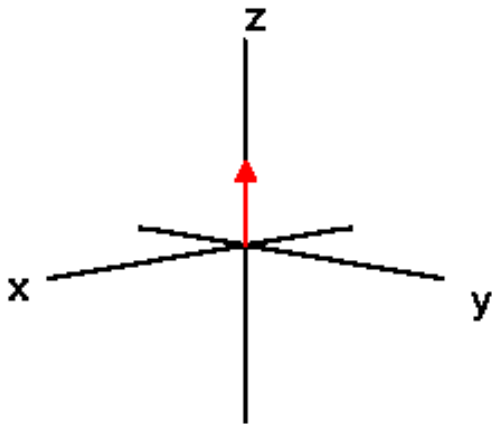
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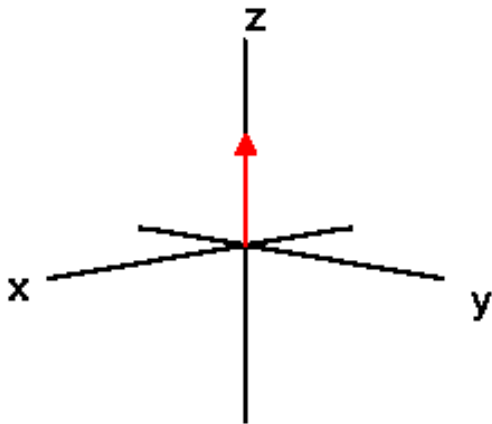
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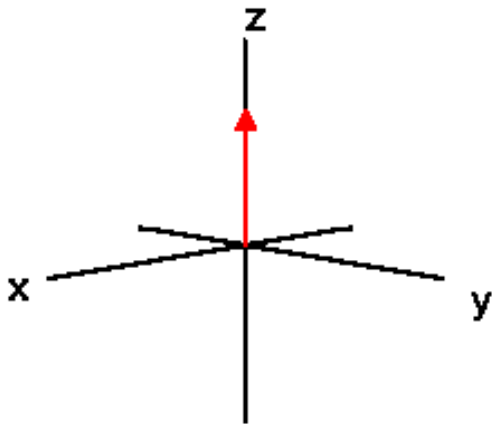
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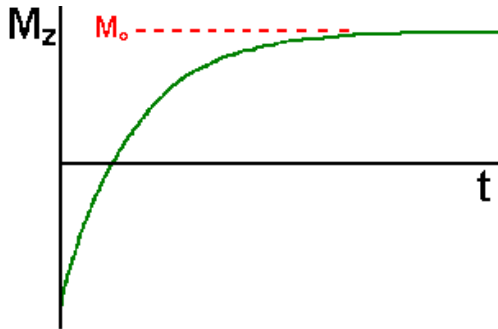
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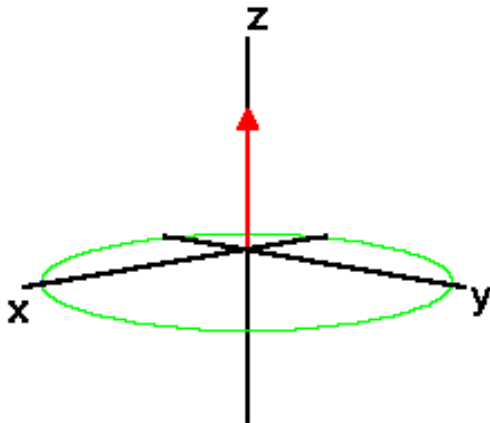
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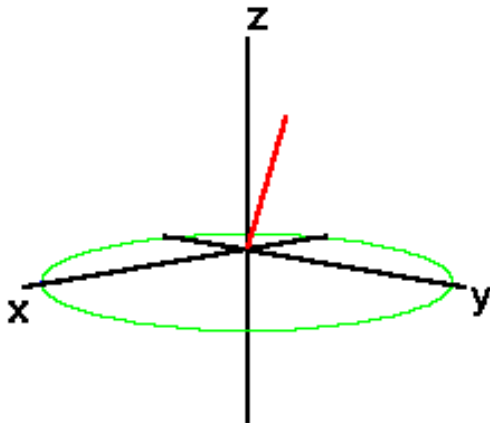
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- Once \mathbf{M} turns away from the z axis...



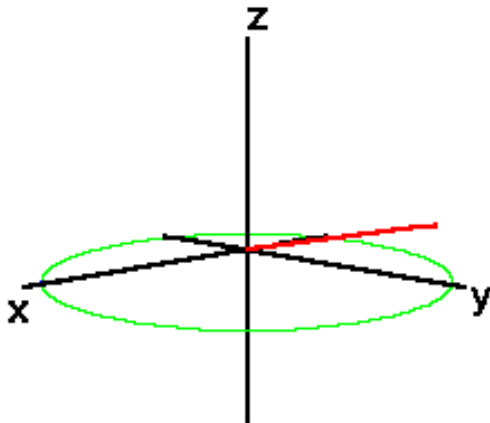
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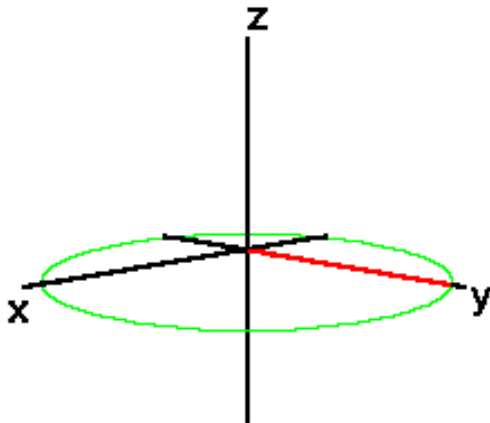
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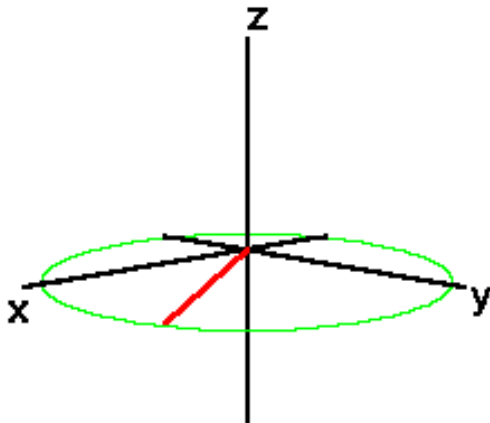
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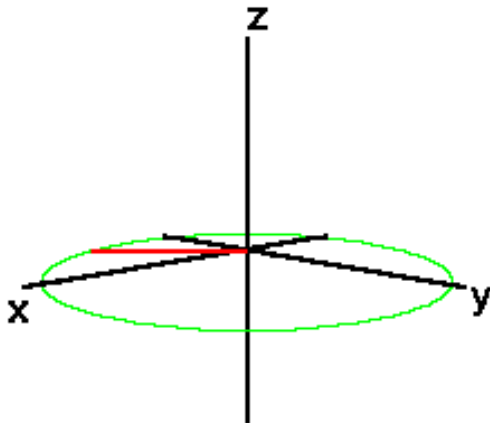
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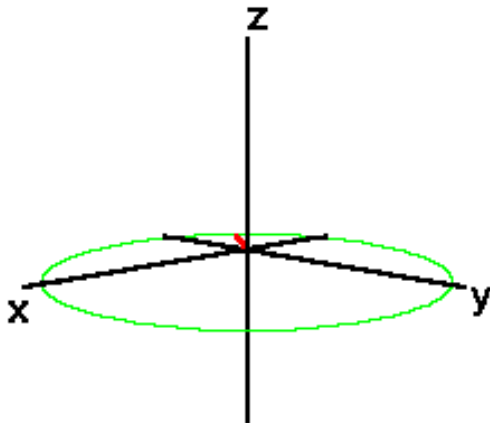
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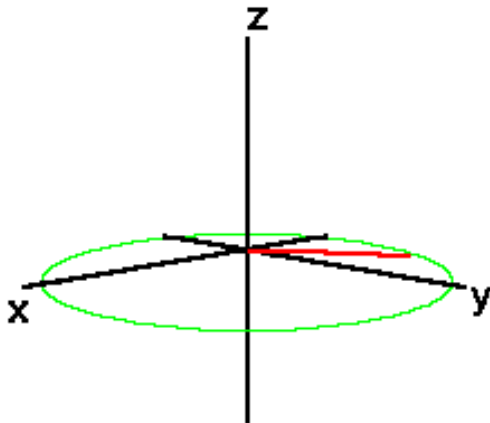
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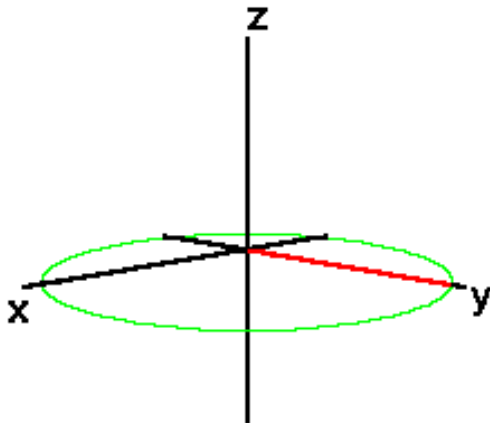
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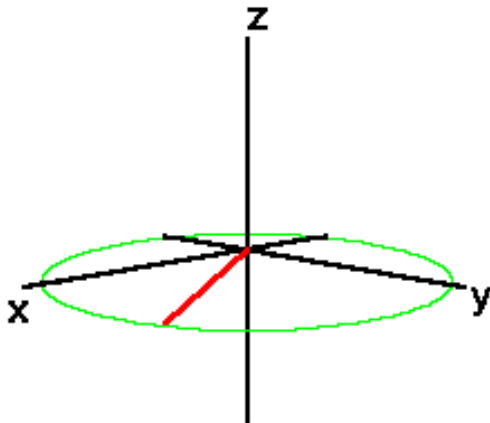
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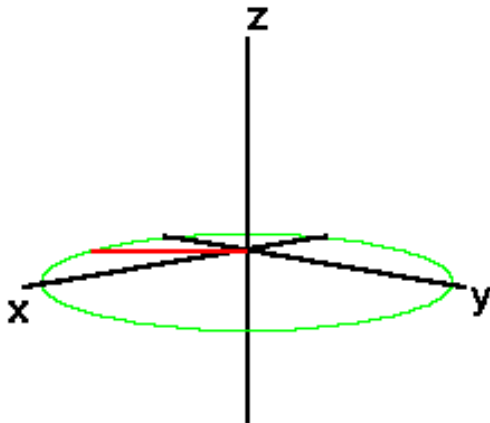
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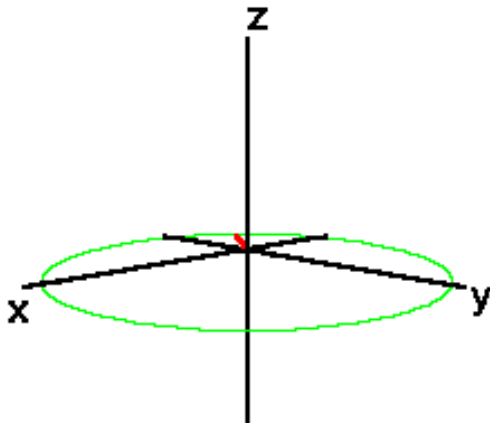
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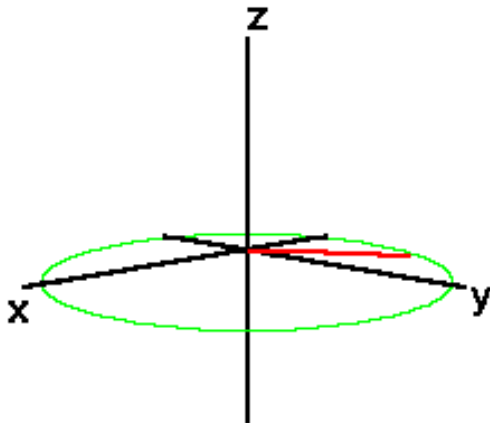
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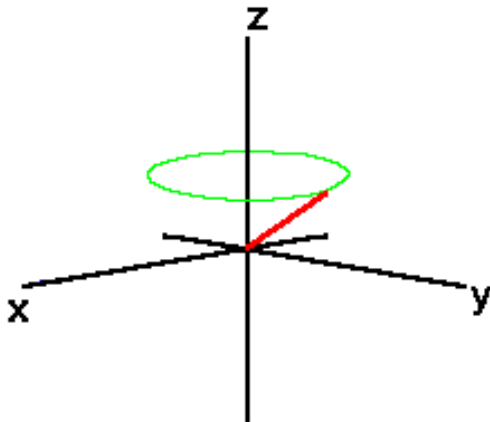
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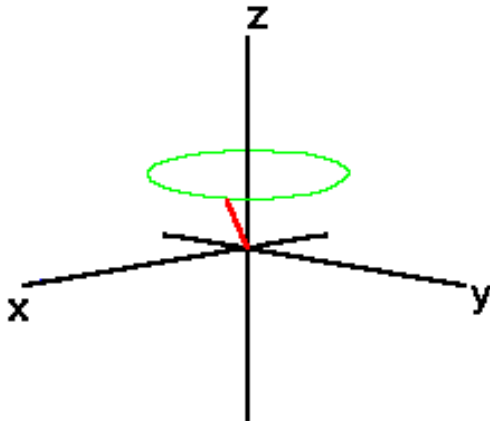
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M does not have to be completely in the xy plane



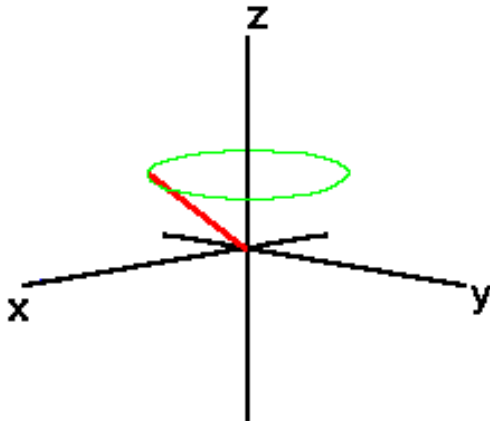
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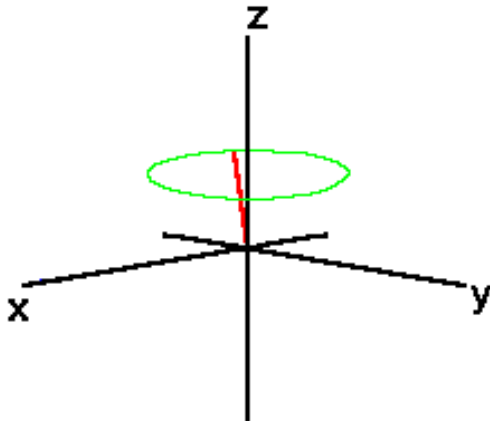
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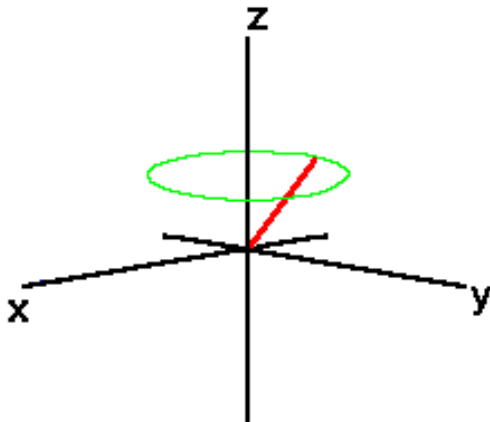
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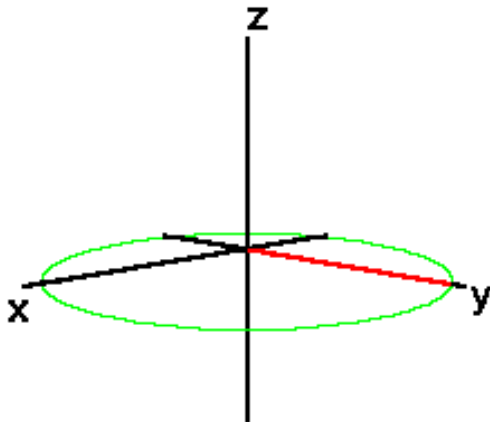
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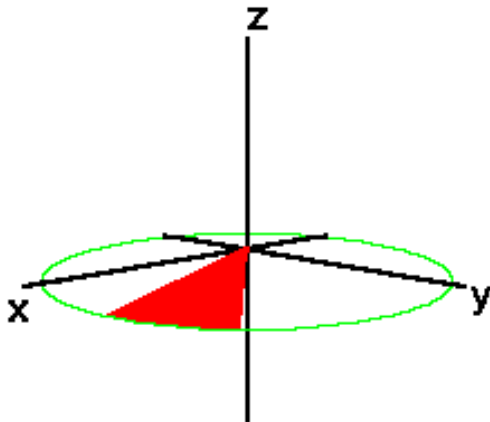
T_2 relaxation

Every spin has a slightly different $f \rightarrow$ desynchronization



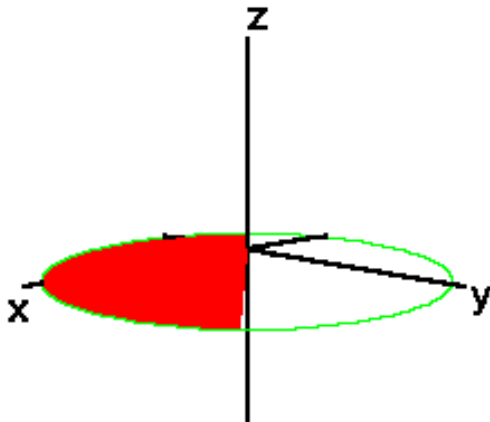
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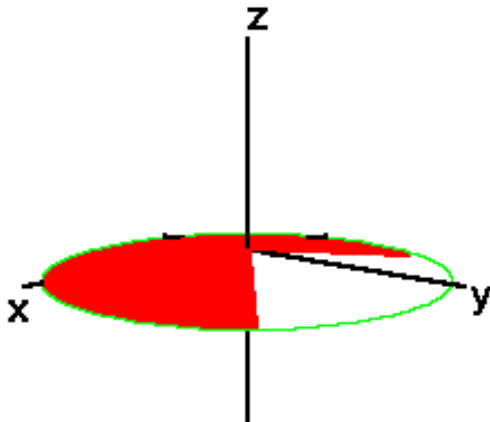
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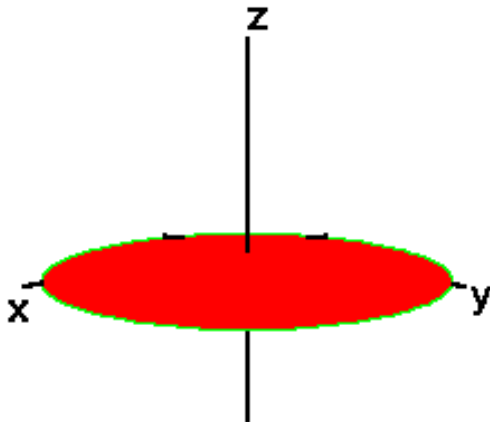
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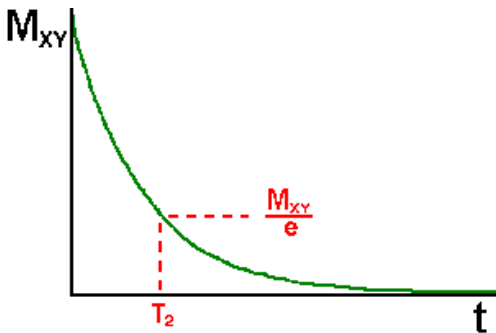
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T_2 relaxation (2)

Transversal magnetization M_{xy} decreases

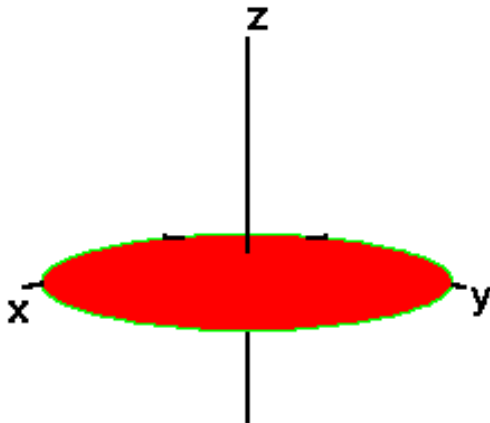
$$M_{xy} = M_{xy0}e^{-\frac{t}{T_2}}$$



T_2 — spin-spin relaxation time
(spinová relaxační časová konstanta), $T_2 < T_1$

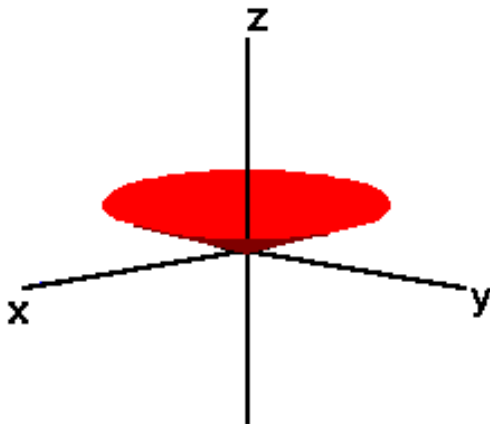
T_1 and T_2 relaxations

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- At the same time (but more slowly) M_z returns to M_0 .



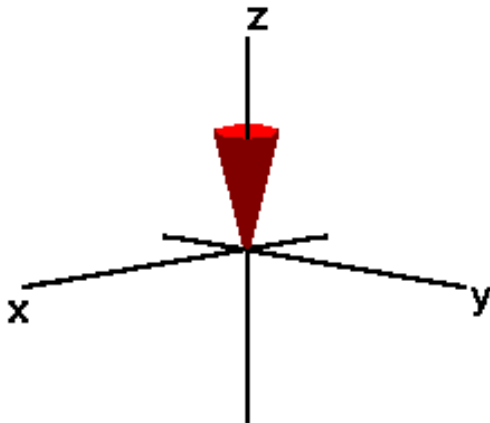
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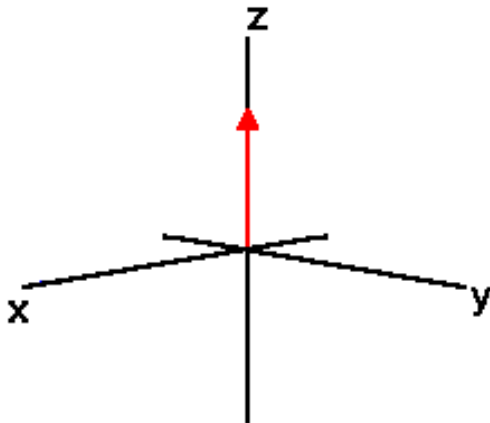
T_1 and T_2 relaxations

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T_1 and T_2 relaxations

- Transversal magnetization M_{xy} decreases
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Reasons for the T_2 relaxation

- Molecular interaction (T_2)
- Inhomogeneity of the magnetic field (T_2^{inhom})

Combined time constant T_2^* :

$$\frac{1}{T_2^*} = \frac{1}{T_2} + \frac{1}{T_2^{\text{inhom}}}$$

Other factors influencing relaxation

- Molecular movement (because of the magnetic field inhomogeneity)
- Temperature
- Viscosity

Typical relaxation times

tissue	1.5 T		3 T	
	T_1 [ms]	T_2 [ms]	T_1 [ms]	T_2 [ms]
fat	260	80	420	100
muscle	870	45	1300	40
brain (gray matter)	900	100	1600	100
brain (white matter)	780	90	900	70
liver	500	40	800	34
cerebrospinal fluid	2400	160	4100	500

Reported values differ significantly.

Introduction

MRI physics

Nuclear spin

Spectroscopy

Excitation

Relaxation

Bloch equation

Bloch equation

$$\frac{d\mathbf{M}}{dt} = \gamma \mathbf{M} \times \mathbf{B}$$

where \mathbf{B} is the total magnetic field ($\mathbf{B}_0 + \mathbf{B}_1$).

Bloch equation (2)

$$\frac{d\mathbf{M}}{dt} = \gamma \mathbf{M} \times \mathbf{B}$$

substituting for \mathbf{B} , add losses and use the rotating frame of reference

$$\begin{aligned}\frac{dM_{x'}}{dt} &= (\omega_0 - \omega)M_{y'} - \frac{M_{x'}}{T_2} \\ \frac{dM_{y'}}{dt} &= -(\omega_0 - \omega)M_{x'} + 2\pi\gamma B_1 M_z - \frac{M_{y'}}{T_2} \\ \frac{dM_z}{dt} &= -2\pi\gamma B_1 M_{y'} - \frac{M_z - M_{z0}}{T_1}\end{aligned}$$

where $\omega_0 = 2\pi f_0 = 2\pi\gamma B_0$, ω is the spin rotation frequency.