Funkční zobrazování a mapování mozku fMRI

J. Kybic, J. Hirsch[1], J. Hornak[2], M. Bock, J. Hozman, a další[3]

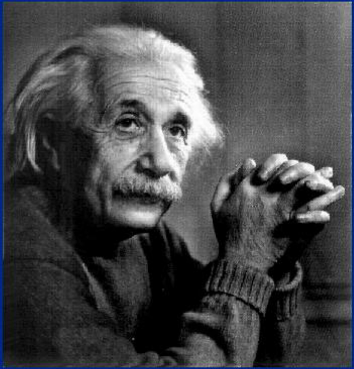
2008–2020

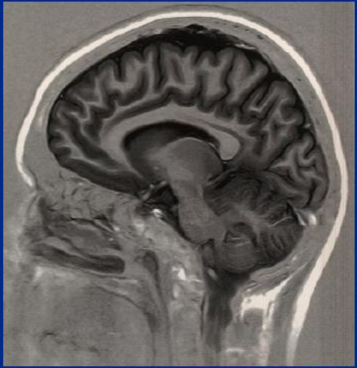
[1] `http://www.fmri.org`

[2] `http://www.cis.rit.edu/htbooks/mri/`

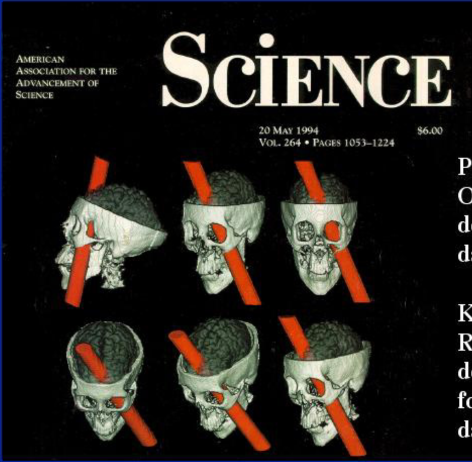
[3] `http://www.biac.duke.edu/education/courses/fall04/fmri/`

A New View of Brain and Mind: Functional Neuroimaging





Columbia fMRI

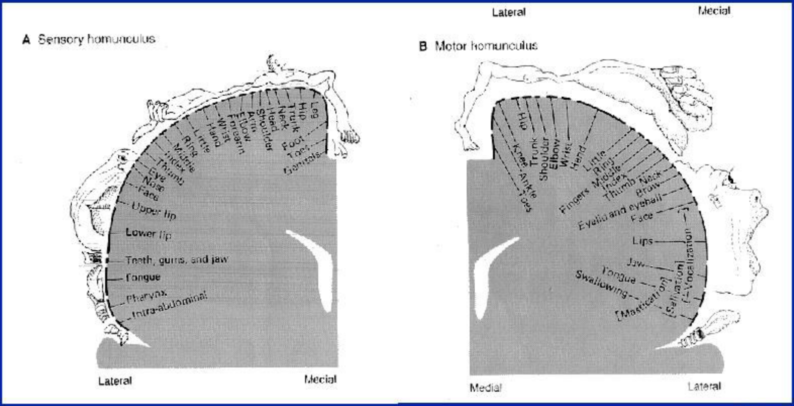


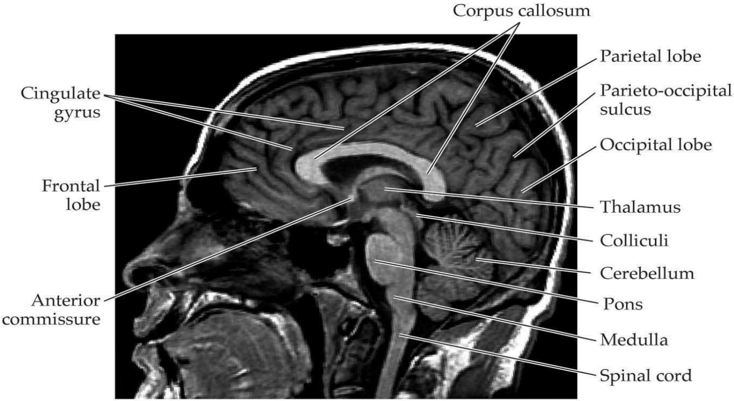
Paul Broca (1861)
Observed language-related deficits following left frontal damage to the brain.

Karl Wernicke (1874)
Reported language-related deficits and motor deficits following left temporal damage to the brain.

Wilder Penfield
(1937-1954)

Direct Cortical Stimulation





FUNCTIONAL MAGNETIC RESONANCE IMAGING, **Figure 6.19**

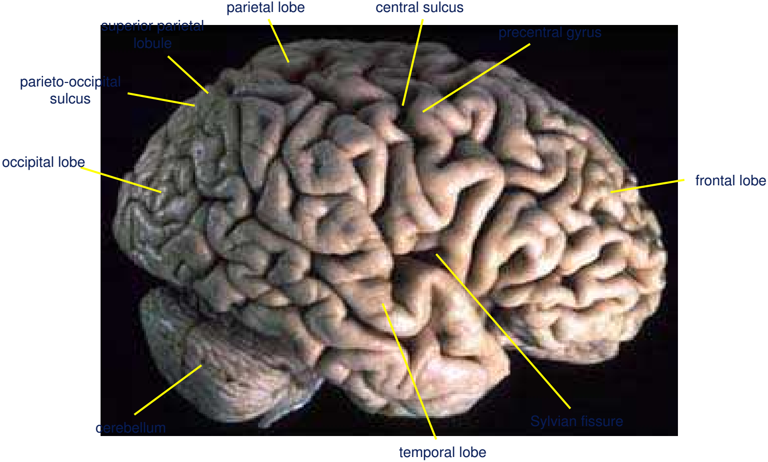
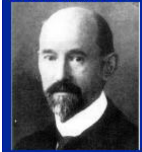
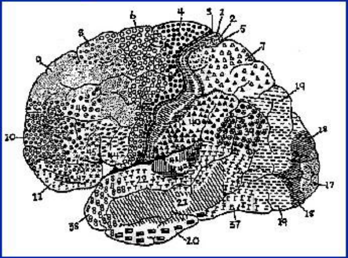

parietal lobe
central sulcus
superior parietal lobule
precentral gyrus
parieto-occipital sulcus
occipital lobe
frontal lobe
cerebellum
Sylvian fissure
temporal lobe

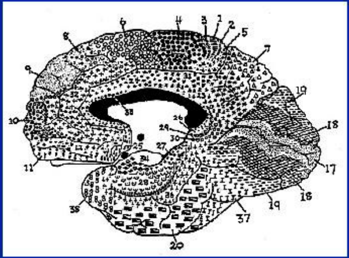
Fig 2.13

Korbinian
Brodmann 1909

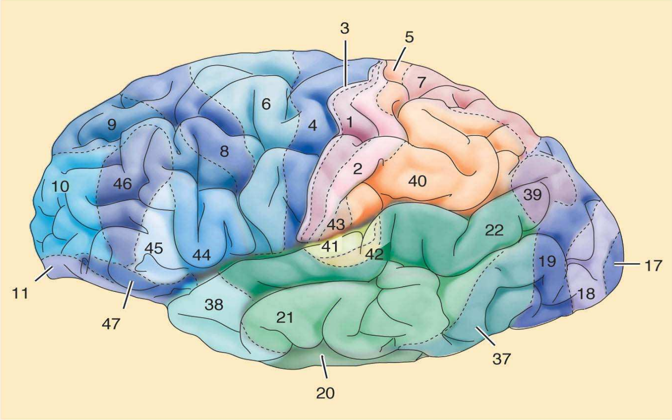


Cortical Cytoarchitecture



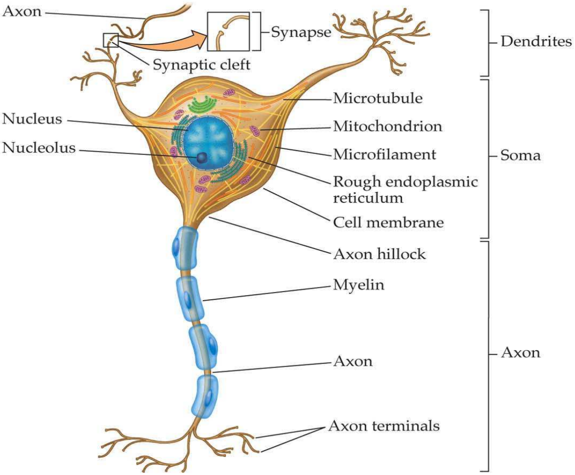


Cytoarchitectonic map, Brodman



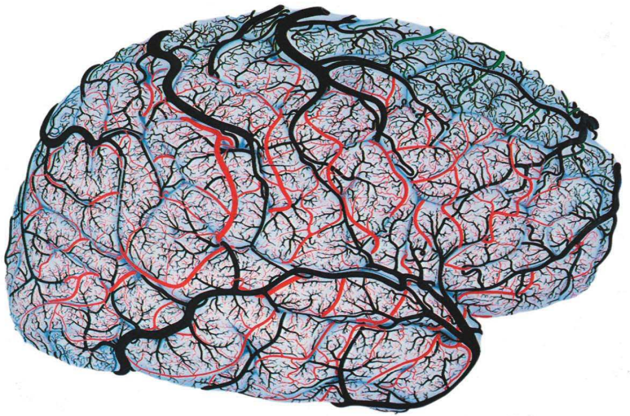
FUNCTIONAL MAGNETIC RESONANCE IMAGING, **Figure 6.22 (Part 1)**

Mikrostruktura



FUNCTIONAL MAGNETIC RESONANCE IMAGING, Figure 6.2

Zásobování mozku krví

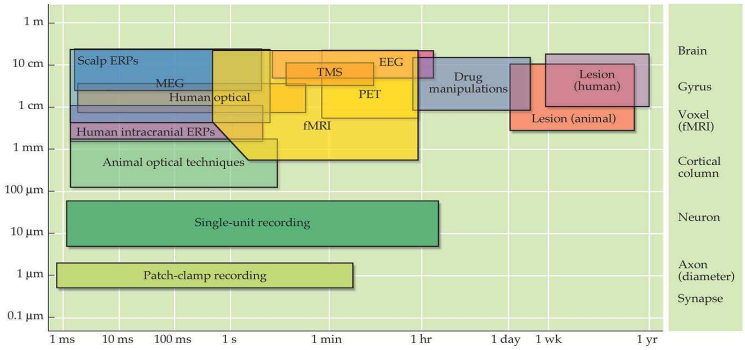


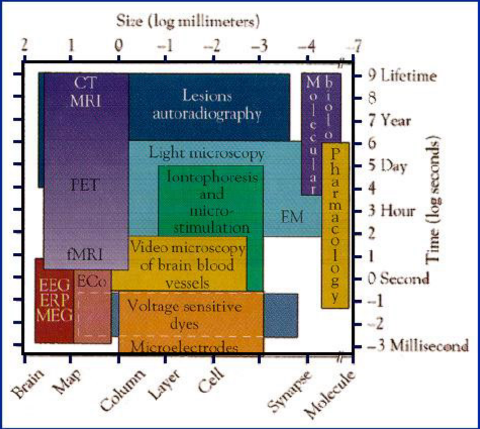
FUNCTIONAL MAGNETIC RESONANCE IMAGING, Figure 6.8

Jak lokalizovat funkci mozku

(Shrnutí a připomenutí)

- Invazivní
  - Následky zranění
  - Následky operací
  - Přímá stimulace (dnes jen na zvířatech)
  - Snímací elektrody
  - Optické snímání (při otevřené lebce svítíme laserem, optické vlastnosti se mění s průtokem krve a s elektrickým polem)
- Neinvazivní
  - MEG, EEG
  - fMRI
  - PET

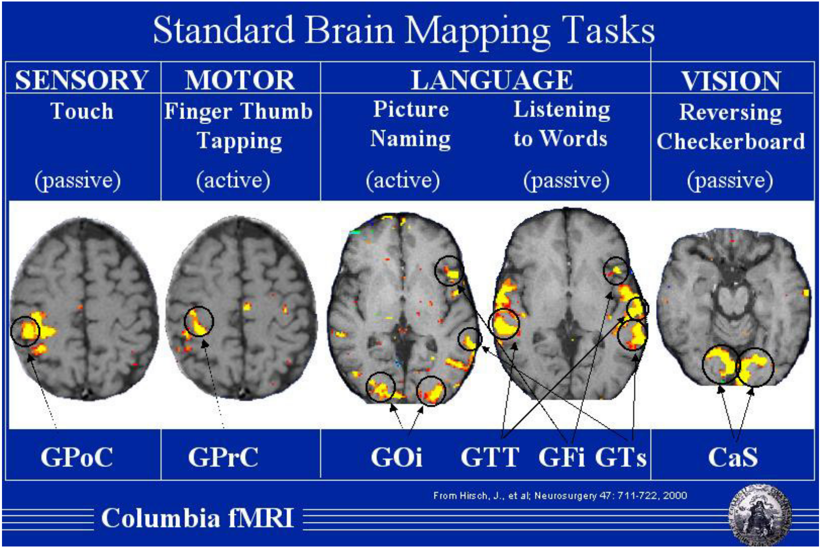

1 m
10 cm
1 cm
1 mm
100 µm
10 µm
1 µm
0.1 µm
1 ms
10 ms
100 ms
1 s
1 min
1 hr
1 day
1 wk
1 yr
Scalp ERPs
MEG
Human optical
Human intracranial ERPs
Animal optical techniques
TMS
EEG
PET
fMRI
Drug manipulations
Lesion (human)
Lesion (animal)
Single-unit recording
Patch-clamp recording
Brain
Gyrus
Voxel (fMRI)
Cortical column
Neuron
Axon (diameter)
Synapse



From: Images of Mind by Posner, M. and Raichle, M.
Scientific American Library, 1994, p. 24

Aplikace funkčního mapování mozku

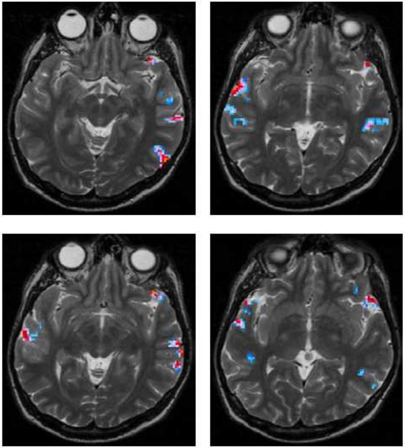
- Porozumění struktuře mozku
- Porozumění procesům vnímání a myšlení
- Nové terapie
  - Porozumění fyziologickým příčinám duševních chorob
  - Porozumění fyziologickým příčinám bolesti a reakci na bolest
  - Porozumění účinkům drog
- Plánování operací
  - Identifikace nefunkčního centra
  - Omezení poškození důležitých center při chirurgické léčbě (epilepsie)



Standard Brain Mapping Tasks
SENSORY
MOTOR
LANGUAGE
VISION
Touch
(passive)
Finger Thumb Tapping
(active)
Picture Naming
(active)
Listening to Words
(passive)
Reversing Checkerboard
(passive)
GPoC
GPrC
GOi
GTT
GFi
GTs
CaS
From Hirsch, J., et al; Neurosurgery 47: 711-722, 2000
Columbia fMRI

Funkční zobrazování (fMRI)

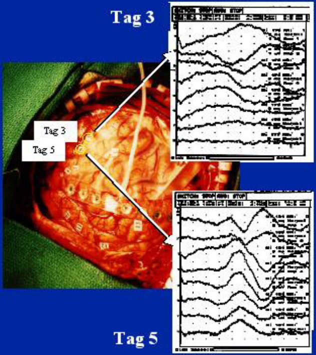
- Jsou vidět části mozku, které se používají při určité činnosti.
- Na obrázcích je činnost mozku při překladu slov.



Sensory Motor Mapping

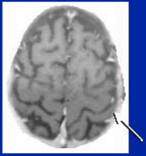
Craniotomy	SSEP	Direct Cortical Stimulation	Reference Image	fMRI Localization

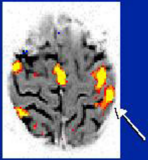
Tag 3



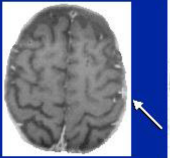
Tag 5

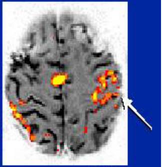
"Twitching of hand, focal seizure involving arm "





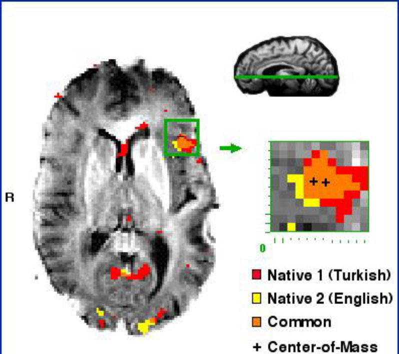
"Twitching in 1st three digits"



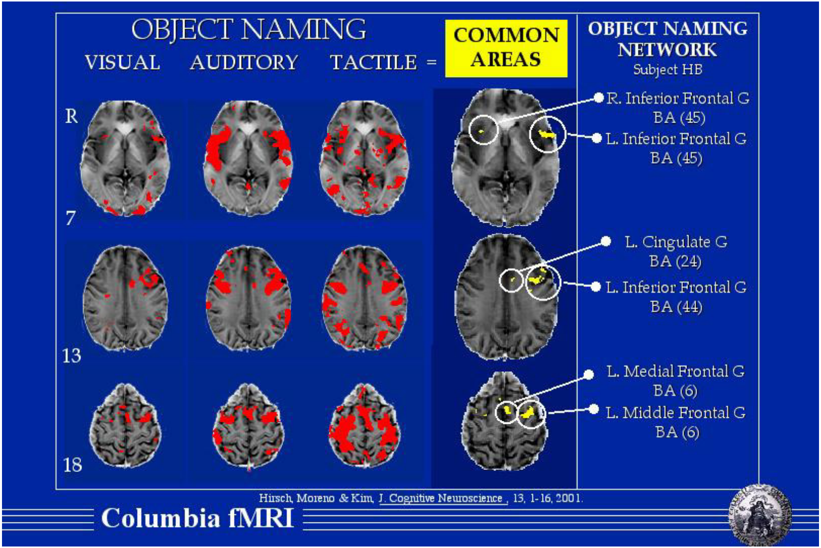


From Hirsch, J., et al; Neurosurgery 47: 711-722, 2000

"EARLY" BILINGUAL (Subject G)
ANTERIOR Language Area



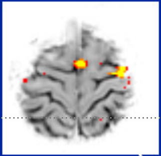
From Kim, et al, Nature, 388, 171-174, 1997



OBJECT NAMING
VISUAL
AUDITORY
TACTILE =
COMMON AREAS
OBJECT NAMING NETWORK
Subject HB
R
7
13
18
R. Inferior Frontal G BA (45)
L. Inferior Frontal G BA (45)
L. Cingulate G BA (24)
L. Inferior Frontal G BA (44)
L. Medial Frontal G BA (6)
L. Middle Frontal G BA (6)
Hirsch, Moreno & Kim, J. Cognitive Neuroscience, 13, 1-16, 2001.
Columbia fMRI

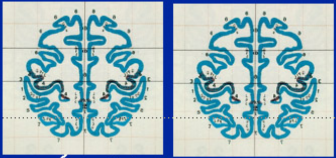
Labeling of Active Brain Areas

Functional Brain



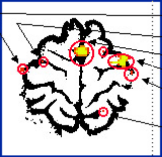
activity

Atlas Brain



labels

transfer



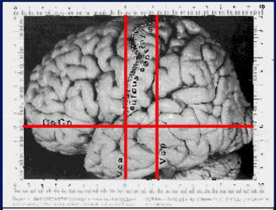
Name	BA	Sector
GPrC	4	c,E
GFs	6	b,E
GFd	6	a,E,60,-a
GFs	6	b,E,60
GRC	4	c,E,60
LPs	7	b,G,60

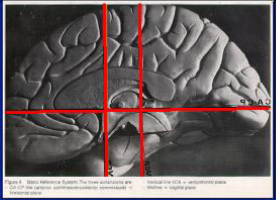
Co-Planar Stereotaxic Atlas of the Human Brain

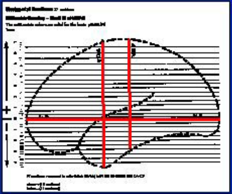
3-Dimensional Proportional System: An Approach to Cerebral Imaging

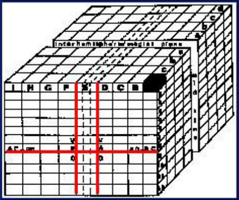
Jean Talairach
Pierre Tournoux

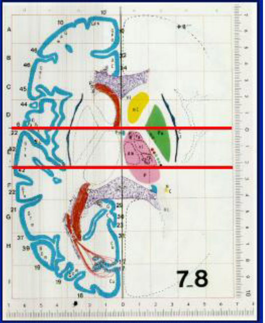
Translated by
Mark Rayport





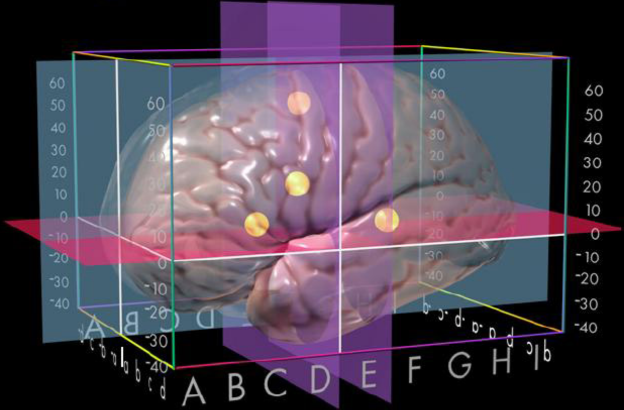






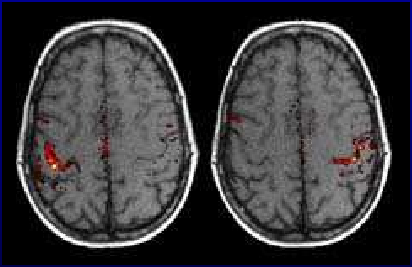
Columbia fMRI

Object Naming Network



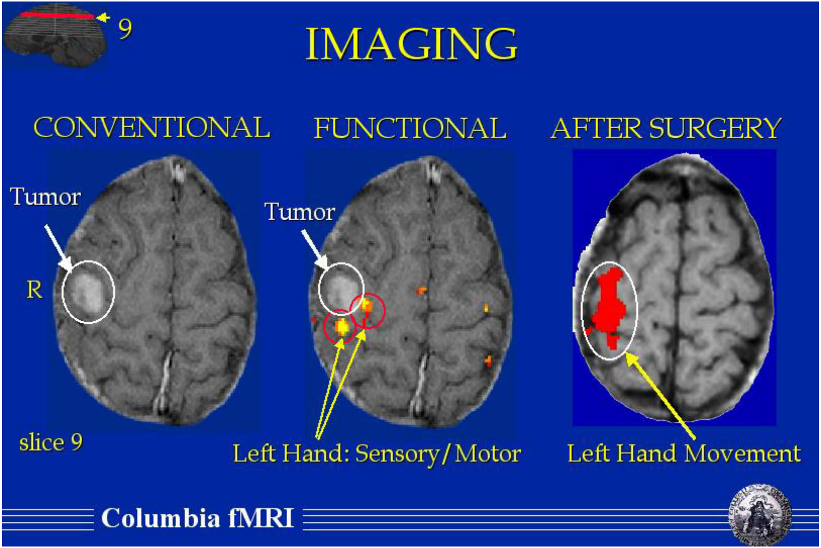
Hirsch, Moreno & Kim, J. Cognitive Neuroscience , 13, 1-16, 2001.

Application: (Neuro)functional MRI



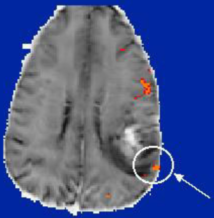
Volunteer

Patient w/ Glioblastoma

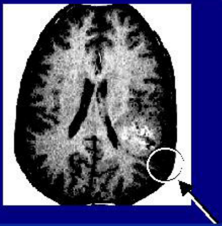

9
IMAGING
CONVENTIONAL
FUNCTIONAL
AFTER SURGERY
Tumor
R
Tumor
slice 9
Left Hand: Sensory/Motor
Left Hand Movement
Columbia fMRI

Intra-Operative Language Mapping

fMRI Map



Cortical Stimulation



Word finding difficulty during picture naming

From Hirsch, J., et al; Neurosurgery 47: 711-722, 2000

Essential Discoveries that enable PET and fMRI

Angelo Mosso

1881 Observed that blood flow changes were associated with mental activity

1890 Roy and Sherrington described an "intrinsic mechanism by which the vascular supply of the brain can be varied locally in correspondence with local variations in functional activity."

Linus Pauling

1936 Discovered the Magnetic Properties of Hgb

Siege Ogawa

1991 Discovered the Blood Oxygen Level Dependent (BOLD) Signal

PHYSIOLOGY

NEURAL ACTIVATION
IS ASSOCIATED WITH AN
INCREASE IN BLOOD FLOW

O2 EXTRACTION IS
RELATIVELY UNCHANGED

RESULT:
REDUCTION IN THE
PROPORTION OF DEOXY HGB
IN THE LOCAL VASCULATURE

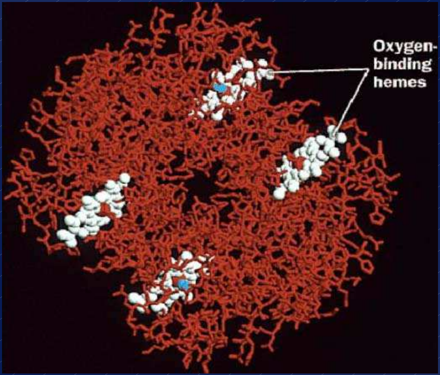
PHYSICS

DEOXY HGB
IS PARAMAGNETIC

AND DISTORTS THE LOCAL
MAGNETIC FIELD CAUSING
SIGNAL LOSS

RESULT:
LESS DISTORTION OF THE
MAGNETIC FIELD RESULTS IN
LOCAL SIGNAL INCREASE

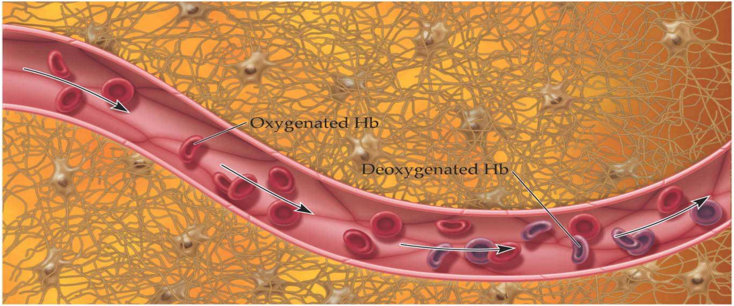
Hemoglobin Molecule



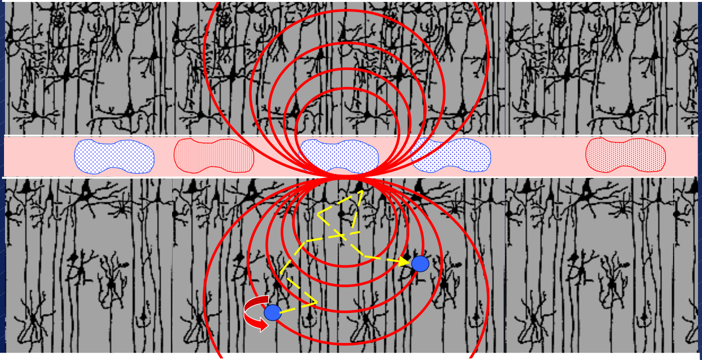
million Hb molecules per red blood cell

BOLD Signal Generation

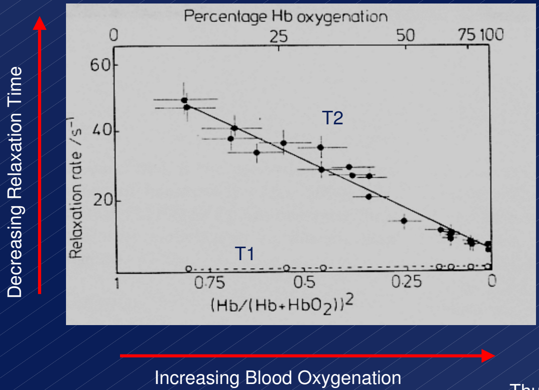
(B)



FUNCTIONAL MAGNETIC RESONANCE IMAGING, Figure 7.14 (Part 2)



Blood Deoxygenation affects T_2 Recovery

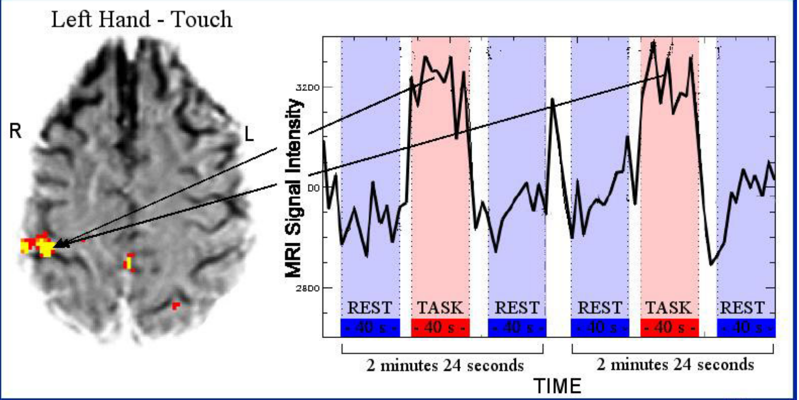


Thulborn et al., 1982

BOLD

- **B**lood **O**xygen **L**evel **D**ependent
- Gradient echo, EPI (kvůli rychlosti)
- Paramagnetické vlastnosti deoxyhemoglobinu $\longrightarrow$ nehomogenita pole $\longrightarrow$ T_2^* efekt
- Velmi slabý signál (SNR ≈ 0.1)
- Průměrování:
  - Opakujeme např. 10 bloků (snímání) bez aktivity
  - ... 10 bloků (snímání) s aktivitou

Magnetic Resonance Signals to Location of Function



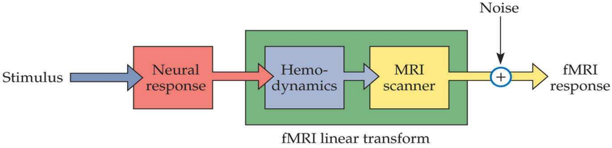
From Hirsch, J., et al; Neurosurgery 47: 711-722, 2000

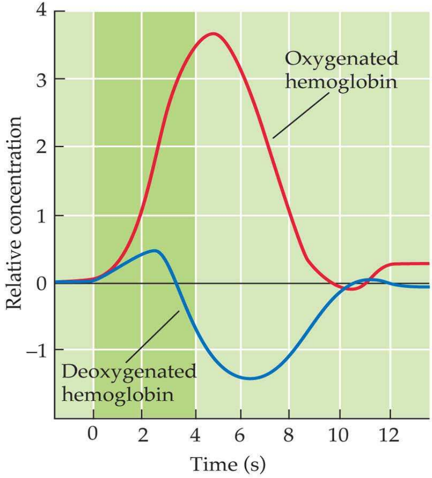
Hemodynamická odezva

Hemodynamic response

- Nervová aktivita $\longrightarrow$ zásobování krví $\longrightarrow$ BOLD signál
- Reakce není okamžitá, impulzní charakteristika se nazývá **hemodynamická odezva**
- Odezva se liší mezi subjekty i v rámci jednoho subjektu

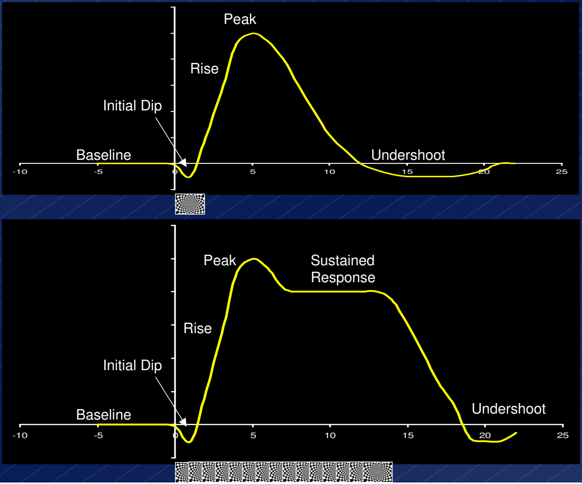
Hemodynamic response





FUNCTIONAL MAGNETIC RESONANCE IMAGING, **Figure 7.5**

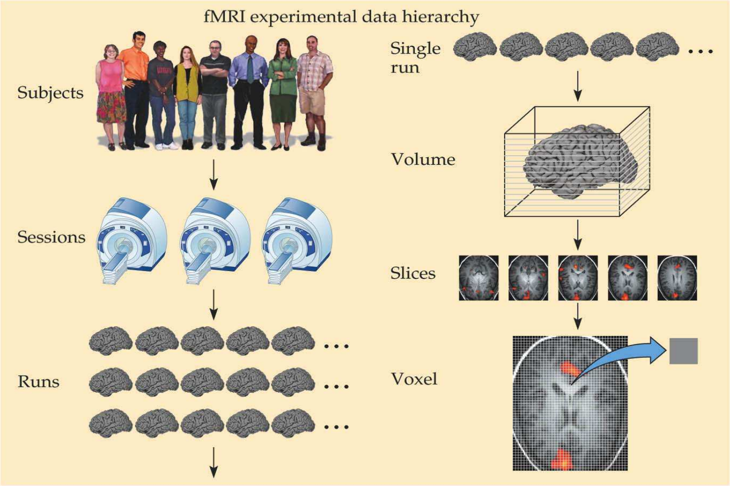
Basic Form of Hemodynamic Response



*f*MRI IMAGING PARAMETERS

SCANNER:	**GE Signa 1.5 T** **EPI Capability**
IN-PLANE RESOLUTION:	**1.5 mm x 1.5 mm**
SLICE THICKNESS:	**4.5 mm**
SLICE SEPARATION:	**0 mm**
NUMBER OF SLICES:	**21**
SLICE ORIENTATION:	**Axial on AC/PC Line**
RESONATOR:	**GE “bird cage”**
SEQUENCE:	**GRADIENT ECHO** **TR = 4000 msec TE = 60 msec** **Flip Angle = 60 deg**

Position of Headcoil and Mirror



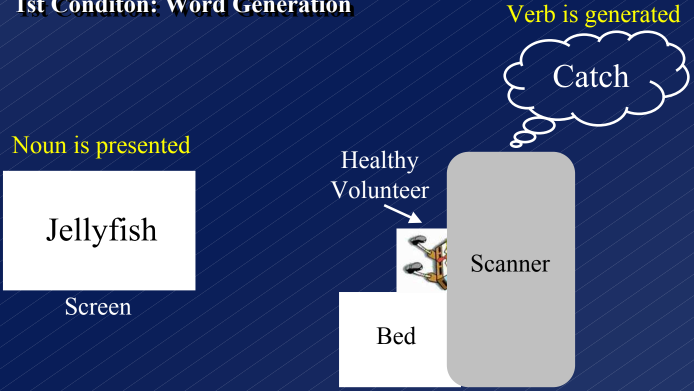
FUNCTIONAL MAGNETIC RESONANCE IMAGING, Figure 8.1

The Experiment:
fMRI adaptation of classic PET experiment

- Three Conditions in 21 second epochs
- 1st Conditon: Word Generation

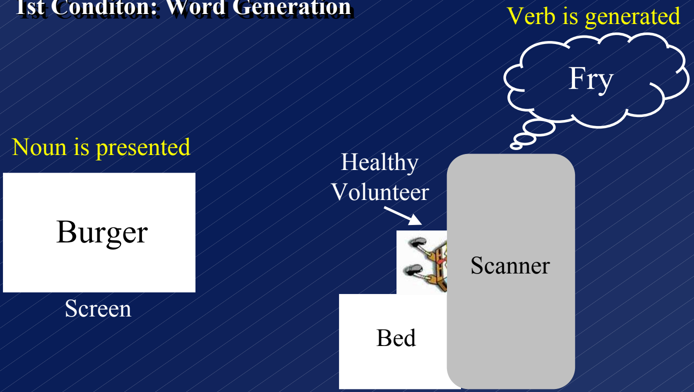
The Experiment:
fMRI adaptation of classic PET experiment

- **Three Conditions in 21 second epochs**
- **1st Conditon: Word Generation**



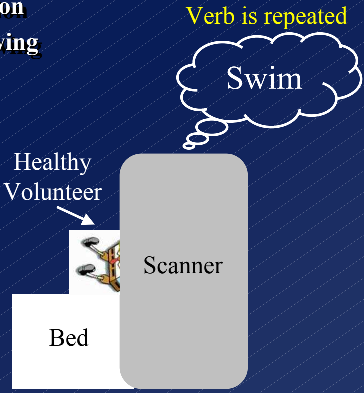
The Experiment:
fMRI adaptation of classic PET experiment

- **Three Conditions in 21 second epochs**
- **1st Conditon: Word Generation**



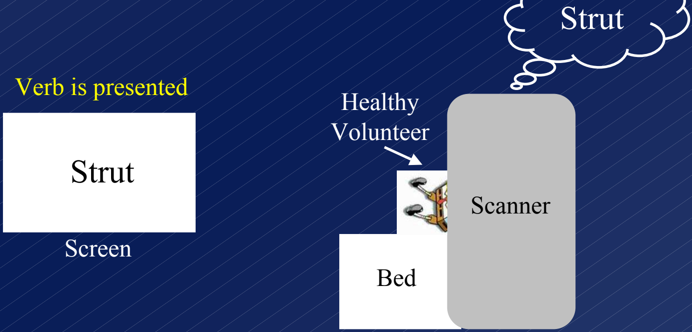
The Experiment:
fMRI adaptation of classic PET experiment

- Three Conditions in 21 second epochs
- 1st Conditon: Word Generation
- 2nd Condition: Word Shadowing



The Experiment:
fMRI adaptation of classic PET experiment

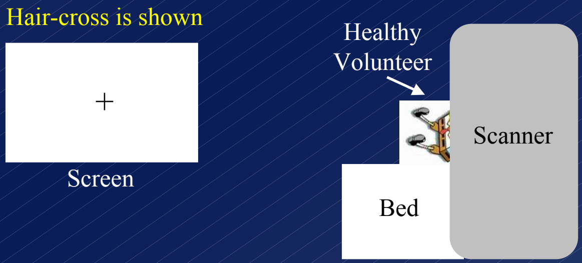
- **Three Conditions in 21 second epochs**
- **1st Conditon: Word Generation**
- **2nd Condition: Word Shadowing**



The Experiment:

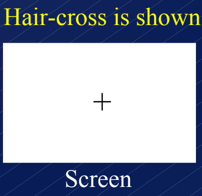
fMRI adaptation of classic PET experiment

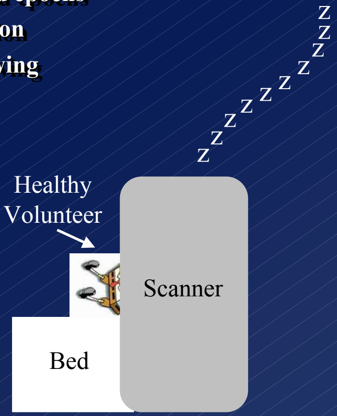
- **Three Conditions in 21 second epochs**
- **1st Conditon: Word Generation**
- **2nd Condition: Word Shadowing**
- **3rd Condition: Baseline**



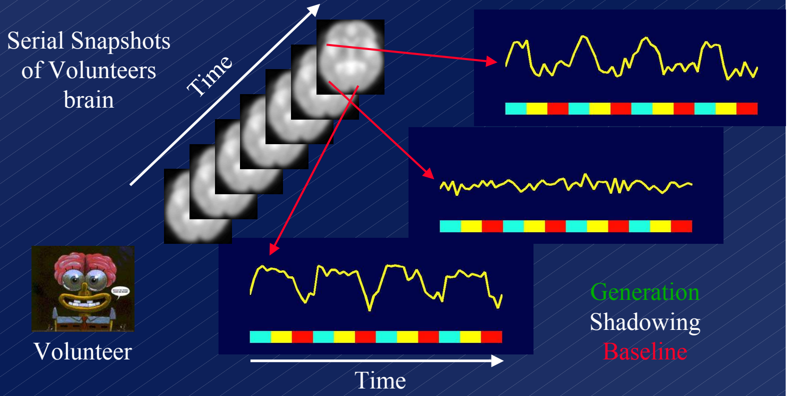
The Experiment:
fMRI adaptation of classic PET experiment

- **Three Conditions in 21 second epochs**
- **1st Conditon: Word Generation**
- **2nd Condition: Word Shadowing**
- **3rd Condition: Baseline**





The Data:
Set of Volumes <u>or</u> Set of Time-series



The Model:
A Set of Hypothetical Time-series

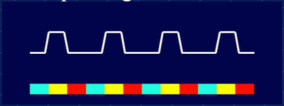
- **A model consists of a set of assumptions of the type:**

"I think a voxel that is into generating words might have a time-series looking like this"

Time

- **and**

"A voxel that is into repeating, like this"



and

"A voxel that just doesn't care, like this"

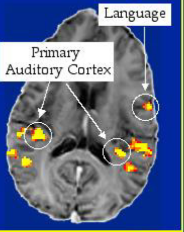
Generation Shadowing Baseline

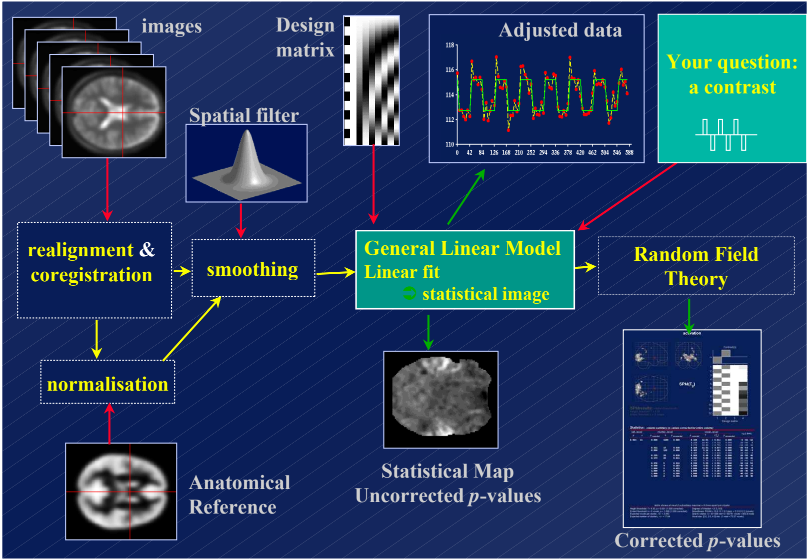
COMPUTATIONS FOR *f*UNCTIONAL IMAGE PROCESSING

Scanner

RECONSTRUCTION
ALIGNMENT
VOXEL BY VOXEL ANALYSIS
GRAPHICAL REPRESENTATION

Functional Brain Map



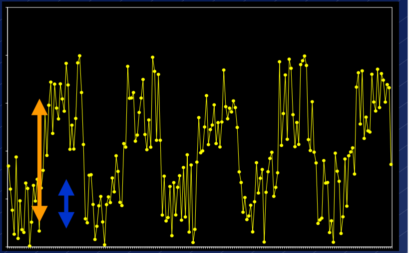


images
Design matrix
Adjusted data
Your question: a contrast
Spatial filter
realignment & coregistration
smoothing
General Linear Model
Linear fit
statistical image
Random Field Theory
normalisation
Anatomical Reference
Statistical Map
Uncorrected p-values
Corrected p-values

Signal-Noise-Ratio (SNR)

Task-Related Variability

Non-task-related Variability



What are typical SNRs for fMRI data?

- Signal amplitude
  - MR units: 5-10 units (baseline: ~700)
  - Percent signal change: 0.5-2%
- Noise amplitude
  - MR units: 10-50
  - Percent signal change: 0.5-5%
- SNR range
  - Total range: 0.1 to 4.0
  - Typical: 0.2 – 0.5

Types of Noise

- Thermal noise
  - Responsible for variation in background
  - Eddy currents, scanner heating
- Power fluctuations
  - Typically caused by scanner problems
- Variation in subject cognition
  - Timing of processes
- Head motion effects
- Physiological changes
- Differences across brain regions
  - Functional differences
  - Large vessel effects
- Artifact-induced problems

Variability in Subject Behavior: Issues

- **Cognitive processes are not static**
  - **May take time to engage**
  - **Often variable across trials**
  - **Subjects' attention/arousal wax and wane**
- **Subjects adopt different strategies**
  - **Feedback- or sequence-based**
  - **Problem-solving methods**
- **Subjects engage in non-task cognition**
  - **Non-task periods do not have the absence of thinking**

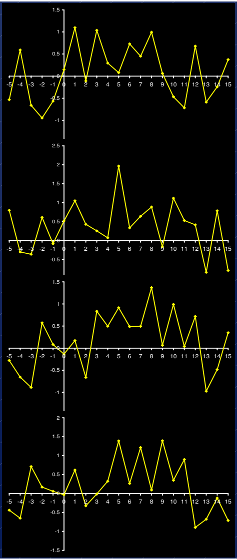
What can we do about these problems?

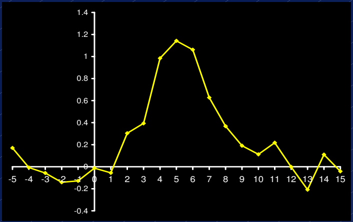
Trial Averaging

- Static signal, variable noise
  - Assumes that the MR data recorded on each trial are composed of a signal + (random) noise

- Effects of averaging
  - Signal is present on every trial, so it remains constant through averaging
  - Noise randomly varies across trials, so it decreases with averaging
  - Thus, SNR increases with averaging

Trial averaging

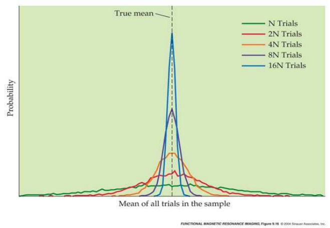




Average of 16 trials with SNR = 0.6

Fundamental Rule of SNR

For Gaussian noise, experimental power increases with the square root of the number of observations



Caveats

- Signal averaging is based on assumptions
  - Data = signal + temporally invariant noise
  - Noise is uncorrelated over time
- If assumptions are violated, then averaging ignores potentially valuable information
  - Amount of noise varies over time
  - Some noise is temporally correlated (physiology)
- Nevertheless, averaging provides robust, reliable method for determining brain activity

Signal, noise, and the General Linear Model

$$Y = \alpha M + \varepsilon$$

Measured Data

Amplitude (solve for)

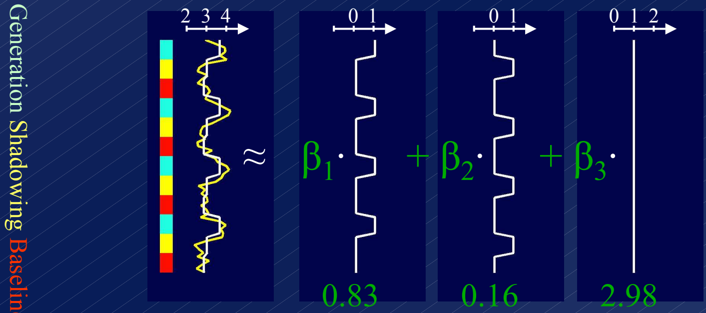
Design Model

Noise

Cf. Boynton et al., 1996

The Estimation: Finding the ”best” parameter values

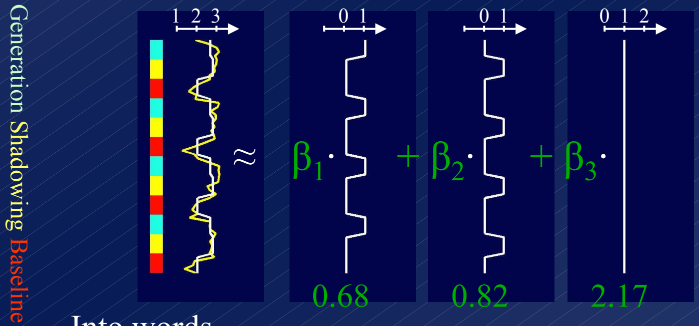
- The estimation entails finding the parameter values such that the linear combination ”best” fits the data.



Cool!

The Estimation: Finding the "best" parameter values

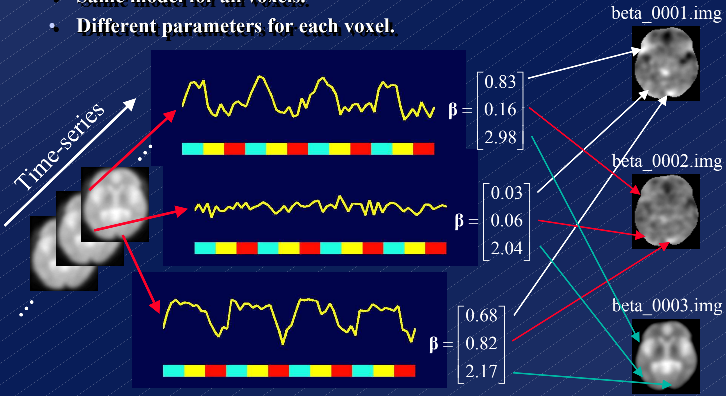
- And the nice thing is that the same model fits all the time-series, only with different parameters.



Into words

The Estimation:
The format of data, model and parameters

- Same model for all voxels.
- Different parameters for each voxel.

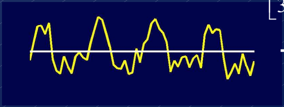


The estimation revisited
What do I mean by ”best” fit

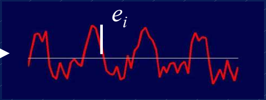
— Data

— Some fit

$$\boldsymbol{\beta} = \begin{bmatrix} 0 \\ 0 \\ 3.31 \end{bmatrix}$$



— Error



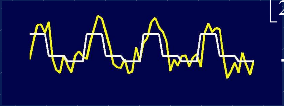
$$\sum_{i=1}^{n} e_i^2 = 17.16$$

$$\sum_{i=1}^{n} e_i = 0$$

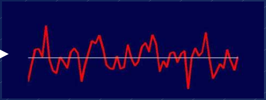
— Data

— Best fit

$$\boldsymbol{\beta} = \begin{bmatrix} 0.83 \\ 0.16 \\ 2.98 \end{bmatrix}$$



— Error

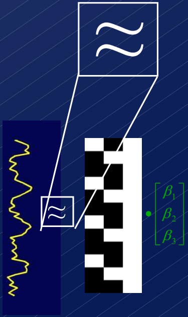


$$\sum_{i=1}^{n} e_i^2 = 9.47$$

$$\sum_{i=1}^{n} e_i = 0$$

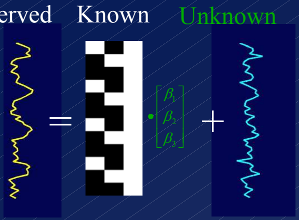
Model revisited – again

Now, what's that all about?



Remember?

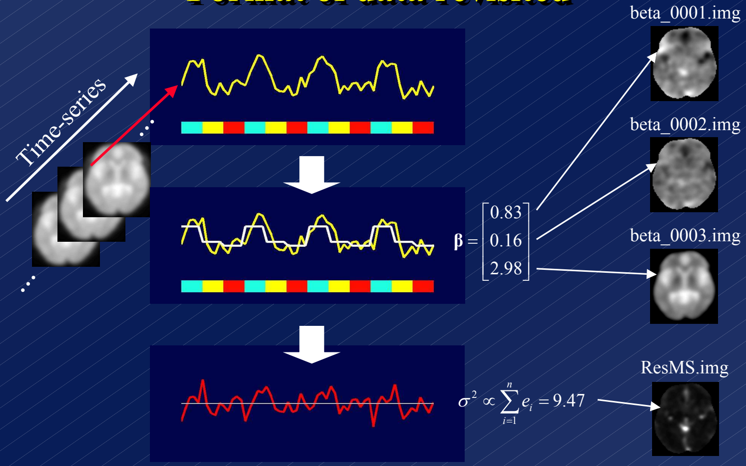
We need a model for the error!



$$\mathbf{y} = \mathbf{X}\boldsymbol{\beta} + \mathbf{e}$$

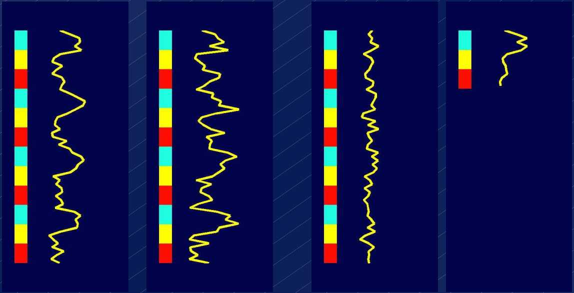
$$\mathbf{e} \sim N(\mathbf{0}, \sigma^2\mathbf{I})$$

Format of data revisited



But why do we need the error?

Would you trust these?



$\beta_1=1$	$\beta_1=1$	$\beta_1=0.3$	$\beta_1=1$
$\sigma=0.2$	$\sigma=0.5$	$\sigma=0.2$	$\sigma=0.2$
$n=60$	$n=60$	$n=60$	$n=15$

But why do we need the error?
In conclusion:

- We trust long series with large effects and small error.

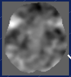
$$t = \frac{\mathbf{c}^T \boldsymbol{\beta}}{\sigma \sqrt{\mathbf{c}^T (\mathbf{X}^T \mathbf{X})^{-1} \mathbf{c}}}$$

Effect size

Uncertainty of effect size

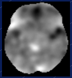
t-test

- We trust: Long series with large effects and small error.

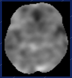


$$t = \frac{\mathbf{c}^T \beta}{\sigma \sqrt{\mathbf{c}^T (\mathbf{X}^T \mathbf{X})^{-1} \mathbf{c}}}$$

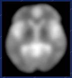
beta_0001.img



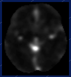
beta_0002.img



beta_0003.img



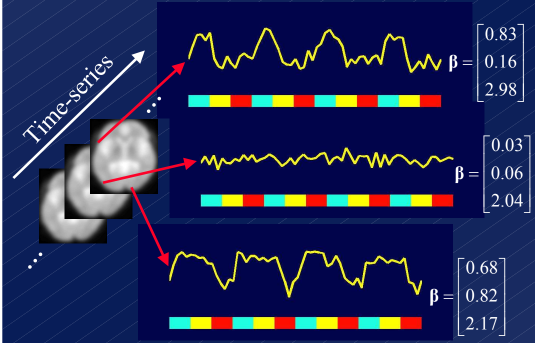
ResMS.img



?

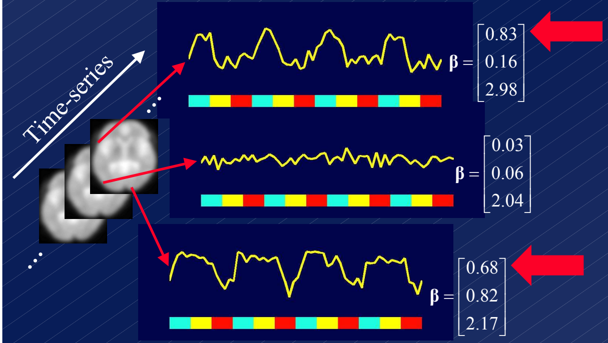
Asking questions of your data
t-contrasts

- Can we find voxels that are active in word-generation taks?



Asking questions of your data
t-contrasts

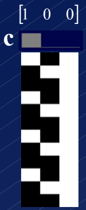
- Can we find voxels that are active in word-generation taks?

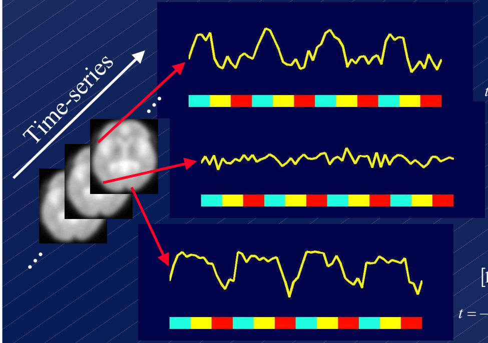


Hmm, seem to have large values for β_1

Asking questions of your data
t-contrasts

- **Can we find voxels that are active in word-generation taks?**





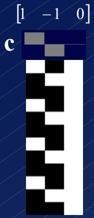
$$t = \frac{\begin{bmatrix}1 & 0 & 0\end{bmatrix}\begin{bmatrix}0.83\\0.16\\2.98\end{bmatrix}}{0.41*0.32} = \frac{0.83}{0.41*0.32} = 6.42^{**}$$

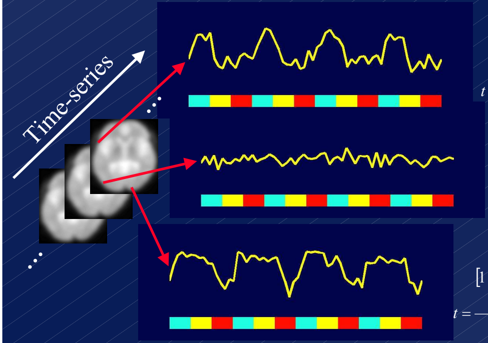
$$t = \frac{\begin{bmatrix}1 & 0 & 0\end{bmatrix}\begin{bmatrix}0.03\\0.06\\2.04\end{bmatrix}}{0.19*0.32} = \frac{0.03}{0.19*0.32} = 0.44$$

$$t = \frac{\begin{bmatrix}1 & 0 & 0\end{bmatrix}\begin{bmatrix}0.68\\0.82\\2.17\end{bmatrix}}{0.40*0.32} = \frac{0.68}{0.40*0.32} = 5.41^{**}$$

Asking questions of your data
t-contrasts

- Voxels that are <u>more</u> active in generation than shadowing?





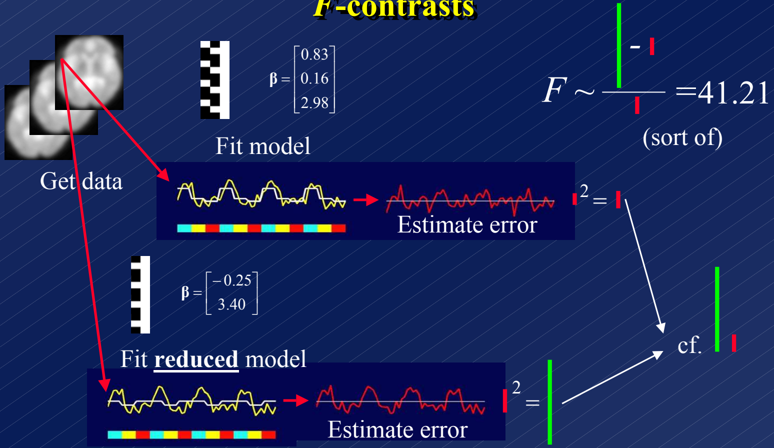
$$t = \frac{\begin{bmatrix}1 & -1 & 0\end{bmatrix}\begin{bmatrix}0.83\\0.16\\2.98\end{bmatrix}}{0.41*0.32} = \frac{0.67}{0.41*0.32} = 5.16^{**}$$

$$t = \frac{\begin{bmatrix}1 & -1 & 0\end{bmatrix}\begin{bmatrix}0.03\\0.06\\2.04\end{bmatrix}}{0.19*0.32} = \frac{-0.03}{0.19*0.32} = -0.58$$

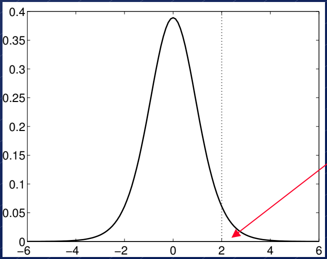
$$t = \frac{\begin{bmatrix}1 & -1 & 0\end{bmatrix}\begin{bmatrix}0.68\\0.82\\2.17\end{bmatrix}}{0.40*0.32} = \frac{-0.14}{0.40*0.32} = -1.12$$

I'm sorry, can you pose that question differently?

F-contrasts



Inference at a single voxel



u=2

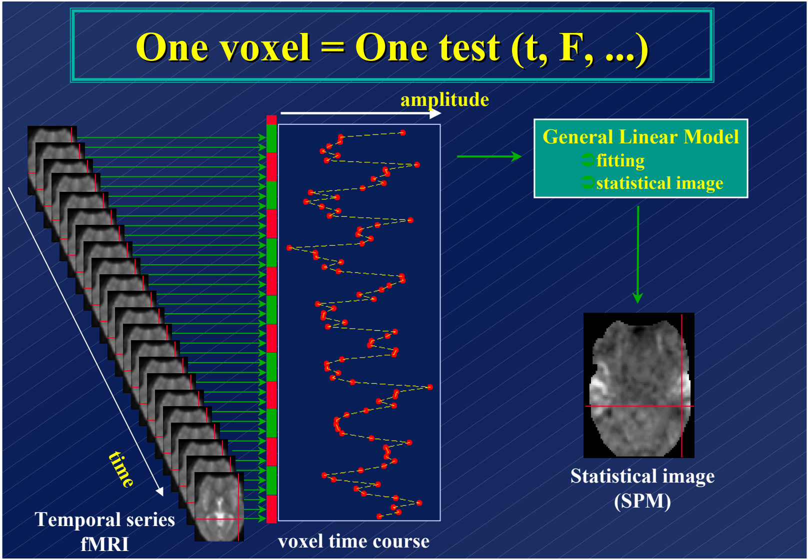
t-distribution

NULL hypothesis, H: activation is zero

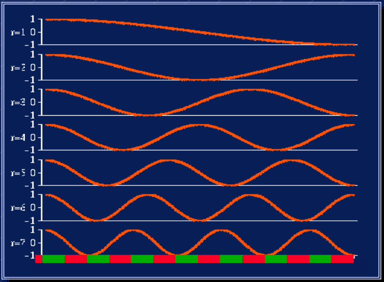
$\alpha = p(t>u|H)$

p-value: probability of getting a value of t at least as extreme as u. If α is small we reject the null hypothesis.

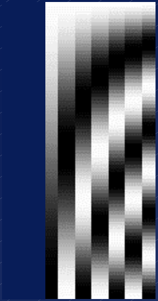
u=(effect size)/std(effect size)


One voxel = One test (t, F, ...)
amplitude
General Linear Model
fitting
statistical image
time
Temporal series
fMRI
voxel time course
Statistical image
(SPM)

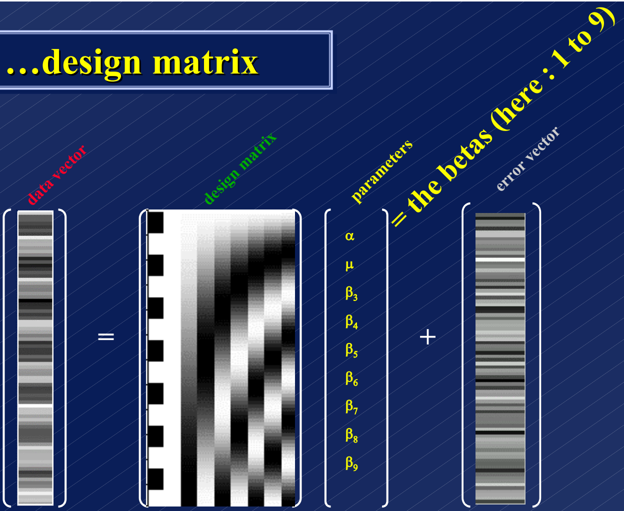
Add more reference functions ...



Discrete cosine transform basis functions

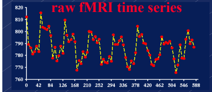


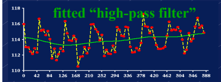
…design matrix

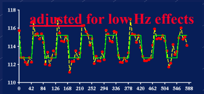


$$Y = X \times \beta + \varepsilon$$

Fitting the model = finding some estimate of the betas = minimising the sum of square of the residuals S^2

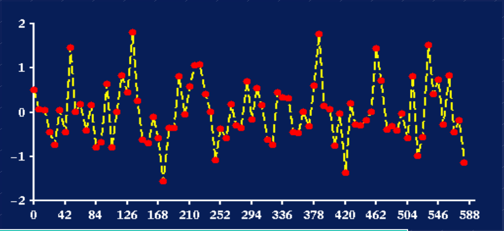






fitted box-car

residuals



$$\frac{\sum \text{the squared values of the residuals}}{\text{number of time points minus the number of estimated betas}} = s^2$$

Summary ...

- *We put in our model regressors (or covariates) that represent how we think the signal is varying (of interest and of no interest alike)*

- *Coefficients (= parameters) are estimated using the Ordinary Least Squares (OLS) or Maximum Likelihood (ML) estimator.*

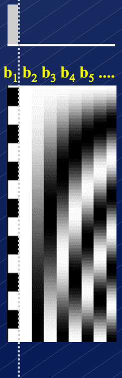
- *These estimated parameters (the "betas") **depend** on the scaling of the regressors.*

- *The residuals, their sum of squares and the resulting tests (t,F), **do not** depend on the scaling of the regressors.*

T test - one dimensional contrasts - SPM{t}

A contrast = a linear combination of parameters: $c' \times \beta$

$c' = 1\ 0\ 0\ 0\ 0\ 0\ 0\ 0$



box-car amplitude > 0 ?

=

$\beta_1 > 0$?

=>

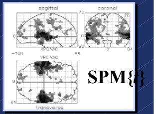
Compute $1 \mathrm{x} b_1 + 0 \mathrm{x} b_2 + 0 \mathrm{x} b_3 + 0 \mathrm{x} b_4 + 0 \mathrm{x} b_5 + \ldots$

and

divide by estimated standard deviation

$$T = \frac{\textit{contrast of estimated parameters}}{\sqrt{\text{variance estimate}}}$$

$$T = \frac{c'b}{\sqrt{s^2 c'(X'X)^+ c}}$$

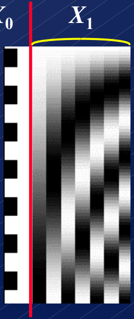


F-test (SPM{*F*}) : a reduced model or ...

Tests multiple linear hypotheses : Does X1 model anything ?

H_0: True (reduced) model is X_0

X_0 X_1



→ S^2

This (full) model ?

X_0

→ S_0^2

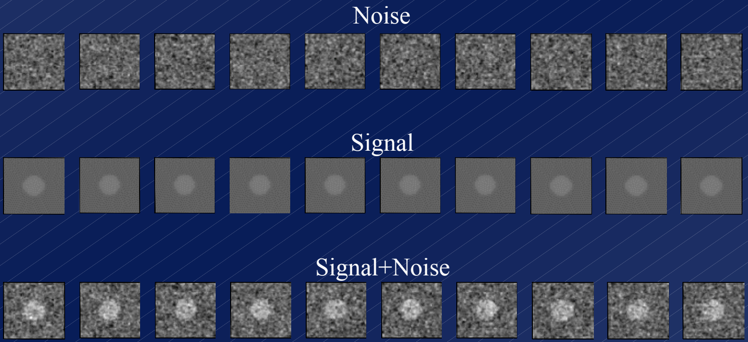
Or this one?

$$F = \frac{\text{additional variance accounted for by tested effects}}{\text{error variance estimate}}$$

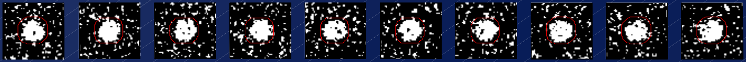
$$F \sim (S_0^2 - S^2) / S^2$$

Bonferroni correction

Inference for Images



Use of ‘uncorrected’ p-value, $\alpha=0.1$



11.3% 11.3% 12.5% 10.8% 11.5% 10.0% 10.7% 11.2% 10.2% 9.5%

Percentage of Null Pixels that are False Positives

Using an ‘uncorrected’ p-value of 0.1 will lead us to conclude on average that 10% of voxels are active when they are not.

This is clearly undesirable. To correct for this we can define a null hypothesis for images of statistics.

Family-wise Null Hypothesis

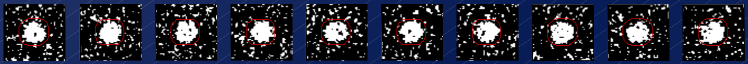
FAMILY-WISE NULL HYPOTHESIS:
Activation is zero everywhere

If we reject a voxel null hypothesis
at *any* voxel, we reject the family-wise
Null hypothesis

A FP **anywhere** in the image
gives a Family Wise Error (FWE)

Family-Wise Error (FWE) rate = ‘corrected’ p-value

Use of ‘uncorrected’ p-value, α=0.1



Use of ‘corrected’ p-value, α=0.1

FWE

The Bonferroni correction

The Family-Wise Error rate (FWE), α, for a family of N **independent** voxels is

$$\alpha = Nv$$

where v is the voxel-wise error rate. Therefore, to ensure a particular FWE set

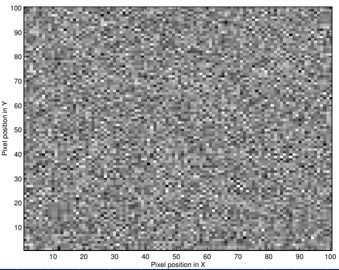
$$v = \alpha / N$$

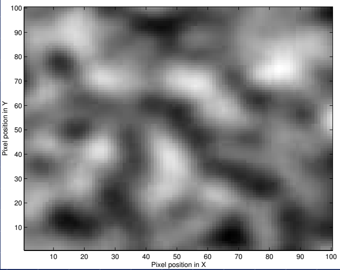
BUT ...

The Bonferroni correction

Independent Voxels

Spatially Correlated Voxels





Bonferroni is too conservative for brain images

Applied Smoothing

Smoothness

smoothness » voxel size

practically

$FWHM \geq 3 \times \texttt{VoxDim}$

Typical applied smoothing:

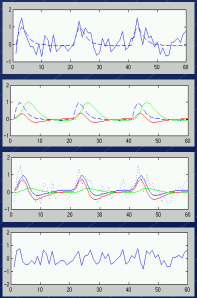
Single Subj fMRI: 6mm

PET: 12mm

Multi Subj fMRI: 8-12mm

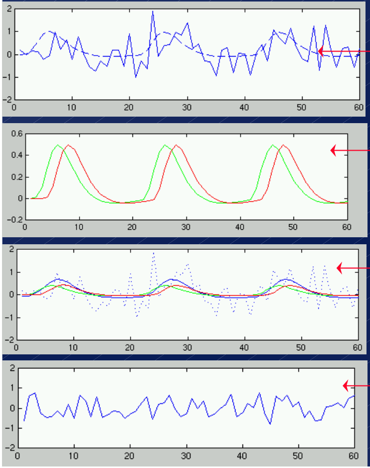
PET: 16mm

Summary ... (2)



- *The residuals should be looked at ...(non random structure ?)*
- *We rather test flexible models if there is little a priori information, and precise ones with a lot a priori information*
- *In general, use the F-tests to look for an overall effect, then look at the betas or the adjusted data to characterise the response shape*
- *Interpreting the test on a single parameter (one regressor) can be difficult: cf the delay or magnitude situation*

Correlation between regressors



True signal

Model (green and red)

Fit (blue : global fit)

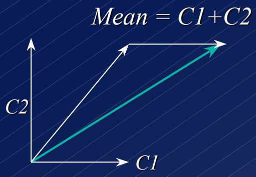
Residual

"completely" correlated ...

$$Y = Xb + e$$

$$X = \begin{matrix} 1 & 0 & 1 \\ 0 & 1 & 1 \\ 1 & 0 & 1 \\ 0 & 1 & 1 \end{matrix}$$

Cond 1 *Cond 2* *Mean*



Parameters are not unique in general ! Some contrasts have no meaning: NON ESTIMABLE

Summary ... (3)

- *We implicitly test for an additional effect only, so we may miss the signal if there is some correlation in the model*

- *Orthogonalisation is not generally needed - parameters and test on the changed regressor don't change*

- *It is always simpler (if possible!) to have orthogonal regressors*

- *In case of correlation, use F-tests to see the overall significance. There is generally no way to decide to which regressor the « common » part should be attributed to*

- *In case of correlation and if you need to orthogonolise a part of the design matrix, there is no need to re-fit a new model: change the contrast*

What is fMRI Experimental Design?

- Controlling the timing and quality of cognitive operations (IVs) to influence resulting brain processes (DVs)

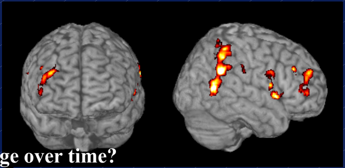
- What can we control?
  - Experimental comparisons (what is to be measured?)
  - Stimulus properties (what is presented?)
  - Stimulus timing (when is it presented?)
  - Subject instructions (what do subjects do with it?)

Refractory Periods

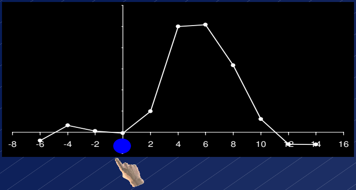
- Definition: a change in the responsiveness to an event based upon the presence or absence of a similar preceding event
  - Neuronal refractory period
  - Vascular refractory period

Detection vs. Estimation

- Detection: What is active?



- Estimation: How does activity change over time?



fMRI Design Types

1) Blocked Designs
2) Event-Related Designs
   a) Periodic Single Trial
   b) Jittered Single Trial
   c) Staggered or Interleaved Single Trial
3) Mixed Designs
   a) Combination blocked/event-related
   b) Variable stimulus probability

fMRI Design Types

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What are Blocked Designs?

- Blocked designs segregate different cognitive processes into distinct time periods

Task A	Task B	Task A	Task B	Task A	Task B	Task A	Task B

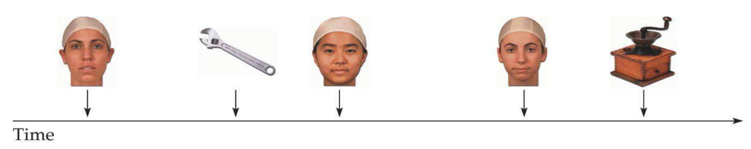
Task A	REST	Task B	REST	Task A	REST	Task B	REST

Limitations of Blocked Designs

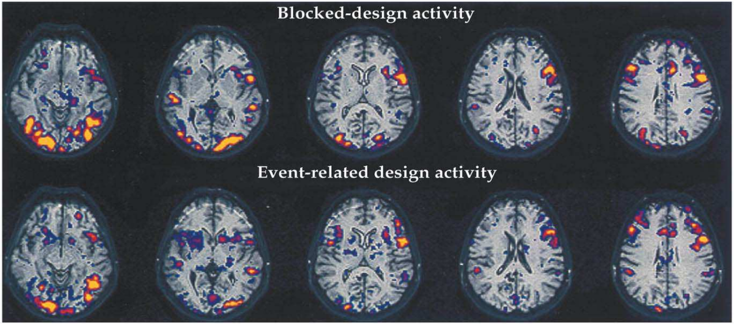
- Very sensitive to signal drift
  - Sensitive to head motion, especially when only a few blocks are used.
- Poor choice of baseline may preclude meaningful conclusions
- Many tasks cannot be conducted repeatedly
- Difficult to estimate the HDR

What are Event-Related Designs?

- Event-related designs associate brain processes with discrete events, which may occur at any point in the scanning session.



(A)



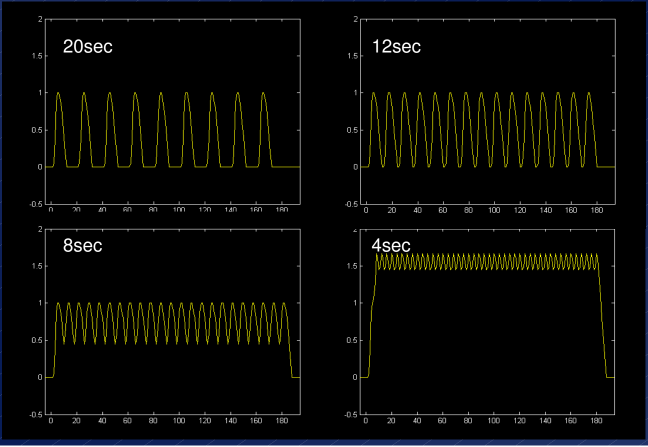
Word-stem completion task. Blocked design: 30s on/off. Event-related design: 15s ISI.

Buckner et al., (1996)

2a. Periodic Single Trial Designs

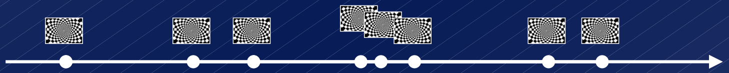
- Stimulus events presented infrequently with long interstimulus intervals

Trial Spacing Effects: Periodic Designs

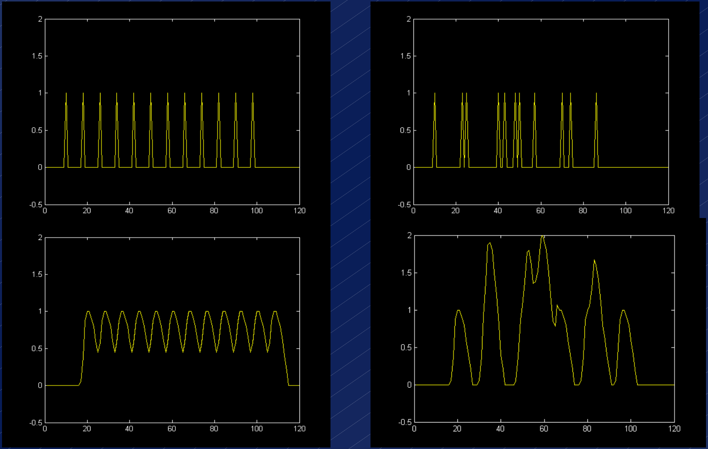


2b. Jittered Single Trial Designs

- Varying the timing of trials within a run
- Varying the timing of events within a trial



Effects of Jittering on Stimulus Variance

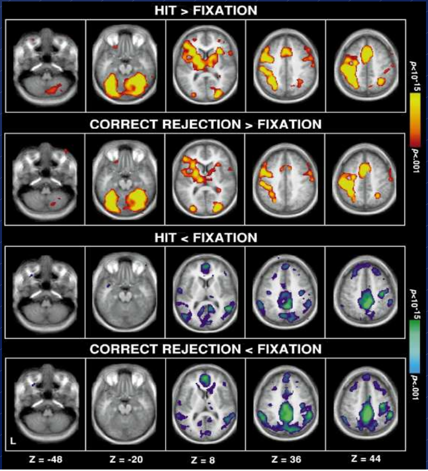


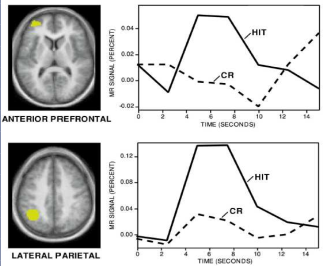
Post-hoc sorting

Dodatečné třídění

- Rozhodneme se až dodatečně (podle výsledku experimentu), do které kategorie pokus zařadíme.
- **Typický příklad:** Subjekt odpověděl správně/špatně.

Post-Hoc Sorting of Trials





Data from old/new episodic memory test.

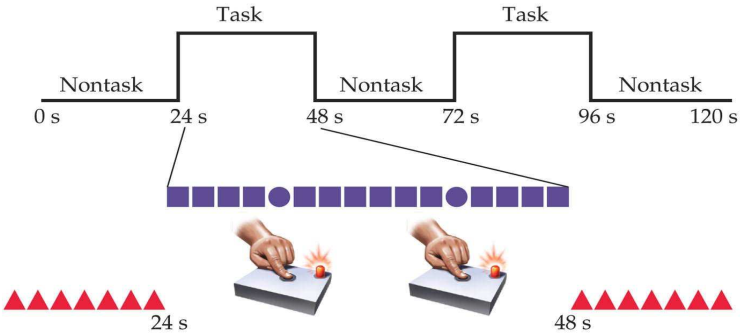
From Konishi, et al., 2000

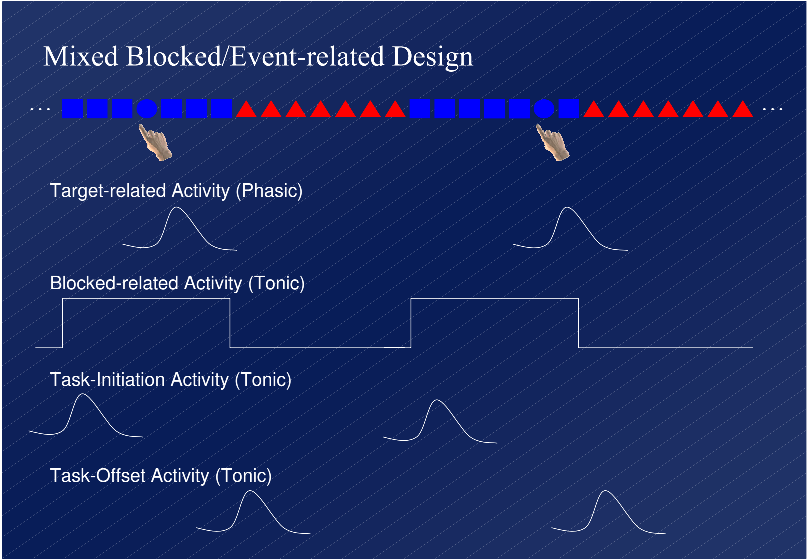
Limitations of Event-Related Designs

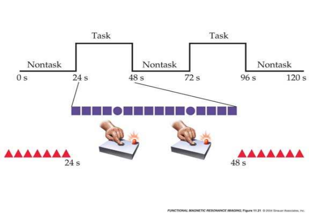
- **Differential effects of interstimulus interval**
  - **Long intervals do not optimally increase stimulus variance**
  - **Short intervals may result in refractory effects**
- **Detection ability dependent on form of HDR**
- **Length of "event" may not be known**

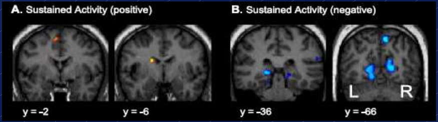
3a. Combination Blocked/Event

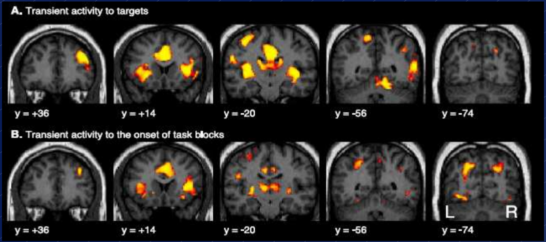
- Both blocked and event-related design aspects are used (for different purposes)
  - Blocked design is used to evaluate *state-dependent* effects
  - Event-related design is used to evaluate *item-related* effects
- Analyses are conducted largely independently between the two measures
  - Cognitive processes are assumed to be independent


Task
Task
Nontask
Nontask
Nontask
0 s
24 s
48 s
72 s
96 s
120 s
24 s
48 s


Mixed Blocked/Event-related Design
Target-related Activity (Phasic)
Blocked-related Activity (Tonic)
Task-Initiation Activity (Tonic)
Task-Offset Activity (Tonic)


Task
Task
Nontask
Nontask
Nontask
0 s
24 s
48 s
72 s
96 s
120 s
24 s
48 s

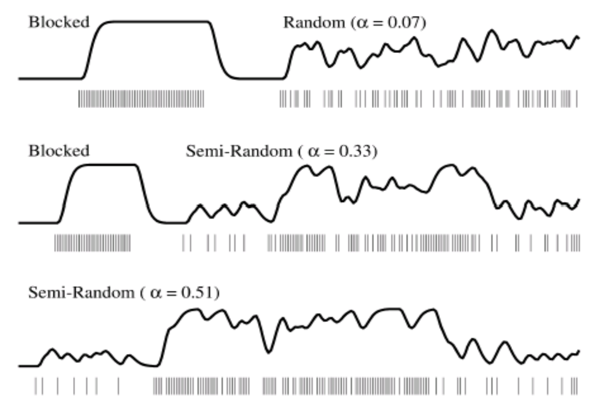

A. Sustained Activity (positive)
B. Sustained Activity (negative)
L
R
y = -2
y = -6
y = -36
y = -66


A. Transient activity to targets
y = +36
y = +14
y = -20
y = -56
y = -74
B. Transient activity to the onset of task blocks
L
R
y = +36
y = +14
y = -20
y = -56
y = -74

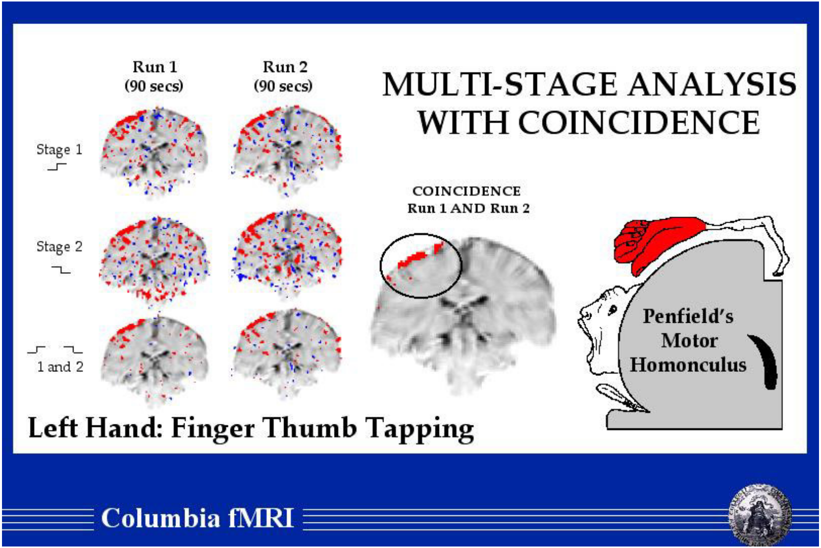
3b. Variable Stimulus Probability

- Stimulus probability is varied in a blocked fashion
  - Appears similar to the combination design
- Mixed design used to maximize experimental power for single design
- Assumes that processes of interest do not vary as a function of stimulus timing
  - Cognitive processing
  - Refractory effects

Random and Semi-Random Designs



From Liu et al., 2001


MULTI-STAGE ANALYSIS
WITH COINCIDENCE
Run 1
(90 secs)
Run 2
(90 secs)
Stage 1
Stage 2
1 and 2
COINCIDENCE
Run 1 AND Run 2
Penfield's
Motor
Homonculus
Left Hand: Finger Thumb Tapping
Columbia fMRI

Summary of Experiment Design

- Main Issues to Consider
  - What design constraints are induced by my task?
  - What am I trying to measure?
  - What sorts of non-task-related variability do I want to avoid?
- Rules of thumb
  - Blocked Designs:
    - Powerful for detecting activation
    - Useful for examining state changes
  - Event-Related Designs:
    - Powerful for estimating time course of activity
    - Allows determination of baseline activity
    - Best for post hoc trial sorting
  - Mixed Designs
    - Best combination of detection and estimation
    - Much more complicated analyses

MRI — závěr

- 3D zobrazování
- Výborné prostorové rozlišení
- Neinvazivní
- Obrovská variabilita — nejuniverzálnější ze zobrazovacích technik

MRI — závěr

- ⊕ 3D zobrazování
- ⊕ Výborné prostorové rozlišení
- ⊕ Neinvazivní
- ⊕ Obrovská variabilita — nejuniverzálnější ze zobrazovacích technik
- ⊖ Cena
- ⊖ Silná (elektro)magnetická pole — opatrnost nutná
- ⊖ Nepohodlí — hluk, stísněný prostor

fMRI — závěr

- ⊕ Lze zjistit, kde mozek pracuje
- ⊕ In-vivo
- ⊕ Neinvazivní
- ⊕ Relativně dobré prostorové rozlišení
- ⊖ Špatné časové rozlišení
- ⊖ Nutnost průměrování (nelze snímat ojedinělé jevy)